A Review of Mesoporous Silica Nanoparticle Delivery Systems in

Chemo-based Combination Cancer Therapies

- 1 Ying Gao^{1,2}, Dongruo Gao^{1,3}, Jie Shen^{1*}, Qiwen Wang^{4*}
- 2 ¹ Department of Pharmacy, School of Medicine, Zhejiang University City College,
- 3 Hangzhou 310015, P. R. China
- 4 ² Department of Pharmaceutics, College of Pharmaceutical Sciences, Zhejiang
- 5 University, Hangzhou 310058, P. R. China
- 6 ³ College of Chemical and Biological Engineering, Zhejiang University, Zhejiang,
- 7 Hangzhou 310027, P. R. China
- 8 ⁴ Department of Cardiology, The First Affiliated Hospital, Zhejiang University School
- 9 of Medicine, Hangzhou 310003, P. R. China

10 * Correspondence:

- 11 Jie Shen; Qiwen Wang
- 12 shenj@zucc.edu.cn; wangqiwen@zju.edu.cn

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15 Abstract

16 Chemotherapy is an important anti-tumor treatment in clinic to date, however, the effectiveness of traditional chemotherapy is limited by its poor selectivity, high 17 18 systemic toxicity, and multidrug resistance. In recent years, mesoporous silica nanoparticles (MSNs) have become exciting drug delivery systems (DDS) due to their 19 20 unique advantages, such as easy large-scale production, adjustable uniform pore size, 21 large surface area and pore volumes. While mesoporous silica-based DDS can 22 improve chemotherapy to a certain extent, when used in combination with other 23 cancer therapies MSN based chemotherapy exhibits a synergistic effect, greatly 24 improving therapeutic outcomes. In this review, we discuss the applications of MSN 25 DDS for a diverse range of chemotherapeutic combination anti-tumor therapies, including phototherapy, gene therapy, immunotherapy and other less common 26 27 modalities. Furthermore, we focus on the characteristics of each nanomaterial and the 28 synergistic advantages of the combination therapies. Lastly, we examine the 29 challenges and future prospects of MSN based chemotherapeutic combination 30 therapies.

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1 1 Introduction

2 Despite the rapid development of medicine, the incidence and mortality of cancers 3 are consistently rising and cancer remains one of the most terrible threats to human 4 lives (Siegel et al., 2020). Traditional chemotherapy is one of the most common cancer 5 treatments and is the most effective systemic treatment, playing an irreplaceable role in 6 current treatment modality (Dai et al., 2016). However, the clinical application of 7 chemotherapy is limited by several deficiencies: First, most chemotherapy drugs have 8 poor aqueous solubility or short half-life in vivo, leading to low drug utilization. Second, 9 chemotherapeutic drugs show poor tumor selectivity (Akhtar et al., 2014), resulting in 10 the undifferentiated killing of both tumor and healthy cells. This nontargeted lethality 11 not only reduces the therapeutic effect against carcinomas but also causes severe side 12 effects. Last, is the multidrug resistance (MDR) induced by chemotherapy. MDR refers 13 to the resistance of cancer cells to a variety of drugs which are structurally and 14 functionally unassociated (Kong M, 2017). This phenomenon is one of the primary 15 causes of chemotherapy failure, leading to the recurrence of tumors, patient relapse, 16 or even death (Wang et al., 2017a).

17 Recent years have witnessed many efforts to overcome the shortcomings of 18 conventional chemotherapy. One of the most promising is the development of nano 19 drug delivery systems (nano-DDS), which can increase the solubility and 20 bioavailability of drugs, prolong the circulation time of drugs, increase the 21 accumulation of drugs in tumor tissues, and improve the pharmacokinetic behaviour in 22 vivo, improving the curative effect of therapies while reducing the side effects (Mu et 23 al., 2020). Common nanocarriers include polymers (Alsehli, 2020), liposomes (Allen 24 and Cullis, 2013), dendrimers (Dias et al., 2020), inorganic nanoparticles like gold 25 nanoparticles (GNPs) (Ajnai et al., 2014), and carbon nanomaterials (Chen et al., 26 2015a). Among these nano-DDS, mesoporous silica nanoparticles (MSNs) are a class 27 of materials that have garnered particular focused by many researchers, due to their 28 facile large-scale production, adjustable uniform pore size (Bouchoucha et al., 2016), 29 and large surface area and pore volume (Farjadian et al., 2019). These properties 30 endow MSNs with good drug encapsulation efficiency and delivery, with 31 uncomplicated preparation like the sol-gel "chimiedouce" methods in aqueous 32 solutions (Jonas G. Croissant, 2018). Since silica-based materials have been 33 considered safe by Food and Drug Administration, dedicated efforts have been made 34 to utilize MSNs to construct nanoplatforms for drug delivery and cancer 35 chemotherapy (Li et al., 2019a). MSN DDS design has been extremely versatile. 36 Some researchers have used active targeting groups to improve MSNs tumor targeting 37 and improve chemotherapy selectivity (Cheng et al., 2015; Liang Chen, 2016; Murugan 38 et al., 2017), while others rely on the characteristics of the tumor microenvironment, 39 such as lower pH and higher glutathione (GSH) content than normal cells. Many pH

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1 and/or redox responsive MSNs to release chemotherapeutic drugs have been designed

2 (Cheng et al., 2017; Murugan et al., 2017; Cheng et al., 2019b). Enzyme, thermal, and

3 ultrasound responsive MSN DDS have also been studied (Dandan Zhu;Baisong

4 Chang, 2013;Li et al., 2018a). More recently, dual therapeutic agents co-delivered by

5 MSNs to exert synergistic action and improve the effect of chemotherapy have been 6 investigated (Zhang et al., 2015c;Murugan et al., 2016;Wang et al., 2018b;Li et al.,

7 2019b;Yang Xing, 2020) (Figure 1).



8 9

Figure 1. Versatile design of MSN DDS

10 The mechanisms of cancer occurrence involves multiple pathways (Xu et al., 11 2015; Qiu et al., 2018a), therefore it is unlikely that a single therapeutic mechanism 12 will be sufficient to completely eradicate cancer. In support of this supposition, every 13 therapy mode including chemotherapy, has demonstrated drawbacks (Fan et al., 14 2017). Combining chemotherapy with other treatment modalities is a good strategy to 15 combat these shortcomings and augment therapeutic efficacy. Furthermore, chemotherapeutic combination therapies can reduce drug dosage to patients, 16 17 lightening side effects while enhancing efficacy(Yu et al., 2018;Shrestha et al., 18 2019; Zhang et al., 2019). Combination chemotherapy possesses great potential for 19 cancer treatment_(Goldin, 1980).

In this review, we summarize the progress made on MSN based chemo-combination therapies according to the different combination treatment modalities (Figure 2). We focus on the synergistic therapeutic effects achieved by these combined systems, emphasizing the advantages of combination therapy over

- 1 monotherapy and highlighting how a successful combination compensates for the
- 2 shortcomings of chemotherapy. Then, we conclude with the challenges faced by MSN
- 3 based combination chemotherapy systems and what improvements are needed for
- 4 these treatment systems to become mainstays in cancer therapy.



6 Figure 2. MSN nano-DDS in chemotherapeutic combination cancer therapies

7 2 Chemotherapy and phototherapy

8 Phototherapy, including photodynamic therapy (PDT) and photothermal therapy 9 (PTT), is a non-invasive therapeutic strategy commonly used as a supplement to 10 chemotherapy in order to overcome the deficits of the monotherapy (Qin et al., 2018; Cheng et al., 2020b). In the presence of light, photoactive therapeutics 11 12 (photosensitizers) of PDT or PTT are excited to produce reactive oxygen species (ROS) 13 or hyperthermia to kill cancer cells (Robertson et al., 2009;Chen et al., 2019b). The 14 high surface area, large pore size and pore volume of MSNs make them ideal candidates for multi-drug loading and therefore, a combined platform for 15 photo-chemotherapy. In the following section we summarize photoactive mesoporous 16 17 silica-based chemotherapeutic nanoplatforms according to the modality of 18 phototherapy used in the combination (Table 1).

19 2.1 Photodynamic-chemotherapy

20 PDT is an emerging therapeutic procedure in cancer treatment that has attracted 21 significant attention due to its high selectivity, noninvasive nature and minimal side 22 effects, when compared to conventional therapy (Liao et al., 2016). Photosensitizer

1 (PS) selection, tissue oxygen levels, and light wavelength are all key factors of PDT. 2 Briefly summarized, under a specific wavelength of light, the PS transfers absorbed 3 energy to oxygen, inducing a transformation from its triplet ground state to its singlet 4 excited state and instigating cytotoxic effects (Leonidova et al., 2014). Due to the 5 limited tissue penetration depths of most wavelengths used to activate PSs, PDT is 6 nonviable for deep-seated tumors or metastasis. However, since the ROS generation 7 from PDT has been reported to promote anti-cancer drug release (Chen et al., 2016a; Cheng et al., 2019a; Wong et al., 2020), a combination of PDT and 8 9 chemotherapy could to enhance the therapeutic outcomes of both treatments.

10 MSNs have attracted substantial attention as a potential PDT partner in recent 11 years, due to their structural merits. Many PSs aggregate easily (reducing their 12 efficacy) and have a poor intracellular uptake, limiting their applicability in solid 13 tumors (Ding et al., 2018;Oh et al., 2019;Fu et al., 2020). Integration with MSNs can 14 prevent the aggregation of PSs as well as improve the targeting ability and 15 biocompatibility of PSs, leading to reduced side-effects and stronger anticancer 16 efficacy (Zhao et al., 2010; Yao et al., 2015; Yang et al., 2016b). Several MSN vehicles 17 have been reported to be able to co-deliver anti carcinogens and PSs into cancer cells 18 (Zhang et al., 2016;Kankala et al., 2017;Chen et al., 2020;Fu et al., 2020;Wang et al., 19 2020a), and these studies showed several advantages to these combination systems 20 such as enhanced biocompatibility, improved cellular uptake of the payloads, and 21 enhanced therapeutic efficiency (Yan et al., 2018). In one such example, Fang and 22 coworkers (Fang et al., 2019) designed a hollow MSN nanoparticles (HMSNs) based 23 nanoplatform into which the chemotherapeutic agent DOX and photosensitizer 24 chlorine e6 (Ce6) were co-loaded at 9.56% and 16.68% (w/w), respectively. The 25 HMSNs-DOX-Ce6 were further modified with bovine serum albumin integrated 26 manganese dioxide nanoparticles (BSA-MnO₂) to construct a multifunctional 27 therapeutic nanoplatform the authors named BMHDC. In which, BSA is intended to 28 improve biocompatibility and tumor accumulation while MnO2 serves to elevate the 29 oxygen content within the hypoxic tumors. Combination index (CI) analysis indicated 30 a great synergy between PDT and chemotherapy in BMHDC (CI = 0.21). In another 31 study, Guo et al. (Guo et al., 2020) decorated MSNs with Au nanoparticles as PSs and 32 mPEG-SH as a GSH-triggered gatekeeper to create a reduction-responsive 33 MSN-Au-PEG nanoplatform. The spherical structure of MSN-Au-PEG was 34 maintained, with a particle size of approximately 155 nm. The pore diameter of 35 MSN-Au decreased from 3.37 nm to 2.67 nm after coating with mPEG-SH. The 36 particles achieved a drug loading content (DLC) and drug loading efficiency (DLE) 37 for DOX of 12.3% and 43.25%, respectively. Cytotoxicity assays in Hela cells 38 demonstrated that MSN-Au-PEG@DOX with laser irradiation exhibited the lowest 39 cell viability (30%) compared with the non-illuminated group (40%) or the free DOX 40 group (35%). The above results indicated that the nanoplatform displayed a

significant enhancement to carcinoma inhibition due to the synergistic effect of
 PDT-chemotherapy.

3 2.2 Photothermal-chemotherapy

4 PTT employs a photothermal agent (PA) to convert light energy into heat, as 5 opposed to ROS in PDT, and induce the thermal ablation of cancer cells (Zhi et al., 6 2020). Similarly to PDT, PTT is a noninvasive therapeutic modality with advantages 7 of simplicity, minimal side effects, and remote activation. However, as with PDT 8 limited light penetration and inevitable light scattering make PTT alone insufficient to 9 completely eliminate tumors (Li et al., 2018b). Since the hyperthermia produced by 10 PTT can enhance cellular metabolism and cell membrane permeability, the concept 11 behind combination photothermal-chemotherapy is to not only improve the uptake of 12 chemotherapy drugs but also prevent tumor recurrence (Zheng et al., 2013;Wang et al., 13 2017b). As tumors have a higher sensitivity to many chemotherapeutics at elevated 14 temperatures (Hauck et al., 2008), the cytotoxicity of chemotherapy can be increased, 15 thereby the dosage of anticancer drugs can be reduced and systemic side-effects minimized (Yang et al., 2017). 16

17 In recent years, MSNs have emerged as powerful candidates for DDSs and they 18 have been widely used for the codelivery of PA and chemotherapy drugs as a 19 combination therapy (Shu et al., 2018; Tian et al., 2018). Copper sulfide nanoparticles 20 (CuS NPs) (Chen et al., 2015b;Zhang et al., 2015a;Zhang et al., 2015b;Peng et al., 21 2017; Wang et al., 2018a; Li et al., 2020), polydopamine (PDA) (Zhang et al., 22 2018; Chen et al., 2019a), gold nanorods (AuNR) (Zhang et al., 2012; Liu et al., 23 2015;Huang et al., 2017;Ramasamy et al., 2018;Sun et al., 2018b;Wang et al., 2019b), 24 gold shells (Rahman et al., 2017), reduced graphene oxide (rGO) (Liu et al., 2019), 25 GO (Tang et al., 2015; Tran et al., 2018) and carbon dots (CDs) (Singh et al., 26 2016;Zhang et al., 2020b) are common PAs introduced in the PTT-chemotherapy 27 systems. Wang and coworkers (Wang et al., 2015) developed a DOX-loaded 28 amino-modified MSNs (DOX@MSN-NH2) with the DOX loading content of 20.9 wt% 29 and modified with reduced graphene oxide (rGO) as a heating gatekeeper coat to 30 achieve a multifunctional DDS. rGO possess a strong NIR absorption at 980 nm (a 31 wavelength with good tissue penetration) and acts as the PA in this work, converting 32 NIR light energy into hermal energy to kill cancer cells. This nanocomposite was able 33 to kill 68% of HEp-2 cells in synergistic therapy, compared with 54% in PTT and 33% 34 in chemotherapy alone. This *in vitro* result illustrates that the combination of PTT and 35 chemotherapy enables a better therapeutic outcome than the monotherapies. Another 36 rGO and MSNs based nanoplatform (162 nm) loaded with (S)-(+)-camptothecin (CPT) 37 for PTT-chemotherapy was also reported to have a great synergistic effect. While 38 DOX killed 33.4% of cells, and PTT killed 52% of cells, their combination was able 39 to kill 68% of cells (Chen et al., 2014).

Black phosphorus (BP) is a new PTT agent featuring low cytotoxicity, good biocompatibility, and efficient photothermal performance (Qiu et al., 2018b). In one study utilizing this new PA, Ren et al. (Ren et al., 2020) constructed a MSNs based platform (150nm) loaded with DOX and black phosphorus quantum dots (BPQDs) together. The *in vitro* results showed that the multimodal therapy of PTT and chemotherapy could induce a higher cell death rate (73.5%) in tumors compared to chemotherapy alone (64.78%).

8 2.3 Photodynamic-photothermal-chemotherapy

9 Since both PDT and PTT are triggered by light irradiation, integrating both 10 methods with chemotherapy into a trimodal nanosystem seems a viable approach. Indeed, this combination has already proven to have superior therapeutic efficacy than 11 any mono or dual therapy (Yang et al., 2016a) and there have been numerous attempts 12 13 to integrate both of the phototherapeutics and chemotherapeutics into MSN-based 14 single formulation (Luo et al., 2016;Sun et al., 2018a;Yan et al., 2020). Fang et al. 15 (Fang et al., 2017a) synthesized mesoporous silica-coated gold nanorods (100 nm) 16 loaded with 5-fluorouracil (5-FU) and conjugated to indocyanine green (ICG). With 17 5-FU, ICG, and the gold nanorods (GNR) responsible for the chemotherapy, the PDT 18 and the PTT, respectively. The addition on an MSN coating was able to improve both 19 the photostability and the loading capacity of the GNR. The as-synthesized 20 GNR@SiO₂-5-FU-ICGrealized a trimodal synergistic therapy of PDT, PTT and 21 chemotherapy under multimodal imaging guidance. Quantitative tumor growth 22 inhibition ratio in nude mice treated by GNR@SiO2-5-FU-ICG under laser irradiation 23 was 100%, while those treated with GNR@SiO2-5-FU under laser and 24 GNR@SiO₂-NH₂ were 88.27% and 69.43%, respectively (saline groups were 25 regarded as 0%) (Figure 3). The nanoplatform was able to completely eradicate tumor 26 without recurrence, demonstrating the superiority of the combination therapy. Wen 27 and coworkers (Xiao et al., 2019) also designed a trimodal nanoplatform (250 nm) by 28 introducing tellurium nanodots (Te NDs) into MSNs through in situ formation and 29 then loading the system with paclitaxel (PTX). Here, the Te NDs work as both PS and 30 PA concurrently, producing ROS and heat under NIR irradiation. When the 31 concentration of PTX was 80 µM, MTT assay showed that HepG2 cells treated with 32 MT@L-PTX@FA under irradiation had the lowest cell viability (~25%), significantly 33 out performing MT@L with irradiation (~45%), MT@L-PTX@FA without 34 irradiation (~40%), and free PTX (~45%). The results prove that this synergistic 35 approach was able to enhance therapeutic outcomes.



3	treatments at different time points upon 808 nm laser irradiation 24 h postinjection. b)
4	Temperature changes in the tumor region of the A375 tumor-bearing mice treated
-	
5	with saline, 5-FU, free ICG-NHS, GNR@SiO ₂ -NH ₂ , GNR@SiO ₂ -ICG, and
6	<u>GNR@SiO₂-5-FU-ICG</u> , which irradiated at 24 h postinjection (808 nm, 1.0 W cm $^{-2}$, 5
7	min). c) Tumor growth of mice received different treatments, d) Tumor weights of
8	nude mice on day 21 after different treatments (Fang et al., 2017b), Copyright 2017,
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MSN-based nanoplatform	Combination therapy	Therapy agent	Chemotherapy drug	Synergistic effect	
BMHDC	PDT	Ce6 PS		Combination index (CI) of 0.21	(Fang et al., 2019)
MSN-Au-PEG		Au NPs	DOX	Cell viability of MSN-Au-PEG group ranged from 73.49% to 12.1%, lower than that of the non-illuminated group and even lower than that of free DOX group.	(Guo et al., 2020)
DOX@MSN-NH2		rGO		Cell death rate: DOX@MSN@rGO-FA with NIR (PTT + chemotherapy): 68%; MSN@rGO-FA with NIR irradiation (PTT alone): 52%; DOX@MSN@rGO-FA without NIR (chemotherapy alone): 33.4%.	(Wang et al., 2015)
rGO@Porous Silica nanocookie	PTT PS		СТР	Cell death rate: Nanocookie-CPT with NIR (PTT + chemotherapy): 90%; CPT-free nanocookie with NIR (PTT alone): 60%; nanocookie-CPT without NIR (chemotherapy alone): 20%.	(Chen et al., 2014)
FMSN@BP-DOX-FA		BPQDs	DOX 9	Cell death rate: FMSN@BP-DOX-FA with NIR: 73.5%; FMSN@BP-DOX-FA without NIR: 64.78%; FMSN@BP-FA with	(Qiu et al.,

Table 1. MSN-based nanoplatforms for Chemotherapy-phototherapy and their synergistic effects

GNR@SiO2-5-FU-ICG	PDT&PTT	PS PA	ICG GNR	5-FU	 Tumor growth inhibition ratio: GNR@SiO₂-5-FU-ICG under laser (PTT + PDT + chemotherapy): 100%; GNR@SiO₂-ICG under laser (PTT + PDT): 88.27%; GNR@SiO₂-NH₂ under laser (PTT alone): 69.43%; ICG-NHS under laser (PDT alone): 38.14%; 5-FU under laser (chemotherapy alone): 15.90%. 	(Fang et al., 2017a)
MT@L-PTX@FA		PS PA	Te NDs	PTX	Cell viability: MT@L-PTX@FA with irradiation: ~25%; MT@L with irradiation: ~45%; MT@L-PTX@FA without irradiation: ~40%; free PTX: ~45%.	(Xiao et al., 2019)

NIR: 10%.

2018b)

1 **3** Chemotherapy and gene therapy

2 Traditional cancer therapies focus on killing cancer cells directly, which can achieve short-term effects but has little effect on drug resistance or metastasis and so does little to prevent tumor relapse. The occurrence of cancer is closely related to gene structure and function changes, 3 4 which provides us with another strategy, gene therapy. With the sequencing of human genome, gene therapy has made noteworthy progress in the past few decades. In particular, the combination of gene therapy and chemotherapy has been widely studied and has been proven to enhance 5 therapeutic efficiency and reduce side effects, achieving a synergistic effect in cancer treatment (Shen et al., 2014). While promising, a crucial 6 step for this combination therapy is the development of suitable carriers for the precise delivery and controlled release of gene therapy agents 7 8 such as plasmids, DNA, small interfering RNA (siRNA), micro RNA (miRNA), and short-hairpin RNA (shRNA). MSNs are easily functionalized with positively charged polymers to enable electrostatic interactions with nucleic acid and their cavities are able to load 9 10 chemotherapeutic drugs effectively. As such, they are an extremely promising carrier for gene/drug codelivery (Table. 2)

1 p53 is a tumor suppressor gene, the disfunction of which has been found to have 2 the highest correlation with human tumors, making it an ideal target for combination 3 chemo-gene therapy. Lin et al. (Lin et al., 2017) conjugated chitosan with poly 4 (amidoamine) (PAMAM), which can adsorb the p53 plasmid and then modified the 5 chitosan derivatives onto the surface of MSNs to be the gatekeeper of DOX loaded 6 into the pores (average diameter 2.3 nm) by a redox-responsive disulfide bond. The 7 size of the nanosystem was about 100 nm, which is suitable for cell uptake. The 8 nanocarrier proved to have excellent DOX/p53 codelivery ability and showed a 9 satisfactory transfection efficiency (27.6%), very close to PEI -25k (29.8%) in vitro. 10 Importantly, the drug/gene dual delivery nanosystem showed a better inhibition for 11 Hela cell (36% cell viability) than the drug (51%) or gene (75%) used alone, 12 exhibiting the synergistic effect of chemotherapy and gene therapy. Zhang et al. 13 (Zhang et al., 2017) also constructed a redox-responsive silica-based nanosystem 14 which enable codelivery of DOX and p53. The primary difference being that the 15 disulfide bond was directly inserted into the silica backbone and covalently linked to DOX by the one pot method, allowing the nanosystem to achieve 16 17 redox-responsiveness, controlled release, and self-degradation. Recently, a smart drug/gene nanocarrier was developed by Zhou et al. (Zhou et al., 2020), which 18 19 utilized UV crosslinked/pH de-crosslinked coumarin as the gatekeeper of MSNs 20 loaded with the chemotherapy drug 5-FU and p53 carried by cationic 21 poly(glycidylmethacrylate)-b-poly(2-(dimethylamino)ethylmethacrylate)

(PGMA-b-PDMAEMA). In addition to achieving a synergistic effect of chemotherapy and gene therapy (21.33% apoptosis rate of cancer cells, compared to 14.32% for 5-Fu and 9.41% for p53 monotherapies), coumarins can also emit blue fluorescence, enabling the nanocarrier to function as a fluorescent probe to detect trace drugs concentrations.

27 In addition to p53 which is associated with most cancers, there are also genes 28 associated with specific cancers. Hepatocyte nuclear factor 4α (HNF4 α) is an 29 important transcription protein that regulates the differentiation of hepatocytes and 30 maintains the biological function of hepatocytes. Based on this, Tsai et al. (Tsai et al., 31 2019) investigated an approach to deliver the gene encoding HNF4 α and the 32 chemotherapeutic drug cisplatin to hepatocellular carcinoma (HCC), via 33 polyethyleneimine-modified MSNs (PMSNs). After treatment with PMSN/HNF4a 34 plasmid DNA/cisplatin, HNF4a in Huh7 cells was over expressed and resulted in the 35 proportion of CD133 enriched cells decreasing significantly.

Since Fire and coworkers (Andrew Fire, 1998) first proposed RNA interference (RNAi) technology its application in cancer therapy has grown rapidly. RNAi molecules include siRNA, shRNA and miRNA, of which siRNA have been studied most. siRNA is a type of chemically synthesized double-stranded RNA. It is

1 transported into cells and then incorporated into the RNA-induced silencing complex 2 (RISC), a protein-RNA complex which separates the strands of the RNA and discards 3 the sense strand. The anti-sense strand then guides RISC to cut the target messenger 4 RNA (mRNA), resulting in hindrance of the production of its encoded protein (Deng 5 et al., 2014). Researchers have used mesoporous silica-based multifunctional carriers 6 to deliver DOX and Bcl-2 siRNA to treat a variety of cancers (Zhou et al., 2016;Zhao 7 et al., 2017;Lee et al., 2018;Pan et al., 2018). For example, Pan et al (Pan et al., 2018) 8 developed a smart nanoplatform based on DOX loaded mesoporous silica as core and 9 Bcl-2 siRNA loaded zeolitic imidazole framework-8 (ZIF-8) as its shell, in which ZIF-8 acted as the gatekeeper of DOX with its pH sensitivity controlling the release of 10 11 DOX and siRNA. Flow cytometry analysis demonstrated that the apoptosis rate of 12 MDR cells reached 88.2% after incubation with Dox-MSN-COOH@ZIF-8/Bcl-2 13 siRNA but was only 36.3% without Bcl-2 siRNA.

14 Survivin, which is highly expressed in many types of human tumors, is a 15 member of the inhibitor of apoptosis protein (IAP) family. Dilnawaz et al. (Dilnawaz 16 and Sahoo, 2018) demonstrated that the combination of the chemotherapeutic drug 17 (etoposide or docetaxel) or the proteasome inhibitor carfilzomib with survivin siRNA 18 could induce a 12.4% or 14.6% increase in apoptosis, respectively, in A549 cells. 19 Considering that the overexpression of multidrug resistance protein 1 (MRP1) is 20 significantly related to the clinical drug resistance of many kinds of tumors, Song et al. 21 (Song et al., 2020) loaded MRP-1 siRNA and myricetin into MSNs and modified the 22 nanoparticles with folic acid to target lung cancer cells. In vitro experiments showed 23 that Myr-MRP-1/MSN-FA can significantly inhibit the proliferation of cancer cells 24 and in vivo experiments further verified this therapeutic effect, in which the tumor 25 volume of mice treated with Myr-MRP-1/MSN-FA decreased the most.

26 As precursors of siRNA, shRNA are often co-transported by MSNs-based 27 carriers along with chemotherapeutic drugs to enhance their therapeutic effects 28 against cancer (Li et al., 2016). Most notably, this approach is taken when reversing 29 MDR (Chen et al., 2016b; Wu et al., 2018). An interesting nanovehicle was developed 30 by Wu et al. (Wu et al., 2018), in which they loaded the DOX prodrug with 31 nitrobenzyl into the pores of MSNs, then covalently linked MSNs to cationic 32 poly[2-(N,N-dimethylaminoethyl)-methacrylate] (PDMAEMA) modified by light 33 sensitive coumarin. P-gp shRNA was then electrostatically adsorbed unto the particle 34 surface and could be released upon activation by 405 nm light. After which, the 35 release of DOX could be triggered by exposure to 365 nm light. In this study, the 36 sequential release of gene agent and drug can be activated in a controllable manner 37 via external illumination and this sequential release greatly increased the 38 accumulation of drugs in the tumor sites, reversed MDR and improved overall 39 therapeutic effect.

1 miRNA is a type of endogenous short RNA molecule, which can be used to 2 regulate the cleavage of target mRNA post-transcriptionally or inhibit its translation 3 (Bartel, 2004). miRNA approaches and anti-miRNA approaches have been applied in 4 cancer therapies, the effectiveness of these methods mostly associated with the 5 efficacy of gene vectors. Liu et al. (Liu et al., 2018) developed a smart silica-based 6 nanosystem with high efficiency loading, stimulation responsivity, active targeting, 7 and biocompatibility. Their MSNs system (Figure 4) was composed of PEI covalently 8 linked inside the silica cavity via disulfide bond, then electrostatically bound to 9 miRNA-145. Meanwhile acting as the gatekeeper of DOX a WL8-PEG shell is coated 10 on the outside of the MSNs, improving the stability and targeting to SW480 cells of 11 the combination therapy. The nanosystem showed a remarkable antitumor effect both 12 in in vivo and in vitro experiments, with an especially excellent antimetastatic effect 13 in an orthotopic colorectal tumor model. The expression of miR211 is upregulated in 14 many kinds of tumors, especially in gliomas; conversely, the downregulation of 15 miR211 can make glioma cells sensitive to temozolomide (TMZ). Working off this, Bertucci et al. (Bertucci et al., 2015) used MSNs incorporated with Cy5 to transport 16 17 TMZ and anti-miR221/polyarginine-peptide nucleic acid (R8-PNA221) complex to 18 drug-resistant glioma cells. In accelerated survival experiment, MSNs with TMZ and 19 anti-miR211 synergistically decreased the C6 glioma cells survival rate more than the 20 sum of the MSNs-TMZ and MSNs-PNA221. The same trend was observed in their 21 apoptosis experiment. Several studies have indicated that anti-miRNA therapy 22 combined with chemotherapy is a potential strategy for reversing MDR. In order to 23 improve the sensitivity of glioma cells to TMZ, Nie et al. (Cunpeng Nie, 2020) used 24 93.5±6.7 nm Mn-doped MSNs to deliver TMZ and10-23 DNAzyme. In acidic and 25 reductive environments the Mn-MSNs decompose, enabling Mn²⁺ to assist 10-23 DNAzyme in silencing the O6-methylguanine-DNA methyltransferase (MGMT) gene. 26 27 Western blot experiments demonstrated the gene silencing effect of 28 Mn-MSNs/TMZ/10-23 DNAzyme and a significant decrease in IC₅₀ (>3.8-fold) 29 validated that the MDR T98G cells became more sensitive to TMZ after chemo-gene 30 combination therapy.



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MSN-based nanoplatform	Gene	Chemotherapy drug	Synergistic effect	Ref
MSN-SS-CP		DOX	Treated with p53, DOX, p53/DOX, HELA cells apoptosis rate: 15.5%, 22.6%, 42.1%	(Lin et al., 2017)
DS-DOX-PEGA	p53		Treated with p53, DOX, p53/DOX, relative tumor volume: 6.0, 4.5, 1.9	(Zhang et al., 2017)
MSN-g-PCAAMC-b-PDMAEMA		5-FU	Treated with p53, 5-FU, 5-FU/p53, MCF-7 cells apoptosis rate: 9.41%, 14.32%, 21.33%	(Zhou et al., 2020)
PMSNs	HNF4α- encoding plasmid	Cisplatin	Treated with HNF4α/cis, the growth of Huh7 cells was about 6, 3 folds decreased than HNF4α, cis singly	(Tsai et al., 2019)

Table 2. MSN-based nanoplatforms for Chemotherapy-gene therapy and their synergistic effects

DPSN			Treated by siRNA, DOX, siRNA/DOX, HELA cells viability: 33.5%, 39.4%, 16.6%	(Lee et al., 2018)
MSN-COOH@ZIF-8			Treated by DOX, siRNA/DOX, MCF-7/ADR cells apoptosis: 36.3%, 88.2%	(Pan et al., 2018)
MSNs-SS-siRNA@DOX	Bcl-2 siRNA	DOX	Treated with DOX, siRNA/DOX, tumor growth inhibition: 85.2%, 96.4%	(Zhao et al., 2017)
MSNs-PPPFA			Treated with DOX, siRNA/DOX, MDA-MB-231 cells apoptotic rate: 22.51%, 36.88%	(Zhou et al., 2016)
MSNs	Survivin siRNA	ETO/DOC+CAR	Treated with DOC+CAR, IC ₅₀ in A549 cell: 1.66, 0.85	(Dilnawaz and Sahoo, 2018)
MSN-FA	MRP-1 siRNA	Myricetin	Treated with Myr/siRNA, tumor weight was about 1/4 of treated with Myr	(Song et al., 2020)

<u>CP-MSNP@DOX/siRNA</u>	<u>PKM2 siRNA</u>	DOX	Compared to monotherapy, combination therapy resulted in an almost 3-fold decrease in the tumor weight	(Shen et al., 2017)	_
<u>MSNs@MONs</u>	<u>p-gp siRNA</u>	DOX	<u>Treated with DOX,</u> <u>H-MSNs-DOX,</u> <u>H-MSNs-DOX/siRNA,</u> inhibition rate of tumor growth: <u>50.7%, 76.8%, 87%</u>	(Sun et al., 2017)	
<u>MSNCs</u>	<u>T-type Ca²⁺channel siRNA</u>	DOX	<u>Treated with pMSNC/siRNA,</u> pMSNC/DOX , pMSNC/DOX/siRNA, inhibition rate of tumor growth: 47%, 45.5%, 76%	(Wang et al., 2019a)	带格式的: 上标
MSN-SS-PEI	shABCG2	DOX	Treated with DOX, DOX/ shRNA, CSC ratio: 1/2368, 1/57193	(Chen et al., 2016b)	带格式表格
МСР	P-gp shRNA	DOC	Treated with DOC/shNC, DOC/shRNA, HepG2/ADR	(Wu et al., 2018)	
		17			

			cells apoptotic rate: 28.05%, 62.93%	
Dm@TMSN	miRNA-145	DOX	Treated with DOX, miRNA, DOX/miRNA, tumor weight: about 140, 100, 30 mg	(Liu et al., 2018)
MSNPs	miR211	TMZ	Treated with TMZ, miRNA, TMZ/miRNA, T98G cells apoptotic rate: 49.1%, 36.88%, 70.86%	(Bertucci et al., 2015)

1 4 Chemotherapy and immunotherapy

2 Immunotherapy, utilizing the body's natural immune system to inhibit tumor, is 3 also a potential treatment option for combination with chemotherapy. The immune 4 system has the dual role of inhibiting and promoting tumor growth (Schreiber et al., 5 2011) and immune checkpoint therapy has become a research hotspot of cancer 6 therapy in recent days (Dyck and Mills, 2017). Compared to other treatment modes, 7 immunotherapy can more specifically target the primary tumor and secondary tumor 8 metastasis, it can also prolong anti-tumor response through immune memory cells to 9 inhibit tumor recurrence (Luo et al., 2017). However, immunotherapy has a low 10 response rate, making it ineffective for some patients (Zheng et al., 2020). 11 Considering the limitations of chemotherapy alone as well as immunotherapy alone 12 mentioned above, the idea of combining chemotherapy and immunotherapy came into 13 being naturally, Though chemotherapeutic agents can induce immunogenic cells death 14 (ICD) (Kroemer et al., 2013), most chemotherapies would induce lymphopaenia, 15 which hampers the anticancer immune response (ACIR) (Lake and Robinson, 2005), 16 making the combination of chemotherapy and immunotherapy difficult to realize. 17 Zheng's group has broken the barrier between the two therapies by designing 18 DOX@HIMSNs, a DOX-loaded and MSN-based nanoplatform (Zheng et al., 2016). 19 The tumor volume in 4T1 tumor bearing Balb/c mice of DOX@HIMSN group was 5 20 times smaller than that of DOX group. And the fluorescent overlap between 21 granzyme-B and caspase-3 of DOX@HIMSN group had a Mander overlap coefficient 22 of 0.95, which was higher than the DOX group (0.88), indicating the enhanced 23 immunological cells killing ability of DOX@HIMSN. These results showed that the 24 highly integrated MSNs can increase tumor cell cytotoxicity as well as stimulate 25 ACIR, indicating the potential of MSN-based nanosystems in immunotherapy 26 combined chemotherapy. There is increasing efforts to combine the two modalities 27 together into an MSN-based nanoplatform to achieve an enhanced therapeutic effect 28 (Choi et al., 2019). Kong(Kong M, 2017) and coworkers developed a 29 HMSN-mediated nanosystem called A/D/I-dHMLB to co-delivery DOX, all-trans 30 retinoic acid (ATRA) and interleukin-2 (IL-2) for chemo-immunotherapy. 31 A/D/I-dHMLB had a higher tumor inhibitory rate of 84.8 ±13.0% compared to DOX 32 group of $17.1 \pm 12.4\%$. After the treatment of A/D/I-dHMLB, the number of 33 myeloid-derived suppressor cells (MDSC), which impede ICD, showed a 2.7-fold 34 decrease, while the number of mature DC and activated CD8⁺ T cell increased 35 14.3-fold and 3.93-fold, respectively. Other cytokines like IL-12p70 and TNF- a also 36 increased while inhibitory cytokines like IL-10 and TGF- β decreased. All the results 37 indicated that the design of A/D/I-dHMLB can effectively kill cancer cells and reach 38 an enhanced antitumor immunity. Dong et al. (Dong et al., 2017) developed a 39 pathogen-mimicking nanocomplex (MSN-SP-LPS) with a mean hydrodynamic

40 diameter of 167.1±3.9 nm by conjugating the sodium phthalate salt of the parent LPS

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to MSN. The amount of TNF-a detected in RAW 264.7 cells treated with 1 2 MSN-SP-LPS (~ 5.5×10^3 pg/mL) or SP-LPS (~ 5.6×10^3 pg/mL) was higher than that 3 released by MSN (~ 0.3×10^3 pg/mL) due to the presence of LPS, indicating a stronger activation of macrophages. In addition, the high amount of INF- γ secretion 4 5 (900 pg/ml) provided the evidence of T cell activation, showing a strong 6 inflammation response by MSN-SP-LPS. When treated with 1.25 µg SP-LPS/mL and 7 0.5 µg DOX/mL, the cell viability of splenocytes treated with MSN-DOX-SP-LPS 8 combination was the lowest (~72%), compared to ~74% for MSN-DOX and ~95% for 9 SP-LPS, indicating the superiority of the synergistic effect of immuno-chemotherapy.

10 5 Chemotherapy and sonodynamic therapy

11 Sonodynamic therapy (SDT), another non-invasive therapeutic modality, has 12 shown specific advantages in cancer therapy when compared to its counterparts like 13 PDT or PTT, since SDT can reach deeper tumor sites due to the high tissue 14 penetrating nature of ultrasound (US) waves (Qian et al., 2016). SDT can kill cancer 15 cells by producing cytotoxic ROS through the combination of US with a 16 sonosensitizer, while minimizing damage to the surrounding normal cells (Chen et al., 17 2016a). Sonosensitizers include organic materials such as porphyrins (Hachimine et 18 al., 2007; Yumita et al., 2010), erythrosine B (EB) (Yumita et al., 2002) and Rose 19 Bengal (RB) (Sugita et al., 2015), as well as inorganic materials like titanium dioxide 20 (TiO2) (Harada et al., 2011) and silicon nanoparticles (Osminkina et al., 2015). 21 Interesting, MSNs have been shown to have impressive SDT activity due to their high 22 porosities, which allow the free diffusion of molecules to generate ROS.

23 Since MSNs can simultaneously play the role of sonosensitizer and drug carrier, 24 there is exciting potential for a synergistic nanoplatform integrating SDT and 25 chemotherapy. While promising, SDT monotherapy still has some limitations such as 26 lacking tumor-targeting ability, hypersensitivity to light (Lafond et al., 2019), tumor 27 hypoxia (Zhao et al., 2020) and insufficient lethality to kill all cancer cells. The US 28 used in SDT promotes drug release in chemotherapy (Ding et al., 2017), while the 29 chemotherapy could compensate for the weaknesses of sonodynamic monotherapy, 30 creating the ideal synergistic environment. Ding (Ding et al., 2017) et al. reported a 50 31 nm core-shell MSN-based nanocomplex with DOX loading and targeting group 32 methacrylated hyaluronic acid (m-HA) gel functionalization to realize a synergistic 33 therapy combining chemotherapy and SDT. The surviving percent of cells treated by 34 DOX@MSN-HA under US was only about 5% compared to that of DOX@MSN-HA 35 (35%) and MSN under US (70%), highlighting the synergistic potential of SDT and 36 chemotherapy.

37 6 Chemotherapy and magnetic hyperthermia therapy

1 Recently, magnetic hyperthermia therapy has been proven to be effective tool in 2 the struggle against cancer. Magnetic hyperthermia utilizes the heat from the energy 3 dissipation of magnetic particles to cause the irreversible necrosis of cancer cells, 4 while leaving normal tissues undamaged (Kobayashi, 2011;Brollo et al., 2016). 5 Additionally, magnetic hyperthermia has been shown to accelerate the release of the 6 anticancer drug DOX from nanoplatforms, making it a potential partner to improve 7 the efficacy of chemotherapy (Tian et al., 2018). In return, chemotherapy as a 8 whole-body treatment can make up the limitation of magnetic hyperthermia therapy 9 as a treatment only for local oncology. Therefore, combining chemotherapy with magnetocaloric therapy is a promising method to inhibit tumor growth and many 10 11 MSN-based systems have been reported to make this a reality.

12 2018) developed Tian (Tian et al., and coworkers 13 poly(N-isopropylacrylamide-co-methacrylic acid) (P(NIPAM-co-MAA)) coated 14 magnetic mesoporous silica nanoparticles (MMSNs) with particle size 255±28 nm 15 and pore size 2.6 nm to achieve a combination chemo-magnetic therapy. Under 16 exposure to an alternating magnetic field (AMF) at a frequency of 409 kHz and 17 magnetic field strength of 180 Gauss, the MMSNs generated enough heat to raise the 18 cell temperature to $64.2 \,^{\circ}{\rm C}$ within 15 min, inducing both hyperthermia and the 19 controlled release of loaded DOX. A CCK-8 assay showed that the cell viability of 20 Hela cells after treatment with the synthesized DOX-MMSN@P (NIPAM-co-MAA) 21 nanoparticles decreased to only 23%, which was significantly lower than that of cells 22 after treatment with DOX (76%) or AMF (42%) alone. This shows the strong 23 synergistic therapeutic effect of chemo-magnetic hyperthermia therapy and provides a 24 promising platform for combined chemotherapy.

25 Iron nanomaterials are used as magnetic therapeutics in many MSN-based synergistic systems due to their strong response to AMFs (Zhu and Tao, 26 27 2015; Guisasola et al., 2018). Cai et al. (Cai et al., 2019) successfully synthesized 28 CSiFePNs (220 nm) by loading superparamagnetic ferroferric oxide and Paclitaxel 29 (PTX) into MSNs coated with MDA-MB-231 cell membranes. The combination 30 system showed the highest anticancer ability (IC₅₀ value of 0.8 μ gL⁻¹) compared to CSiFeNs with AMF (IC₅₀ value of 3.6 µgL⁻¹) or CSiFePNs without AMF (>0.8 31 32 $\mu g L^{-1}$), further demonstrating that the combination of magnetotherapy and 33 chemotherapy possesses great potential for the treatment of carcinomas.

34 7 Chemotherapy, chemodynamic therapy, and starvation therapy

35 Chemodynamic therapy (CDT) is a novel modality to treat tumors by using 36 transition metals to convert local hydrogen peroxide (H_2O_2) into highly toxic 37 hydroxyl radicals (•OH) to kill cancer cells (Huo et al., 2017). Because CDT responds 38 to the acidic and hydrogen peroxide rich microenvironment of tumors, it is highly

1 selective. However, there are still challenges to face in CDT such as insufficient

2 intratumor H_2O_2 , inadequate H^+ , as well as the unsatisfactory catalytic capacity of 3 chemodynamic agents (Cheng et al., 2020a;Wang et al., 2020b). As a local treatment

4 modal, CDT could be a supplement to chemotherapy to enhance overall therapeutic

5 efficacy. Combinations of chemotherapy and CDT with MSNs as the DDS have

6 reported strong potential in anticancer treatment (Kankala et al., 2017;Zhang et al.,

7 2020a).

Another oncotherapy strategy, starvation therapy, also responds to the tumor 8 9 microenvironment, is a superb strategy to treat cancer, and may address the 10 shortcomings of CDT (Hao et al., 2019). In contrast to normal cells, the glycolysis of 11 cancer cells is upregulated even in an oxygen-sufficient situation (Warburg et al., 12 1927). Starvation therapy attempts to exploit this by utilizing glucose oxidase (GOx) 13 to cut off nutrients to cancer cells, starving them to death. Several synergistic 14 MSN-based nanoplatforms integrating chemo and starvation therapy have been 15 reported (Cheng et al., 2019a;Zhang et al., 2020b). As discussed above, CDT is 16 limited by the concentrations of H₂O₂ and H⁺. Starvation therapy produces excess 17 H₂O₂ and causes a decrease in pH, making it a perfect pair for CDT. Furthermore, 18 starvation therapy itself is not enough for completely eliminate cancer cells, 19 necessitating combination with additional treatment modalities to achieve the desired 20 therapeutic effect (Fu et al., 2018). As both CDT and starvation therapy have been 21 successfully integrated with chemotherapy and GOx-triggered starvation therapy can 22 induce sequential CDT and chemotherapy, it is possible to construct an all-in-one 23 system featuring tri-modal therapy.

In one such example, starvation therapy and chemodynamic therapy were 24 25 reported to combine with chemotherapy in a single nanosystem designed by Cheng (Cheng et al., 2020a) and coworkers. Hypoxic prodrug tirapazamine (TPZ) and high 26 27 efficiency catalyst Fe₃O₄ were loaded into MSNs and the MSNs surface 28 functionalized with GOx. The drug loading rate of TPZ and GOx achieved by the 29 authors were 14.9% and 5.8%, respectively and the hydrodynamic diameter size of 30 Fe₃O₄@MSN was 88 nm. When GOx consumes the oxygen and glucose in the tumor 31 microenvironment, it causes increased endogenous H2O2, decreased acidity, and more 32 extreme hypoxia. Then, through the iron ion-mediated Fenton reaction (Lafond et al., 33 2019) using the Fe₃O₄ catalyst, H₂O₂ is transformed into cytotoxic •OH and induces 34 chemodynamic therapy. The hypoxia then activates the hypoxia-responsive TPZ, to 35 kill cancer cells while avoiding healthy cells (Figure 5). Under hypoxic conditions, 36 MTT assays showed that the cell viability of MCF-7 cells after treatment with 37 TPZ/Fe₃O₄@MSN-GOX was 8.6%, while that of the TPZ/Fe₃O₄@MSN group was 38 29.9% and the TPZ group was 33.3%, indicating the as-synthesized 39 TPZ/Fe₃O₄@MSN-GOX displayed excellent tumor inhibition, with the GOx-induced





4 Figure 5. (a) Cell viability rates of different MSN concentrations at different oxygen 5 concentrations. (b) L-02 cell viability rates of different TPZ dose-dependent concentrations of different nanoparticles in 20% O2 concentration with glucose (1 mg 6 7 mL⁻¹). (c) MCF-7 cell viability rates of different TPZ dose-dependent concentrations 8 of different nanoparticles in 5% O₂ concentration. (d) MCF-7 cell viability rates of 9 different TPZ dose-dependent concentrations of different nanoparticles in 5% O2 10 concentration, which was treated by different nanoparticles calculated by the MTT 11 assay(Cheng et al., 2020a), Copyright 2020, RSC

12 **Cross-modal chemo-combination therapies** 8

13 The development of multifunctional nanocarriers has enabled the development of 14 chemotherapeutic combination therapies that include more than one other synergistic 15 modality. In order to reverse multidrug resistance, Yang et al. (Hong Yang, 2017) 16 assembled sodium alginate/chitosan polyelectrolyte multilayers onto Fe₃O₄/Au/MSNs 17 loaded with DOX and photosensitizer Ce6 to adsorb P-gp shRNA. After incubation

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with the nanoparticles and laser irradiation, the survival rate of drug-resistant cells
 MCF-7/ADR was inhibited by >60% compared with any monotherapy.
 Demonstrating that chemo-gene-photodynamic therapy had a synergistic anti-tumor
 effect and the ability to reverse MDR. Additionally, Fe₃O₄/Au endowed the
 nanoparticles with dual imaging modes of magnetic resonance and CT imaging,
 enabling real-time guided therapy.

7 Gold nanotriangles are excellent radiation/PTT therapeutic agents but possess 8 high toxicity and poor drug loading capacity (S. R. Bhattaraia). To overcome these 9 limitations, a kind of "Hedgehog like" Janus gold triangle-MSNs were developed by 10 Wang and co-works to deliver the hypoxia-activated prodrug TPZ, with surface functionalized FA-PEG to improve targeting and biocompatibility (Wang et al., 11 12 2019c). In vivo and in vitro experimentation revealed that FA-GT-MSNs@TPZ 13 nanoplatforms showed superior anti-tumor effects to monotherapies alone, 14 demonstrating that hypoxia-activated radio-chemo-photothermal therapy is a very 15 promising strategy for cancer treatment.

16 Lu et al. (Lu et al., 2020) prepared mesoporous silica nanorods of a specific width 17 (100 nm) and precisely controlled aspect ratio (AR: length/width). They loaded DOX 18 and GOx with AR6 into MSNs, then coated the nanoparticles with an a polydopamine 19 (PDA) layer to absorb Siramesine, a drug that can damage lysosomes and induce 20 apoptosis. The multifunctional nanoplatform integrated chemotherapy, PTT, CDT and ST, and targeted cancer cells with FA, exhibit in a much higher lethality to cancer 21 cells than any single therapy. These studies highlight the potential for MSN 22 23 chemotherapy combinations to go beyond a two pronged assault on cancer and 24 incorporate a whole host of therapeutic modalities.

25 9 Conclusions and outlook

26 As a standard therapy modality for cancer treatment, chemotherapy urgently 27 needs a more targeted drug accumulation in tumor sites and strategies to overcome 28 MDR in order to improve its practical application in the clinic. Recently, 29 chemotherapy-based combination therapies have become an irresistible trend due to 30 the superiority in therapeutic efficacy compared to monotherapies. MSNs with large 31 pore sizes, diverse functionality, ease of modification and good biocompatibility are 32 ideal materials to realize such synergistic nanoplatforms, since they can not only serve 33 as drug carriers but also function as therapeutic agents in therapies complementary to 34 chemotherapy. In this review, we have discussed many MSN-based nanosystems 35 featuring the integration of chemotherapy with other therapy modals namely 36 immunotherapy, gene therapy, phototherapy, magnetic hyperthermia therapy and 37 sonodynamic therapy and emphasized the effects of dual- or multi-modal therapy. As 38 expected, most of the reported cases demonstrate that MSN mediated combination

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therapy achieved at least 1+1>1 effect in cellular or animal level, providing 1 2 experimental evidence for further promising applications of these MSN-based 3 delivery systems. Naturally, there is no objectively best combination, as each 4 combination has its advantages and disadvantages. However, the chemo-immuno 5 combination therapy may have the most promising future for further clinical 6 translation considering that immunotherapy using PD-1/PD-L1 antibodies, CTAL-4 7 antibodies and CAR-T treatment has been recently revealed as a powerful clinical 8 strategy for treating cancer.

9 Though MSN-based combination chemotherapies have shown preliminary 10 success in in vitro and in vivo testing, several challenges remain before these nanoparticles can put into clinical use. As highlighted in this review, nanocomposites 11 12 serve as the multimodal therapy platforms, necessitating long-term biosafety tests as 13 well as more detailed pharmacokinetic/pharmacodynamic analyses for each 14 participating component in the complexes. Additionally, the optimal dosing ratio 15 between chemotherapeutics and other therapeutic agents must be investigated further. 16 Furthermore, the integration of combination therapies should be strategic, that is, they should achieve interlocking effects and smart drug delivery and release systems to 17 18 maximize the synergistic benefits. Lastly, developing simpler syntheses of 19 MSN-based nanocomplexes is a high priority, as is improving their cancer targeting 20 capabilities.

The existing researches about MSN-based chemotherapy combination therapies are immature, however, as our understanding of materials and diseases deepens, potential applications of MSN-based DDS broaden. It is sure that chemotherapy-based nanosystems utilizing biocompatible MSNs have a bright adaptable future and great potential for clinical translation.

26 Conflict of Interest

27 The authors declare no conflict of interest.

28 Author Contributions

Writing—original draft preparation, Ying Gao and Dongruo Gao; writing—review and editing, Jie Shen and Qiwen Wang; funding acquisition, Jie Shen and Qiwen

31 Wang. All authors have read and agreed to the published version of the manuscript.

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