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A commentary on

Effects of parametrical and trial-to-trial variation in prior probability processing revealed by simultaneous electroencephalogram/functional magnetic resonance imaging

by Scheibe, C., Ullsperger, M., Sommer, W., and Heekeren, H. R. (2010). J. Neurosci. 30, 16709–16717.

Event-related potentials (ERP) observed in the electroencephalogram (EEG) have traditionally provided neural markers for an array of cognitive phenomena through averaging time-locked amplitudes over many trials. However, it is becoming clear that understanding trial-to-trial variability in neural activity and its behavioral consequences is an important venture in cognitive and systems neuroscience. Recent studies have begun to focus on how fluctuations in functional magnetic resonance imaging (fMRI) and electrophysiological (EEG/MEG) signals are correlated with moment-to-moment fluctuations in behavior (e.g., Fox et al., 2005; Pessoa and Padmala, 2005; Mars et al., 2008). Indeed, neural responses can vary in theoretically important ways which may reflect a signature of task-relevant brain-state changes such as a subject's cognitive "context" (Lutz et al., 2002). As such, focusing on single-trial data can provide a more direct link between neural activity and cognitive processes, such as executive function and decision making (Debener et al., 2006).

Examining trial-to-trial variability may provide a unique window for exploring dynamic modulations in the decisionmaking process, which frequently requires computing many variables that inform and optimize the decision (e.g., Mulert et al., 2005; Weissman et al., 2006; Esposito et al., 2009). One such variable is prior probability (PP), the prior knowledge of the probability concerning the decision alternatives. This PP must be integrated into the decision-making process to form expectations about which event is the most probable to occur. Behavioral studies have previously shown that PP modulates behavior, with increasing PP predicting faster reaction times (e.g., Carpenter, 2004). Neural correlates of this behavioral effect have been linked to changes in the contingent negative variation (CNV), whose mean amplitude increases with increasing PP (Scheibe et al., 2009). Nevertheless, while mean amplitude ERPs such as the CNV can provide insight into PP processing, it neglects to consider trialspecific neural processes and their associated brain regions.

Scheibe et al. (2010) tackled this problem in a recent issue of The Journal of Neuroscience by simultaneously recording EEG and fMRI as participants performed a simple number comparison task (Scheibe et al., 2010; Figure 1A). On each trial, participants saw a fixation cross, followed by a number (S1; 1, 3, 5, 7, 9) presented at either side. After 2000 ms, a second number (S2; any number not used in S1) was then displayed at the opposite side of the fixation and remained until the participant responded by indicating the numerically larger number. Essentially, S1 served as a cue with information about the probability of the side with the largest value with a predictive value of 1.0 (1 or 9), 0.75 (3 or 5), or 0.5 (5). As expected, this design produced a robust parametric behavioral effect of PP, with increasing PP predicting faster RTs (Scheibe et al., 2010; Figure 1B).

When examining the neural basis of these behavioral effects, Scheibe et al. (2010) observed substantial trial-to-trial variability in the CNV response (Scheibe et al., 2010; Figure 2A). To identify the neural correlates of trial-to-trial fluctuations of PP processing, Scheibe et al. (2010) conducted three distinct analyses. First, the authors identified voxels parametrically modulated by PP. Using this method, they demonstrated that the posterior medial frontal cortex (pMFC) increased parametrically with increasing PP. Next, Scheibe et al. (2010) employed an EEG-informed fMRI analysis, which utilizes the variability in EEG data to predict changes in BOLD response (e.g., Goldman et al., 2009). In order to identify voxels whose activity covaried with the CNV, Scheibe et al. (2010) added a regressor using the CNV amplitude for each trial. This identified a network of regions including the middle frontal gyrus (MFG), dorsolateral prefrontal cortex (DLPFC), and putamen (Scheibe et al., 2010; Figure 4A). The authors then regressed out the variance attributable to PP, and used the residuals in a follow up regression model. Finally, by comparing the model derived from the EEG-informed fMRI analysis and the follow up regression model, regions that were only activated in the former and not the latter model were identified as being attributable only to PP processing. Here, the authors showed that the DLPFC, right inferior frontal gyrus (IFG), and right inferior parietal lobule (IPL; Scheibe et al., 2010; Figure 4B) were modulated exclusively by the processing and integration of PP into response preparation.

These results provide novel insights into trial-specific information processing of PP during decision making. Scheibe et al. (2010) show that the neural integration of PP has at least three levels. Firstly, increasing PP indexes the need for behavioral adjustment, which is reflected by increases in pMFC and the CNV in order to successfully prepare motor responses and guide future decisions. Previously, the pMFC has been shown to be involved in performance monitoring and cognitive control induced behavioral adjustments (Ridderinkhof et al., 2004). Next, Scheibe et al. (2010) were able to identify regions that covaried with the CNV, which they suggest might index unspecific

preparatory processes. Finally, regions including the DLPFC were exclusively related to PP-induced CNV fluctuations. Given the role of the DLPFC in establishing, regulating, and actively maintaining attention (MacDonald et al., 2000; Weissman et al., 2006), the authors suggest that this reflects trial-specific attentional effort, depending on the probability information. However, it is worth noting that the exact cognitive mechanisms would need to be elucidated with future studies that manipulate attentional control.

In addition, the results of Scheibe et al. (2010) are accompanied by at least two caveats. First, methods that alter the relationship between correlated factors in a general linear model (e.g., orthogonalization) can sometimes impose interpretational challenges on the resulting estimates, depending on the degree of correlation between the factors (Hunt, 2008). Applying this logic to Scheibe et al. (2010) it is important to note that their analyses proceeded in three stages, with the third and final stage utilizing the residuals from a previous - but related - model. Although this approach allows Scheibe et al. (2010) to partial out variance that is attributable to PP, the results and interpretations could depend on the correlation between the original model factors. Second, while Scheibe et al. (2010) used a 200-ms time window for their mean amplitude CNV analysis, they used a significantly larger window of 1000 ms in their single-trial analysis of the CNV. This 1000 ms epoch could potentially conflate other processes with the CNV quantification. Indeed, the CNV may have at least two phases: an early, frontal phase relating to orientation and a later, more posterior phase relating to the motor preparation of the response (Gómez et al., 2003). By focusing their analysis on a large temporal window over one central electrode site (Cz), Scheibe et al. (2010) may have failed to capture distinct processes relating the CNV.

More generally, concurrent EEG–fMRI recordings also present some key challenges for researchers. Importantly, either method alone suffers from a lack of consistency in distinguishing between trial-to-trial variability that is functionally significant and variability that is simply noise. There are many algorithms that have been proposed for quantifying trial-to-trial variability in EEG data. These include techniques such as hierarchical Bayesian modeling (Wu et al., 2011), linear dynamical system response and independent response modeling (Limpiti et al., 2009). Nevertheless, estimating trialto-trial variability still represents an important venture in future research in order to adequately utilize this in EEG-informed fMRI analysis. Particularly important to multimodal studies is that fMRI does not necessarily identify the neural generators of EEG signals as each can differ in their sensitivity to experimental manipulations (Debener et al., 2006). Indeed, the variability observed in the electrophysiological data may not necessarily be reflected in the fMRI signal. Vartiainen et al. (2011) recently tested this issue empirically, demonstrating that hemodynamic and electrophysiological measures show strikingly different functional patterns within the same tasks. Exploring these differences should serve as a first step toward a principled combined use of hemodynamic and electrophysiological measures.

Despite these challenges, Scheibe et al. (2010) provide novel insights into the neural mechanisms of PP processing - thus highlighting the power of multimodal studies. However, it could also be important probe the dynamic interplay between intrinsic and task-evoked brain activity (Northoff et al., 2010). Indeed, neuroscience has only begun to fully exploit the dynamic changes in restingstate networks and link those to changes in mental function. The brain can be considered a dynamic system which can itself determine properties of the response to any given stimulus (Debener et al., 2006) and so intrinsic ongoing brain activity may also be an important determinant of the trial-to-trial fluctuations observed in Scheibe et al. (2010). Along these lines, behavioral performance should not automatically be attributed to fluctuations in task-related cognitive processes, as ongoing fluctuations in intrinsic neuronal activity have been shown to play an important role (Fox et al., 2007). Elucidating the relationship between these two forms of brain activity could provide a unique window for examining the cause of trial-to-trial variability in brain and behavior.

ACKNOWLEDGMENTS

We wish to thank Dr. Scott Huettel and Rene San Martin for helpful comments and discussion regarding this commentary. We were supported by an ESRC grant (Amy R. Bland) and by a NIMH National Research Service Award F31-086248 (David Victor Smith).

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Received: 28 February 2011; accepted: 26 July 2011; published online: 15 August 2011.

Citation: Bland AR, Mushtaq F and Smith DV (2011) Exploiting trial-to-trial variability in multimodal experiments. Front. Hum. Neurosci. 5:80. doi: 10.3389/ fnhum.2011.00080

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