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# May the force be with you: The role of hyper-mechanostability of the bone sialoprotein binding protein during early stages of *Staphylococci* infections

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The bone sialoprotein-binding protein (Bbp) is a mechanoactive MSCRAMM protein expressed on the surface of *Staphylococcus aureus* that mediates adherence of the bacterium to fibrinogen- $\alpha$  (Fg $\alpha$ ), a component of the bone and dentine extracellular matrix of the host cell. Mechanoactive proteins like Bbp have key roles in several physiological and pathological processes. Particularly, the Bbp: Fg $\alpha$  interaction is important in the formation of biofilms, an important virulence factor of pathogenic bacteria. Here, we investigated the mechanostability of the Bbp: Fg $\alpha$  complex using *in silico* single-molecule force spectroscopy (SMFS), in an approach that combines results from all-atom and coarse-grained steered molecular dynamics (SMD) simulations. Our results show that Bbp is the most mechanostable MSCRAMM investigated thus far, reaching rupture forces beyond the 2 nN range in typical experimental SMFS pulling rates. Our results show that high force-loads, which are common during initial stages of bacterial infection, stabilize the interconnection between the protein's amino acids, making the protein more "rigid". Our data offer new insights that are crucial on the development of novel anti-adhesion strategies.

#### KEYWORDS

mechanobiology, Staphylococcus infection, biofilm, adhesins, molecular dynamics

# 1 Introduction

*Staphylococcus aureus* infections have a high clinical and communal impact with an estimated mortality rate that can reach 30.2% Bai et al. (2022). The persistence of these infections lies on the *Staphylococcus aureus*' ability to form biofilms Costerton et al. (1999); Archer et al. (2011); Suresh et al. (2019), and the eventual dissemination of these pathogenic bacteria throughout the body Kwiecinski and Horswill (2020). Despite the increase in sterilization and hygienic measures, modern medical devices play a key role in the transfer of these bacterial colonies through device-associated biofilm infections Wertheim et al. (2004); Otto (2009); Lister and Horswill (2014). The contamination of patients during medical and dental procedures is of increasing relevance, particularly with the emergence of drug-resistant bacteria. In the dental field, it has been estimated that the carrier prevalence of *S. aureus* in healthy adults varies from 24% to 84% Donkor and Kotey (2020). Additionally, the oral cavity is a source for cross infection and dissemination of the infection directly into the bloodstream, increasing the likelihood of septicemia and possibly death McCormack et al. (2015); Garbacz et al. (2021); Jevon et al. (2021).



Biofilms shelter the bacteria and enhance the persistence of infection by eluding innate and adaptive host defenses González et al. (2018); Versey et al. (2021). Biofilms also form a barrier, protecting colonies from biocides and antibiotic chemotherapies Sharma et al. (2019). Adhesins play critical roles during infection, especially during the early step of adhesion when bacterial cells are exposed to mechanical stress Latasa et al. (2006). Adhesins bind to their target ligands, holding it tight to them even at extreme force loadings that largely outperform classical binding forces Gomes P. S. F. C. et al. (2022). The resilience to mechanical forces provides the pathogen with a means to withstand high levels of mechanical stress during biofilm formation, thus yielding these pathogens highly resistant to breaking these cell adhesion bonds. These unusual stress-dependent molecular interactions play an integral role during bacterial colonization and dissemination and when studied, reveal critical information about pathosis Dufrêne and Viljoen (2020).

Among S. aureus adhesins, the bone sialoprotein binding protein (Bbp) is a bifunctional Microbial Surface Component Recognizing Adhesive Matrix Molecule (MSCRAMM) Gillaspy et al. (1998). Bbp is part of the MSCRAMM serine-aspartate repeat (Sdr) family that also includes SdrF and SdrG in Staphylococcus epidermidis, and clumping factor A (ClfA), B (ClfB), SdrC, and SdrE in S. aureus Josefsson et al. (1998); McDevitt et al. (1994); Ní Eidhin et al. (1998); Tung et al. (2000). Ligand-binding for Bbp occurs generally in the N-terminal region, from residues 273 to 598, where Bbp binds to fibrinogen- $\alpha$  (Fg $\alpha$ ), a glycopeptide on bone and dentine extracellular matrix (ECM). Bbp's binding region is subdivided into domains N2 and N3, which are made up of two layers of  $\beta$ -sheets with an open groove at the C-terminus where primary ligand binding occurs Zhang et al. (2015) (Figure 1B). The binding of Fg $\alpha$  follows a "dock, lock, and latch" mechanism O'Connell (2003); Ponnuraj et al. (2003); Bowden et al. (2008); Foster et al. (2014); Zhang et al. (2017), that has been previously investigated by a myriad of techniques Herman et al. (2014); Vanzieleghem et al. (2015); Vitry et al. (2017); Herman-Bausier et al. (2018); Milles et al. (2018). Thus, the pathogenic bacteria does not invade a host cell, but rather adheres to the ECM via Bbp: Fg $\alpha$  interactions Patti et al. (1994).

Using a combination of *in silico* and *in vitro* single-molecule force spectroscopy (SMFS), we have previously reported that *S. epidermidis*'

adhesin SdrG, when in complex with Fg $\beta$ , was able to withstand extreme mechanical loads Milles et al. (2018). The necessary force applied to rupture the SdrG: Fg $\beta$  complex was shown to be an order of magnitude stronger than that needed to rupture the widely employed Streptavidin: biotin complex Sedlak et al. (2018), and more than twice of that of cellulosomal cohesin:dockerin interactions Schoeler et al. (2014); Bernardi et al. (2019). Most biological complexes rupture at a relatively low force range Seppälä et al. (2017); Haataja et al. (2019); Hoelz et al. (2011; 2012); Mendes et al. (2012); Bernardi and Pascutti (2012), including other host-pathogen interactions Bauer et al. (2022). A molecular mechanism for a catch-bond behavior of the SdrG: Fg $\beta$ was then revealed by investigating the system in a "force-clamp" regime Melo et al. (2022), with magnetic tweezers based SMFS revealing that the SdrG: Fg $\beta$  bond can live for hours under force loads Huang et al. (2022). Here, taking advantage of a powerful in silico SMFS approach, we describe how Bbp plays a key role in bacterial adhesion during nosocomial infections, by investigating the Bbp:  $Fg\alpha$ complex at different pulling velocities combining all-atom (aa) and coarse-grained (CG) steered molecular dynamics (SMD) simulations (Figures 1A, B). Building on *in vitro* SMFS data, our results point to Bbp's interaction with the extracellular matrix fibrinopeptide as the most mechanostable so far investigated, independent of the loading rate. Our findings reveal that a few key interactions are responsible for the outstanding force resilience of the complex. Furthermore, our results offer insights into the development of anti-adhesion strategies.

## 2 Results

### 2.1 Bbp is highly mechanostable under stress

To probe the mechanics of the interaction between Bbp and Fg $\alpha$ , and to characterize the atomic details of the complex under force load, we performed aa-SMD simulations with Bbp anchored by its C-terminal while Fg $\alpha$  was pulled at different velocities (Supplementay Table S1). The simulations resulted in Force vs extension curves that reveal a clear one-step rupture event, as



#### FIGURE 2

Bbp mechanostability under high mechanical load. (A) Force *versus* extension curve as an exemplary trace, with rupture peak force at 3,510 pN. (B) Histogram for the most probable rupture force (blue, rugged plot in red) with the Bell-Evans (BE) model for the first rupture peak (red), based on the all-atom steered molecular dynamics simulation replicas with the slowest simulated pulling velocity (2.5×10<sup>-4</sup> nm/ps).



Dynamic Force spectrum for the Bbp: Fg $\alpha$  complex combining data from all-atom and coarse-grained SMD simulations. All-atom, and Coarse-grained steered molecular dynamics simulations (CG-SMD and aa-SMD) were performed at different velocities:  $2.5 \times 10^{-6}$  to  $2.5 \times 10^{-3}$  nm/ps (blue) and  $2.5 \times 10^{-4}$  to  $2.5 \times 10^{-3}$  nm/ps (green), respectively. A Dudko-Hummer-Szabo Dudko et al. (2006) (DHS) fit was performed through the SMD dataset predicting  $\Delta x = 7.489 \times 10^{-2}$  nm,  $k_{off}^0 = 2.596 \times 10^{-12} \text{ s}^{-1}$ ,  $\Delta G = 2.293 \times 10^2 \text{ k}_B T$ .

represented in Figure 2A. For the slowest pulling velocity, 160 replicas were performed following a wide-sampling paradigm previously developed in our group Sedlak et al. (2020). At the pulling velocity of  $2.5 \times 10^{-04}$  nm/ps, we observed that the most probable rupture force for the complex was 3,510 pN, as described by the Bell-Evans (BE) Bell (1978); Evans and Ritchie (1997) fit of the peak forces at that pulling speed (see Figure 2B). Our results reveal that Bbp: Fg $\alpha$  is the most mechanostable complex investigated thus far, which is in agreement with previous experimental data where we showed that SdrG: Fg $\beta$  complex can withstand forces on the 2 nN range, equivalent to breaking of covalent bonds Milles et al. (2018).

To investigate the dependence of the mechanostability of Bbp: Fg $\alpha$  on the force loading rate, we performed CG-SMD simulations at

several, much lower, pulling speeds (Supplementary Table S1). We have recently shown that aa-SMD and CG-SMD can be combined to in an *in silico* SMFS approach Gomes D. E. et al. (2022); Melo et al. (2022). Here, the combination of the two levels of molecular details is capable of rendering predictions that are consistent with theory and experimentation with the advantage of being 10 to approximately 100 times faster than aa-SMD simulations, depending on the pulling speed Gomes D. E. et al. (2022); Melo et al. (2022). A Dudko-Hummer-Szabo Dudko et al. (2006) (DHS) fit was performed through the SMD data, including both the aa-SMD, and the CG-SMD (see Figure 3). The DHS fit suggests that the system should rupture at forces higher than 2 nN at  $10^5$  pN/s force loading rate, in agreement with experimental data Milles et al. (2018). It is interesting

TABLE 1 Hydrogen bonds occupancy between Bbp and Fg $\alpha$  residues calculated and averaged before the main rupture event.

Bbp	Fgα	Occupancy (%)	Nature
Asp334	Thr565	54.84	Side-chain
Asp556	Lys562	45.39	Salt-bridge
Leu584	Thr565	36.14	Backbone
Thr582	Ser567	35.62	Backbone
Thr586	Gln563	35.03	Backbone:Side-chain
Ser333	Phe564	18.54	Side-chain
Asp588	Gln563	12.77	Side-chain
Thr587	Ser561	12.66	Side-chain

to note that the BE model is able to fit well all the simulation results, at both aa and CG level, as evidenced by the density plots in Figure 3.

The influence of the peptide size on the rupture force was also investigated. We have shown previously that SdrG complexed with shortened Fg $\beta$  peptides had lower unbinding forces Milles et al. (2018). Here, we simulated a model of Bbp complexed with Fg $\alpha$ elongated by nine residues (See Methods section) by an and CG-SMD simulations (Supplementary Table S1). Our results show that the force loading rate was not significantly impacted by the size of the peptide (Supplementary Figure S1), indicating that the original complex formed at the crystal structure has the minimal length to keep the important contacts with the protein latch to hold the DLL configuration.

# 2.2 Key hydrogen bonds are responsible for Bbp: Fg $\alpha$ high mechanostability

After confirming that Bbp:  $Fg\alpha$  complex presents a hyperstable interaction under shear mechanical load, we used the approximately 3  $\mu$ s of aa-SMD simulation data to investigate the molecular origin of the mechanostability of the complex. Previously, simulations of the SdrG: Fg $\beta$  revealed the presence of frequent and persistent hydrogen bonds (H-bonds) between the peptide and the protein backbone, showing that the high-force resilience of the complex was largely independent of the peptide side-chains interactions, and therefore the peptide's sequence Milles et al. (2018). Here, we computed the occupancy of the H-bonds between the Bbp and Fg $\alpha$  before the complex rupture. We identified the key amino acid interactions responsible for keeping the complex together at high force loads (Table 1). Different than SdrG: Fg $\beta$ , Bbp: Fg $\alpha$  interactions are not dominated by backbone-backbone interactions, with a significant amount of side-chain interaction of the peptide playing an important role in the complex mechanostability. The backbone interactions between Bbp  $^{\rm Leu584,\ Thr582,\ Thr586}$  and  $Fg\alpha^{\rm Thr565,Ser567,Thr586}$ have been previously described as important for  $Fg\alpha$  binding at the crystal structure Zhang et al. (2015). However, we noticed that the side-chain H-bonds are rearranged upon application of mechanical stress on the complex. On the crystal, Bbp<sup>Asp334</sup> forms a side-chain H-bond with  $Fg\alpha^{Ser566}$  , and during the SMD simulations, this interaction shifts to  $Fg\alpha^{Thr565}$ , being the H-bond with the highest occupancy over the trajectories. Another shift occurs between

Bbp<sup>Asp334,Ile335</sup> interacting with Fg $\alpha$ <sup>Phe564</sup>, on the crystal, to Bbp<sup>Ser333</sup> interacting with Fg $\alpha$ <sup>Phe564</sup> in our simulations. The H-bond between Bbp<sup>Asp588</sup> and Fg $\alpha$ <sup>Gln563</sup> is described as important to lock the peptide N-terminus and is still present before the rupture of the complex, although with lower occupancy. Instead, a charged side-chain interaction arises with significant occupancy values: Bbp<sup>Asp562</sup>. Fg $\alpha$ <sup>Lys562</sup>. These data corroborates the importance of backbone interactions to maintain the high mechanostability and also highlights important side chain H-bonds plasticity that occurs when Bbp: Fg $\alpha$  is exposed to mechanical stress.

# 2.3 The force propagates indirectly from the latch to the peptide

How a shear force load "activates" the hyperstability of the complex can be investigated by analysing the evolution of pairwise interactions during the force-loading event. Such analysis can be used to investigate how a catch-bond may be formed in the Bbp: Fg $\alpha$  complex Liu et al. (2020). Previously, it has been shown that SdrG: Fg $\beta$  presents a catch-bond behavior Huang et al. (2022), which is expected also for Bbp: Fg $\alpha$ . To analyse the pairwise interactions during the SMD, we employed the generalized correlation-based dynamical network analysis method Melo et al. (2020), which can also be used to calculate force propagation pathways Schoeler et al. (2015). Figure 4A shows the pairwise interactions obtained from the network analysis. The thickness of the connections between nodes (amino acid residues) represents how well correlated the motion of these nodes are, and therefore how well connected are these amino acid residues.

The force propagation pathway that connects the pulling and the anchoring residues shows that most of the force is propagating from the protein latch directly to the peptide, passing by the center of Bbp's N2 domain (Figure 4B). These results are slightly different than the ones obtained for the SdrG: Fg $\beta$  complex upon high mechanical stress Milles et al. (2018). However, in a previous study, it was observed that changes in the pulling velocities can lead to different force propagation pathways, suggesting different unbinding mechanisms at different pulling rates Melo et al. (2022).

The rigidity of the protein under high-force load can also be studied using the betweenness map from the dynamical network analysis (see Figure 4C). The betweenness is defined as the number of shortest paths from all vertices to all others that pass through that node, in this case, an amino acid residue. If an amino acid residue has high betweenness, it tends to be important for controlling interdomain communication within a protein Melo et al. (2020). High betweenness values (thicker red tubes) are seen on the latch that is in direct contact with Fg $\alpha$ , highlighting the strong correlation between the motif and the peptide. Interestingly, high betweenness is also found at connections intra N2 domain, pointing that Bbp: Fg $\alpha$  complex becomes more rigid under high force loads, particularly in the region interconnecting the latch, the peptide and the N2 domains. Such behavior helps the stabilization of the interactions under high forces.

A representation of the network in subgroups, or communities, is shown at Figure 4D. The communities group the amino acid residues that are most inter-connected in relation to the rest of the network. We can see that Bbp: Fg $\alpha$  is subdivided in a handful of communities. The latch, most of Fg $\alpha$ , and part of the N2 domains are united in the same community in light blue, showing that these amino acids are highly



#### FIGURE 4

Bbp:  $Fg\alpha$  dynamical network under high mechanical load. (A) Representation of the dynamical network. The thickness of the links between the nodes (amino acid residues) represents the correlation of motion between these residues. (B) The force propagates from the latch indirectly to the peptide, passing by the N2 domain of the protein. The color scheme of the complex is the same from Figure 1. The network's optimal path is colored in dark blue while the sub-optimal paths are colored in red. (C) Full dynamical network revealing the most correlated regions of the complex. The weight of the network edges (represented by the thickness of red tubes) is given by the betweenness values. (D) Generalized correlation-based communities represented by different colors of the nodes and edges in the network.



connected. We also measured the correlation between motions on the interface residues to determine how cooperative their motion is and the essential contacts that are keeping the complex stable under high mechanical load. Essentially, the higher the correlation between

residues, the more relevant is their interaction for the stability of the protein complex. We noticed that two Fg $\alpha$  residues are highly correlated (values equal or superior to 0.5) to Bbp at the interface, namely: Fg $\alpha$ <sup>Gln563</sup>: Bbp<sup>Asp588,Ser585,Thr586,Thr587</sup> and Fg $\alpha$ <sup>Phe564</sup>:Bbp<sup>Ser585</sup>

(Figure 5). The importance of  $Fg\alpha^{Gln563}$  described as a persistent H-bond contact with Bbp<sup>Asp588,Thr586</sup> and important locking contact is reinforced by its high correlation values. The same analysis was performed for the simulations of Bbp complexed with the elongated Fg $\alpha$  peptide (Supplementary Figure S2). The pattern of contacts is very similar, reinforcing the importance of Fg $\alpha^{Gln563}$ , and we observe the absence of new contacts made by the extra residues, corroborating that the short peptide contains the key residues responsible for holding the complex tight at the DLL configuration.

## **3** Discussion

During infection, Gram-positive bacteria are frequently exposed to high mechanical stress. These bacteria have evolved an intricate hostbinding mechanism to efficiently form colonies under the most inhospitable conditions. Key for the maintenance of the colonies, biofilms are an important virulence factor developed by *S. aureus* among other bacteria. In the initial steps of infection and biofilm formation, MSCRAMMS adhesins have an important role in clinging the bacteria to their human hosts Otto (2009); Latasa et al. (2006). *Staphylococcus aureus* isolated from patients suffering from septic arthritis and osteomyelitis specifically interacts with bone sialoprotein, present at bone and dentine extracellular matrix. This interaction is mediated by an specific adhesin protein, namely Bbp Ryden et al. (1987); Ganss et al. (1999); Tung et al. (2000).

Here we have explored the interaction of Bbp with Fg $\alpha$  by using an in silico SMFS approach that relies on aa- and CG-SMD simulations. CG-SMD simulations have proven to bridge the force-loading gap between in vitro SMFS data with in silico data obtained from aa-SMD simulations, distanced by orders of magnitude Gomes D. E. et al. (2022). In addition, CG-SMD simulations require much less computational power Liu et al. (2021); Poma et al. (2019), enabling us to explore pulling speeds unfeasible to simulate via aa-SMD Gomes D. E. et al. (2022). Using an approach previously described Souza et al. (2019), we combined GõMartini approach Poma et al. (2017) with Martini 3 Souza et al. (2021) obtaining sensible results. The higher spread of rupture force at faster pulling rates suggests that forceinduced extensions may result in lost of relevant interactions between CG-bead pairs, indicating that further optimization of the contact map or redefinition of the native contacts is necessary to improve the results Mahmood et al. (2021).

Here, we showed that Bbp: Fg $\alpha$  complex can withstand forces even higher than the previously investigated SdrG: Fg $\beta$  complex Milles et al. (2018), overcoming the 2 nN force range for rupture forces, equivalent to breaking covalent bonds, demonstrating the high mechanostability of the Bbp:  $Fg\alpha$  complex. We revealed that the force propagation pathway between the anchoring and pulling points of the Bbp: Fga complex goes beyond the interactions between the latch and the peptide, passing through an intricate network involving several amino acids of the Bbp N2 domain (Figure 4). We were also able to point the key residues H-bonds responsible for keeping the complex stable at such high mechanical stress, highlighting important backbone-backbone interactions between  $Bbp^{Leu584,\ Thr582,\ Thr586}$  and  $Fg\alpha^{Thr565, Ser567, Thr586}$  but also side-chain connections, such as  $Bbp^{Asp334}$ : Fg $\alpha^{Thr565}$ , Bbp<sup>Ser333</sup>:Fg $\alpha^{Phe564}$  and Bbp<sup>Asp588</sup>:Fg $\alpha^{Gln563}$  (Table 1). The latter being an important contact to lock the peptide N-terminus Zhang et al. (2015). Fg $\alpha^{Gln563}$  has also revealed to be a key network hub, being highly correlated with several residues on the complex interface such as Bbp<sup>Asp588,Ser585,Thr586,Thr587</sup> (Figure 5). We also showed that the short Fg $\alpha$  peptide is able to hold the key interactions responsible for its mechanostability by probing an elongated Fg $\alpha$  in complex with Bbp (Supplementary Figures S1 and S2).

By probing the Bbp:  $Fg\alpha$  complex under high mechanical load, we discovered the molecular mechanism that triggers Bbp's unique resilience to shear forces. The high force-loads that can be found during initial stages of bacterial infection stabilize the interconnection between the protein's amino acids, particularly along the  $\beta$ -sheets that, due to their force-loading geometry, cannot be "peeled" like other  $\beta$ -sheet-rich proteins, such as green fluorescent protein (GFP) Hughes and Dougan (2016); Dietz et al. (2006) and human filamins Seppälä et al. (2017); Haataja et al. (2019). Our results build on previous knowledge of host-microbial interactions, supporting the idea that anti-adhesion therapies might be fundamental in our fight against nosocomial bacteria infections.

Antiadhesion therapies are attractive since they would not target essential processes and have the potential advantage of eliciting less and slower resistance aquisition. Some of the approaches using peptides have been reviewed elsewhere Dufrêne and Viljoen (2020). Our findings support that a short peptide is capable of holding the essential interactions to keep the protein locked in the DLL configuration. This could be explored on the design of small peptidomimetic compounds that can mimic these interactions. Moreover, peptidomimetics overcome the poor pharmacokinetic profile and low selectivity associated with peptide therapies, the main drawback for this kind of approach Li Petri et al. (2022). Another possible strategy would be to replace the peptide backbone for a small drug-like molecule with substituents that could mimic the bioactive conformation of the native peptide Spiegel et al. (2012).

Due to the good agreement between our *in silico* SMFS protocol and experiments, we could use our simulations as a platform to study structure-activity relationships and not only screen the early potential drug candidates, but also decipher their mechanisms of action. The best candidates can be later probed by SMFS experiments. In summary, our work presents a key step in creating a intelligent design for a new class of antibiotics that act on the initial stages of bacterial infection.

# 4 Methods

### 4.1 Structure preparation

The structure of Bbp in complex with Fg $\alpha$  has been previously solved by means of X-ray crystallography at 1.45 Å resolution Zhang et al. (2015) and deposited at the Protein Data Bank (PDB ID: 5CFA). Here we retrieved this structure and prepared it for molecular dynamics (MD) simulations using VMD Humphrey et al. (1996) and its plugin QwikMD Ribeiro et al. (2016). To investigate the loading rate dependency on the size of the peptide, we used Modeller v.10.1 Webb and Sali (2016) to create an additional structure of the complex where the Fg $\alpha$  was elongated by nine residues at its C-terminal end, in respect of the crystal structure, following the sequence of Fg $\alpha$  from *Homo sapiens* (Uniprot ID: P02671). The model followed the same preparation as described for the crystal structure.

### 4.2 All-atom molecular dynamics simulations

The complexes between BBP and Fg $\alpha$  in its short or longer configuration were solvated using the TIP3P water model

Jorgensen et al. (1983), with the net charge of the protein neutralized using a 150 mM concentration of sodium chloride. Steered molecular dynamics (SMD) simulations were carried out using NAMD 3 Phillips et al. (2020), with the CHARMM36 force field Best et al. (2012). The simulations were performed assuming periodic boundary conditions in the isothermal-isobaric ensemble (NPT) with temperature maintained at 300 K using Langevin dynamics for temperature and pressure coupling, the latter kept at 1 bar. A distance cut-off of 11.0 Å was applied to short-range non-bonded interactions, whereas longrange electrostatic interactions were treated using the particle-mesh Ewald (PME) Darden et al. (1993) method. Taking advantage of a hydrogen-mass repartitioning method implemented in VMD's autopsfgen, the time step of integration was chosen to be 4 fs for all production aa-MD simulations performed. Before the SMD simulations, the system was submitted to an energy minimization protocol for 1,000 steps. An MD simulation with position restraints in the protein backbone atoms was performed for 1 ns, with temperature ramping from 0 K to 300 K in the first 0.5 ns at a timestep of 2.0 fs in the NVT ensemble, which served to pre-equilibrate the system. In an in silico single-molecule force spectroscopy (SMFS) strategy Verdorfer et al. (2017); Bernardi et al. (2019), SMD simulations were carried out in several replicas, using a constant velocity stretching protocol at three different pulling speeds (Supplementary Table S1). SMD was employed by harmonically restraining the position of the amino acid at the C-ter of Bbp and moving a second restraint point at the C-ter of Fg $\alpha$  peptide with a 5 kcal/mol Å<sup>2</sup> spring constant, with constant velocity in the z-axis. The force applied to the harmonic spring is then monitored during the time of the SMD. The pulling point was moved with constant velocity along the z-axis and due to the single anchoring point and the single pulling point the system is quickly aligned along the z-axis. The number of replicas for each velocity is indicated at Supplementary Table S1.

# 4.3 Coarse-grained molecular dynamics simulations

The atomistic model of Bbp:  $Fg\alpha$  was modeled onto the Martini 3.0 Coarse-grained (CG) force field (v.3.0.b.3.2) Souza et al. (2021) using martinize2 v0.7.3 Kroon (2020). A set of native contacts, based on the rCSU + OV contact map protocol, was computed from the equilibrated all-atom structure using the rCSU server Wołek et al. (2015) and used to determine Gö-MARTINI interactions Poma et al. (2017) used to restraint the secondary and tertiary structures with the effective depth  $\epsilon$  of Lennard-Jones potential set to 9.414 kJ.mol<sup>-1</sup>. All CG-MD simulations were performed using GROMACS version 2021.5 Abraham et al. (2015). The Bbp: Fg $\alpha$  complex was centered in a rectangular box measuring with 10.0, 10.0, 25.0 nm to the x, y, and z directions. The anchor (Bbp C-terminal) and pulling (peptide C-terminal) backbone (BB) atoms were used to align the protein to the Z-axis. The box was then solvated with Martini3 water molecules. Systems were minimized for 10,000 steps with steepest descent, followed by a 10 ns equilibration at the NPT ensemble using the Berendsen thermostat at 298K, while pressure was kept at 1 bar with compressibility set to 3e<sup>-4</sup>bar<sup>-1</sup>, using the Berendsen barostat. A time step of 10 fs was used to integrate the equations of motion. Pulling simulations were subsequently done at the NVT ensemble with a time step of 20 fs the temperature was controlled using the v-rescale thermostat Bussi et al. (2007) with a coupling time of 1 ps for all CG-MD simulations, the cutoff distance for Coulombic and Lennard-Jones interactions was set to 1.1 nm De Jong et al. (2016), with the long-range Coulomb interactions treated by a reaction field (RF) Tironi et al. (1995) with  $\epsilon_r = 15$ . The Verlet neighbor search Verlet (1967) was used in combination with the neighbor list, updated every 20 steps. The LINCS Hess et al. (1997) algorithm was used to constrain the bonds and the leapfrog integration algorithm for the solution of the equations of motion. Several replicas of CG-SMD simulations were performed at a range of speeds described at Supplementary Table S1.

## 4.4 Simulation data analysis

All analysis presented at the main text correspond to the Bbp:  $Fg\alpha$  original complex. Force loading rate and mean correlation values for Bbp complexed with the elongated  $Fg\alpha$  peptide are found on the Supplementary Information material. H-bonds occupancy between Bbp and Fg $\alpha$  were calculated and averaged for aa-MD simulations 1 ns before the main rupture event, using VMD Humphrey et al. (1996) with standard parameters for the calculation: residue pairs; donor-acceptor distance of 3.0 Å; angle cutoff of 20°. Mean correlation and dynamical network pathways were calculated using the generalized dynamical network analysis Melo et al. (2020) and VMD for aa-SMD at pulling velocity of  $2.5 \times$ 10<sup>-4</sup> nm/ps. In this analysis, a network is defined as a set of nodes that represent amino acid residues, and the node's position is mapped to that of the residue's  $\alpha$ -carbon. Edges connect pairs of nodes if their corresponding residues are in contact, and two nonconsecutive residues are said to be in contact if they are within 4.5 Å of each other for at least 75% of analyzed frames. The interface residues between Bbp: Fg $\alpha$  were defined in a radius of 10 Å between nodes in each molecule. A representative for the full-network, optimal and suboptimal paths and communities was rendered using one of the SMD trajectory replicas. The mean correlation analysis was carried out 1 ns before the first rupture event using a cutoff of 0.35 for the mean correlation coefficients. All charts were generated using in-house python scripts. The protein image was rendered using VMD.

## Data availability statement

The raw data supporting the conclusion of this article will be made available upon request to the corresponding author.

# Author contributions

PG, MF and MP contributed to performing simulations, analysing data, and writing of the manuscript. DG contributed to analysing data and discussion. RB contributed to writing and discussion on *in silico* force spectroscopy, proof-reading, manuscript revision and approval of the submitted version. PG and RB coordinated the project.

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# Conflict of interest

The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

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### Supplementary material

The Supplementary Material for this article can be found online at: https://www.frontiersin.org/articles/10.3389/fchem.2023.1107427/full#supplementary-material

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