



Constructing Cu₇S₄@SiO₂/DOX Multifunctional Nanoplatforms for Synergistic Photothermal– Chemotherapy on Melanoma Tumors

Leilei Zhang^{1,2}, Hui Pan^{1,2}, Yongyun Li^{1,2}, Fang Li^{1,2} and Xiaolin Huang^{1,2*}

¹ Department of Ophthalmology, Ninth People's Hospital, Shanghai Jiao Tong University School of Medicine, Shanghai, China, ² Shanghai Key Laboratory of Orbital Diseases and Ocular Oncology, Shanghai, China

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> *Correspondence: Xiaolin Huang drmaureenhuang@163.com

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Zhang L, Pan H, Li Y, Li F and Huang X (2020) Constructing Cu₇S₄@SiO₂/DOX Multifunctional Nanoplatforms for Synergistic Photothermal– Chemotherapy on Melanoma Tumors. Front. Bioeng. Biotechnol. 8:579439. doi: 10.3389/fbioe.2020.579439 The integration of photothermal therapy and chemotherapy has been recognized to be an efficient strategy through the instant thermally ablation and long-term chemical inhibition, thus achieving high therapeutical effect. In the present work, we designed and prepared Cu₇S₄@SiO₂/DOX nanocomposites and used them as efficient nanoplatforms for synergistic photothermal-chemo therapy on melanoma tumors. The Cu₇S₄@SiO₂/DOX was constructed by firstly synthesizing Cu₇S₄ nanocrystals, then in situ growing SiO₂ shell on the surface of Cu_7S_4 nanocrystals, and finally loading DOX within SiO2 shell. The Cu7S4@SiO2/DOX was composed of Cu7S4 core as the photothermal transducer, SiO2 shell as DOX carrier and DOX as the model of anticancer drug. Once exposed to a 1064 nm laser, the Cu₇S₄@SiO₂/DOX could simultaneous generate heat for photothermal therapy and accelerate the DOX release. When the Cu₇S₄@SiO₂/DOX was injected into the center of tumor, the tumor exhibit rapid temperature elevation once exposed to the NIR laser and the tumor growth is significantly inhibited through the synergistic photothermal-chemo therapy, in comparison to the limited therapeutical effect of photothermal therapy or chemotherapy alone. Therefore, the $Cu_7S_4@SiO_2/DOX$ with photothermal-chemo function can be used as excellent nanoplatforms for treating solid tumor with high theoretical effect.

Keywords: $Cu_{2-x}S$ nanocrystals, mesoporous SiO₂, photothermal therapy, chemotherapy, melanoma

INTRODUCTION

The near infrared (NIR) light-driven cancer treatments have caught a numerous attention for years due to the NIR light with higher tissue-penetration depth than visible light and the better safety than ultraviolet light (Cheng et al., 2014; Vankayala and Hwang, 2018). Among these NIR-induced therapy modalities, the photothermal therapy is an emerging one that utilizes NIR absorbents as energy transducers to convert NIR laser energy into heat (>42°C), so that thermally ablate cancer cells (Zou et al., 2016; Yu et al., 2018b). For the development of photothermal therapy, the photothermal nanoagents are the key point and they should be capable of strong and broad NIR photoabsorption and high photothermal conversion efficiency. Apart from the noble metal nanostructures (Dreaden et al., 2011; Huang et al., 2011) and the organic-based nanoparticles (Liu et al., 2013; Zha et al., 2013), the recent progress of photothermal nanoagents focus on

semiconductor nanomaterials because of their abundant types, tunable composites, photostability as well as efficient photothermal effect (Huang et al., 2017). The semiconductorbased photothermal nanomaterials mainly include the metal oxides such as the doped TiO_{2-x} nanocrystals (Ren et al., 2015; Ou et al., 2016; Yu et al., 2017) and oxygen-deficient WO_{3-x} nanocrystals (Xu et al., 2015; Wen et al., 2016), and the metal sulfides including $Cu_{2-x}S$ nanostructures (Tian et al., 2011a,b) and Bi₂S₃ nanodots (Li et al., 2016). For example, Cu_{7.2}S₄ nanoparticles were prepared by the thermolysis of Cu(DEDTC)₂ precursors and they exhibited strong NIR absorption, photostability and photothermal conversion efficiency up to 56.7%, which were used as a photothermal nanoagent for the photothermal ablation of cancer cells (Li et al., 2014). However, the therapeutical effect of photothermal therapy is executed only under the illumination of laser and it would disappear instantly when laser is switched off. Thus, to achieve the long-term therapeutical effect for photothermal nanoagents, it is quite necessary to combine with other therapeutical modalities.

The integration of photothermal therapy and chemotherapy has been recognized to be an efficient strategy through the instant thermally ablation and long-term chemical inhibition (You et al., 2012; Yu et al., 2018a; Zhang et al., 2020). Importantly, the photothermal effect can accelerate the drug releasing rate and induce the chemo-sensitization effect, thus achieving the synergistic effect with higher therapeutical results than photothermal therapy or chemotherapy alone. Up to data, there are a number of nanoagents with the photothermal effect and drug loading capacity, which can be allocated into two types. The first type consists the photothermal nanomaterials with a large volume of inner cavity or high specific surface area, such as CuS hollow nanospheres (Wang et al., 2018), two-dimensional MoS₂ nanosheets (Liu et al., 2014) and metal-organic frameworks (Zhang et al., 2018). For instance, CuS hollow nanospheres with 87.7% of high doxorubicin (DOX) content were prepared while the DOX release rate at pH 7.4 was only 4.6% and at pH 5.0 was 10.3% within 10 h (Wang et al., 2018). The second type is the combination of photothermal nanoagent and drug carrier, which includes Cu₉S₅@mSiO₂-PEG core-shell structures (Song et al., 2013), Au@copolymer-liposome nanostructures (Zheng et al., 2016) and CuS@gel nanocomposites (Meng et al., 2016). For example, a thermosensitive MEO₂MA@MEO₂MA-co-OEGMA nanogels were firstly prepared and then CuS nanoagents were in situ deposited within nanogels, whereas the DOX loading content was less than 10%, (Meng et al., 2016). Therefore, it is of great importance to design and synthesis of photothermal-chemo nanoagents with the high photothermal conversion efficiency and high drug loading capacity.

In order to integrate synergistic photothermalchemo functions, we prepared a $Cu_7S_4@SiO_2/DOX$. The $Cu_7S_4@SiO_2/DOX$ was constructed by firstly synthesizing Cu_7S_4 nanocrystals, then *in situ* growing SiO_2 shell on the surface of Cu_7S_4 nanocrystals, and finally loading DOX within SiO_2 shell. The $Cu_7S_4@SiO_2$ nanoplatforms exhibited the strong and broad NIR absorption and could rapidly convert 1064 nm laser energy into heat with the efficiency of 48.2%, and they also demonstrated large specific surface area and pores with high DOX loading content of 59.8%. Importantly, After the irradiation cycles, 90.1% of DOX was released from $Cu_7S_4@SiO_2/DOX$ with the help of 1064 nm NIR laser at pH 5.4 in comparison to 61.5% of the released DOX without irradiation, indicating photothermal effect accelerated the DOX release. More importantly, when $Cu_7S_4@SiO_2/DOX$ was intratumorally injected into tumor-bearing mice, the tumor growth was heavily inhibited through the synergistic photothermal-chemo therapy compared with the limited therapeutical effect of photothermal therapy or chemotherapy alone. Therefore, the $Cu_7S_4@SiO_2/DOX$ with high photothermal conversion efficiency and drug loading capacity can be used for treating solid tumor with high therapeutical effect.

MATERIALS AND METHODS

Materials

Sodium diethyldithiocarbamate (SDEDTC), CuCl₂·2H₂O (AR), oleic acid (AR), oleylamine (80–90%), cetyltrimethylammonium bromide (CTAB), sodium hydroxide (NaOH, AR), doxorubicin hydrochloride (DOX) and tetraethylorthosilicate (TEOS, GR) were brought from Sigma Aldrich.

Preparation of Cu₇S₄ Nanocrystals

The Cu₇S₄ nanocrystals were prepared by a typical thermolysis method (Li et al., 2014). Firstly, CuCl₂·2H₂O (20 mmol) was dissolved into 10 mL deionized water, which was then dropwise added into aqueous solution of SDEDTC (90 mL, 50 mmol) under magnetically stirring. After stirring for 2 h, the above solution was centrifuged (5000 rpm, 5 min) and washed with deionized water. The precipitate [Cu(DEDTC)₂ precursor] was dried in vacuum at 50°C for further use. Secondly, oleic acid (15 mL) and oleylamine (10 mL) were added into threeneck bottle and heated to 280°C within 30 min under the continuous nitrogen flow to remove any moisture and oxygen. The Cu(DEDTC)₂ precursor (1 mmol) dissolved in 2 mL oleic acid was injected to the three-neck bottle and heated at 280°C for 10 min. The dark green mixture was quickly cooled to 60°C by air flow and then 20 mL ethanol was introduced to precipitate Cu₇S₄ nanocrystals. Finally, the Cu₇S₄ nanocrystals were dispersed in ethanol followed by centrifuging and washed with ethanol for three times.

Preparation of Cu₇S₄@SiO₂ Nanoplatforms

The Cu₇S₄@SiO₂ nanoplatforms were prepared by *in situ* growing SiO₂ shell on the surface of Cu₇S₄ nanocrystals. Firstly, the hydrophobic Cu₇S₄ nanocrystals were converted into hydrophilic Cu₇S₄ through the surface-modification with CTAB. The Cu₇S₄ nanocrystals in chloroform solution (5 mL, 10 mg/mL) were added into aqueous solution of CTAB (20 mL, 100 mg/mL), which was stirred vigorously at 40°C for 24 h and then centrifuged to collect hydrophilic Cu₇S₄ nanocrystals. Secondly, the hydrophilic Cu₇S₄ nanocrystals were dispersed

into 50 mL deionized water, followed by the introduction of NaOH solution (0.1 mL, 10 mg/mL) and TEOS (0.1 mL) under sonication. After 1 h of sonication, then 100 μ L of PEG-silane was added and the mixture was maintained at 40°C for another 8 h. The products were centrifuged and washed with deionized water for three times for collecting Cu₂S₄@SiO₂ nanoplatforms.

Characterizations

The size, morphology, phase of $Cu_7S_4@SiO_2$ nanoplatforms were characterized by using JEOL 2100F transmission electron microscopy (TEM). The photoabsorption of $Cu_7S_4@SiO_2$ nanoplatforms was studied on a Shimadzu UV-1900 spectrophotometer. The concentration of copper irons released from the $Cu_7S_4@SiO_2$ nanoplatforms was determined by an inductively coupled plasma atomic emission spectroscopy (ICP-AES). The specific surface area and pore diameter of $Cu_7S_4@SiO_2$ powder were investigated on the Autosorb-iQ/Autosorb-iQ Brunauer-Emmett-Teller (BET).

Photothermal Conversion Efficiency

The photothermal performance of $Cu_7S_4@SiO_2$ nanoplatforms was investigated by illuminating their aqueous dispersion at a series of concentrations under a 1064 nm laser with the output power density of 0.6 Wcm⁻². The temperature change was recorded by using a thermal imaging camera. The photothermal conversion efficiency of $Cu_7S_4@SiO_2$ was calculated according to the previous report (Li et al., 2014) by applying the below equations:

$$\eta = \frac{hA(\Delta T_{\max, dis} - \Delta T_{\max, H_2O})}{I(1 - 10^{-A_{1064}})}$$
(1)

$$\tau_s = \frac{m_D C_D}{hA} \tag{2}$$

Where *I* and A_{1064} , respectively, stand for the NIR laser intensity and the absorbance at 1064 nm. $\Delta T_{\max,dis}$ and $\Delta T_{\max,H_2O}$ are the temperature change of deionized water and the solution containing Cu₇S₄@SiO₂ nanoplatforms. The *h* and *A* are the heat transfer coefficient and the surface area, and the value of *hA* is determined from Eq. 2 by using the system time constant τ_s with the help of the mass (*m*_D) and the heat capacity (*C*_D) of deionized water.

Dox Loading and Releasing

For loading DOX, $Cu_7S_4@SiO_2$ (2.5 mL, 10 mg/mL) and DOX (10 mg) were dispersed into PBS solution, which was magnetically stirred in the dark. After 24 h of stir, the mixture was centrifuged (12,000 rpm, 30 min) and the supernatant was collected. The DOX loading content was calculated based on (load weight of DOX/Cu_7S_4@SiO_2/DOX) × 100%, in which the load weight of DOX was determined by (10 mg – DOX in the supernatant). For DOX releasing, $Cu_7S_4@SiO_2/DOX$ was dispersed into PBS at pH 7.4 or pH 5.4 and divided into two groups. One group was used as control and 0.5 mL solution were taken out which was centrifuged (12,000 rpm, 15 min) at each time point. Another group was irradiated by a 1064 nm NIR laser (0.6 Wcm⁻²) at a specific time. The DOX releasing rate was calculated by using (the release weight of DOX/the load weight of DOX) \times 100%.

Photothermal-Chemo Therapy in vitro

Melanoma cells were seeded into a 96-well plate $(1.2 \times 10^4 \text{ cells per well})$ at 37°C in the presence of 5% CO₂ for 24 h. After incubation, the cell medium was removed, the cells were divided into four groups: (1) control, (2) DOX, (3) Cu₇S₄@SiO₂/DOX+NIR, (4) Cu₇S₄@SiO₂+NIR. Hundred microliter of the dispersion at varied concentrations was then added into the wells. After incubation for another 24 h, the cells were washed with PBS buffer solution for three times. Then the cells were irradiated with/without a 1064 nm laser. Cell viability was measured using the CCK-8 assay.

To visually compare the viability difference in cellular level among four groups, cells were seeded into a 24-well plate at a density of 1.2×10^5 cells per well. After the cells in the four groups were treated, the cells were stained with calcein AM (live cells) and propidium iodide (dead cells) to distinguish live cells with green fluorescence and dead cells with red fluorescence.

Photothermal-Chemo Therapy *in vivo* and Histological Examination

The BALB/c mice (~16 g, male) with 4T1 tumors (the surface diameter of $0.3\sim0.5$ cm) on the back were divided into four groups (n = 3): (1) The control group; (2) DOX group; (3) Cu₇S₄@SiO₂+NIR group; (4) Cu₇S₄@SiO₂/DOX+NIR group. The mice in (2) group were intratumorally injected with DOX PBS solution (50 µL, 80 µg), and mice in (3 and 4) group were, respectively, injected with Cu₇S₄@SiO₂ (50 µL, 0.1 mg mL⁻¹) or Cu₇S₄@SiO₂/DOX PBS solution (50 µL, 0.1 mg mL⁻¹). The tumors on mice in (3, 4) group were exposed to a 1064 nm NIR laser (0.6 Wcm⁻²) at the 0.5 h post-injection and mice body. After treatments, mice in all groups were observed regarding their body weight and tumor sizes. When a tumor size was beyond 1.0 cm, mice in all groups were sacrificed and tumors were extracted for histological examination.

RESULTS AND DISCUSSION

The Cu₇S₄@SiO₂ nanoplatforms were prepared by in situ growing SiO₂ shell on the surface of Cu₇S₄ nanocrystals. Firstly, Cu₇S₄ nanocrystals were synthesized through a typical thermolysis method, where the Cu(DEDTC)₂ precursor with Cu source and S source was heated to 280°C for 10 min to produce uniform Cu₇S₄ nanocrystals. Secondly, the Cu₇S₄ nanocrystals were served as the core to allow the coating of SiO₂ shell through the hydrolysis of TEOS. During the SiO₂ coating, CTAB were used as a soft template. SiO₂ grew around the template due to electrostatic interactions. Supplementary Figure S1 shows the size and zeta potential of nanoparticles during the process of synthesis. FTIR spectra in Supplementary Figure S2 demonstrated that PEG was coated on the surface of Cu7S4@SiO₂ nanoplatforms, thus the nanoplatforms could be realized the bioapplication directly. The as-obtained Cu₇S₄@SiO₂ nanoplatforms have a uniform morphology and the average size

of 100 nm, as shown in the TEM image (Figure 1a). Obviously, the Cu₇S₄@SiO₂ nanoplatforms consist of Cu₇S₄ as the core and SiO₂ as the shell, and the Cu₇S₄ nanocrystals have the average diameter of 50 nm and the SiO₂ shells have the average thickness of 25 nm. The nanoplatforms showed good dispersion as the size in water showed little change over time demonstrated by dynamic light scattering (DLS, Supplementary Figure S3). Furthermore, the high-resolution (HR-TEM) image in Figure 1b demonstrates the apparent lattice with an interplane d spacing of ~ 0.277 nm, which can be indexed to the (110) plane of the orthorhombic Cu₇S₄ (JCPDS card no. 22-0250), which verifies the core is Cu₇S₄ nanocrystals. Subsequently, the phase of Cu₇S₄@SiO₂ powders was characterized by using XRD. The XRD pattern (Figure 1c) reveals that there are four prominent peaks centered at 27.87°, 32.30°, 46.40°, and 54.70°, which can be respectively, corresponded to the (202), (220), (224), and (422) planes for the orthorhombic Cu₇S₄ (JCPDS card no. 22-0250). It should be noted that there is a broad peak between 10° and 40° , which should be attributed to the characteristic peak originating from the amorphous SiO₂ shell. Supplementary Figure S4 shows the XPS spectra of Cu 2p in the Cu₇S₄@SiO₂ nanoparticles. The binding energy peaks at 932.8 and 954.6 eV can be assigned to Cu⁺ coordinated to Cu in Cu₇S₄@SiO₂ nanoparticles, whereas the binding energy peak at 943.2 eV is formally described as Cu²⁺. The coexistence of Cu⁺ and Cu²⁺ indicated the Cu vacancies on the surface of Cu₇S₄ nanocrystals (Li et al., 2015). Thus, the above results confirmed the successful preparation of Cu₇S₄@SiO₂ nanoplatforms with Cu₇S₄ core and SiO₂ shell.

Subsequently, the photoabsorption of $Cu_7S_4@SiO_2$ nanoplatforms was studied by using UV-vis-NIR spectrometer. The $Cu_7S_4@SiO_2$ nanoplatforms can be well dispersed into deionized water and their aqueous solution shows the dark green. As demonstrated in UV-vis-NIR photoabsorption spectra (**Figure 1d**), the aqueous solution containing $Cu_7S_4@SiO_2$ nanoplatforms exhibits the strong absorption in the UV-vis region with the edge at ~590 nm, which can be ascribed to the bandgap absorption of $Cu_7S_4@SiO_2$ demonstrates a strong and broad NIR absorption (>650 nm) and the absorption intensity goes up with the increase of wavelength





up to 1100 nm. Compared to the bandgap-induced UV-vis absorption, this kind of NIR absorption should be attributed to the localized surface plasmon resonances (LSPR) effect because of Cu vacancies on the surface of Cu_7S_4 nanocrystals, which has been reported for other $Cu_{2-x}S$ nanocrystals (Zhao et al., 2009; Luther et al., 2011). By determining the $Cu_7S_4@SiO_2$ nanoparticle concentration via ICP-AES, the extinction coefficient of the nanoparticles at 1064 nm was measured to be 13.9 L g⁻¹ cm⁻¹, which was higher than the that of cobalt/manganese oxide (CMO) nanocrystals (Liu et al., 2019). Thus, $Cu_7S_4@SiO_2$ nanoplatforms are capable of strong and broad NIR photoabsorption because of Cu_7S_4 core.

Owing to the strong NIR absorption, we further explored the photothermal performance of $Cu_7S_4@SiO_2$ nanoparticles. The wavelength of NIR laser is quite important for photothermal therapy, and two biological transparency windows are reported as NIR-I (650–950 nm) and NIR-II (1000–1350 nm). Compared to the commonly used 808 nm, 915 m and 980 nm NIR laser, 1064 nm NIR laser can offer more efficient tissue

penetration depth by considering absorption and scattering effects (Tsai et al., 2013). Therefore, we selected 1064 nm NIR laser to study the photothermal effect of Cu₇S₄@SiO₂ nanoparticles. When exposed to a 1064 nm NIR laser at the intensity of 0.6 W cm⁻², the temperature of deionized water increases slightly (~1.3°C) within 5 min of irradiation, which confirmed the negligible photothermal effect from deionized water (Figure 2A). In contrast, once exposed to laser, the aqueous solutions containing Cu₇S₄@SiO₂ nanoparticles exhibit rapid temperature elevation within 120 s and then show a slow temperature elevation due to the balance between heat production and loss. Figure 2B summarizes the temperature elevation versus to the concentration, and they are determined to be 14.2, 21.8, 31.5, and 39.4°C for the concentration of 10, 20, 30, and 40 ppm, respectively. To further clarify the photothermal performance of Cu₇S₄@SiO₂ nanoparticles, we carried out an experiment to calculate its photothermal conversion efficiency. The aqueous solution of Cu₇S₄@SiO₂ nanoparticles were subjected to a 1064 nm NIR laser on/off, and







FIGURE 3 | (A) The nitrogen adsorption-desorption curve of Cu₇S₄@SiO₂ nanoparticles. (B) The pore diameter of Cu₇S₄@SiO₂ nanoparticles.



the whole temperature change was recorded in **Figure 2C**. The system time constant τ_s can be obtained by linearly plotting the time data with $\ln(\theta)$, as shown in **Figure 2D**. By referencing to the previous reports, the photothermal conversion efficiency of Cu₇S₄@SiO₂ nanoparticles is 48.2% which is comparable to the reported CuS nanomaterials (Li et al., 2014). Therefore, the Cu₇S₄@SiO₂ nanoparticles can rapidly and efficiently convert 1064 nm NIR laser energy into heat with the concentration-relied photothermal performance.

After demonstrating the photothermal performance of $Cu_7S_4@SiO_2$ nanoparticles, we evaluated their DOX loading capacity due to the SiO_2 shell. Prior to loading DOX, the Brunauer-Emmett-Teller (BET) surface area and pore size were investigated by using nitrogen adsorption-desorption curves. The nitrogen adsorption/desorption isotherms (**Figure 3A**) illustrate that the $Cu_7S_4@SiO_2$ nanoparticles have a specific surface area of 125.9 m²/g, showing the high surface area. In addition, the

pore diameter of $Cu_7S_4@SiO_2$ nanoparticles was also recorded and the average pore diameter was determined to be ~4.5 nm (**Figure 3B**). Therefore, the mesoporous SiO₂ shell confers high specific surface area and pores, which will facilitate the following DOX loading.

The release ability of DOX from $Cu_7S_4@SiO_2/DOX$ (the DOX loading content is 29.8%) was studied by dispersing $Cu_7S_4@SiO_2/DOX$ into PBS solution. At the time point of 1, 2, 3, 4, 6, 8, and 10 h, part of solution was taken out from the original 10 mL dispersion and centrifuged for collecting the released DOX in the supernatant, and the amount of DOX in the supernatant was calculated by applying absorption-concentration curve. **Figure 4A** shows the DOX releasing profile at pH 7.4, and it is clear that, with the prolong of time, the DOX releasing rate unceasingly goes up which can be determined to be 19.5% at 1 h, 28.4% at 2 h, and 39.4% at 4 h. After 4 h, the DOX releasing rate becomes



 $\label{eq:FIGURE 5 | Confocal images of calcein AM (green, live cells) and propidium iodide (red, dead cells) co-stained cells after incubation with Cu_7S_4@SiO_2/DOX for different treatments. Magnification: 100 times.$

very slow. In order to study the effect of NIR laser-induced photothermal effect on the DOX releasing rate, we irradiated the Cu₇S₄@SiO₂/DOX dispersion at the time point of 1, 2, 3, 4, 6, 8, and 10 h by using a 1064 nm NIR laser (5 min, 0.6 W cm⁻²). For instance, after the firstly irradiation, the DOX releasing rate is calculated to be 45.8% which is much higher than that (28.4%) at the 2 h, indicating NIR laser-induced photothermal effect can significantly enhance the DOX releasing rate. After the irradiation cycles, 75.6% of DOX is released from Cu₇S₄@SiO₂/DOX with the help of 1064 nm NIR laser in comparison to 47.4% of the released DOX without irradiation, within 10 h. Thereby, it is concluded that the Cu₇S₄ ananocrystals within Cu₇S₄@SiO₂/DOX can produce heat

to accelerate the DOX release. To study the DOX release behavior from $Cu_7S_4@SiO_2/DOX$ at the simulating tumor microenvironment, the release of the DOX against buffer solution at pH 5.4 was measured. It was found that the drug release rate became much faster at pH 5.4 (**Figure 4B**) due to the increase in the solubility of the DOX under acidic conditions, which is beneficial for cancer therapy since the microenvironments of extracellular tissues of tumors and intracellular lysosomes and endosomes are acidic.

Giving the efficient photothermal conversion effect, the high DOX loading capacity and the NIR-enhanced DOX releasing, Cu₇S₄@SiO₂/DOX can be used as excellent nanoagents for photothermal-chemo therapy. To demonstrate the synergy effect of photothermal-chemo therapy, the combination index of Cu₇S₄@SiO₂/DOX nanoparticles was measured according to previous work (Wang et al., 2013). The half-maximal inhibitory concentration (IC50) of cancer cells incubated with Cu₇S₄@SiO₂/DOX nanoparticles for combination photothermalchemo therapy is 0.52 mg mL^{-1} , while the IC50 for the sole photothermal therapy and chemotherapy is 0.67 and 1.35 mg mL^{-1} , respectively. The combination index was calculated to evaluate the combination effect of different therapies and found to be 0.823, which demonstrated the synergistic effect of Cu₇S₄@SiO₂/DOX nanoparticles for photothermal-chemo therapy. Additionally, to visualize the efficiency of photothermalchemo therapy, cells after the indicated treatments were costained with calcein-AM and propidium iodide (PI, Figure 5). The results further demonstrated the synergetic effect.

Before realizing bioapplication, the Cu²⁺ release of Cu₇S₄@SiO₂ nanoparticles in PBS was evaluated because of Cu²⁺ being toxic. It was revealed that the concentration of the released Cu²⁺ from Cu₇S₄@SiO₂ nanoparticles was very low (**Supplementary Figure S5**), which caused almost no toxicity. We then evaluated the toxicity *in vivo* of Cu₇S₄@SiO₂. In the experimental group, the material was injected intravenously into mice, while mice in the control group were injected with PBS.



1064 nm NIR laser at the power density of 0.6 Wcm⁻². (b) The temperature curves showing the temperature change in tumor area.



FIGURE 7 | (A) The relative tumor volumes of mice after different treatments over a period of 14 days. (B) The body weight of mice in these groups. (C) The typical photographs of mice at the 14th day.



FIGURE 8 | The typical images of tumor slices stained with H&E assay for (a) $Cu_7S_4@SiO_2/DOX+NIR$ group, (b) $Cu_7S_4@SiO_2+NIR$ group, (c) DOX group, and (d) Control group.

After a month, HE analysis of the main organs of mice in the two groups showed no significant difference (**Supplementary Figure S6**). To perform photothermal-chemo therapy of tumors,

mice bearing with melanoma tumor were randomly allocated into four groups as follow: (1) The control group; (2) DOX group; (3) $Cu_7S_4@SiO_2+NIR$ group; (4) $Cu_7S_4@SiO_2/DOX+NIR$ group. The mice in (2) group were intratumorally injected with DOX PBS solution (50 µL, 80 µg), and mice in (3 and 4) group were intratumorally injected with Cu₇S₄@SiO₂ (50 µL, 0.1 mg mL⁻¹) and Cu₇S₄@SiO₂/DOX PBS solution (50 µL, 0.1 mg mL⁻¹). Figure 6a shows the typical thermal image of mice with the tumor area exposed to a 1064 nm NIR laser (0.6 Wcm⁻²), in which the tumor treated with Cu₇S₄@SiO₂/DOX shows the bright red while the tumor received PBS exhibits the normal color. The surface temperature of tumor treated with Cu₇S₄@SiO₂/DOX increases from ~34.2°C to the balanced \sim 57.9 °C at 300 s, resulting in temperature elevation of 23.7 °C which was much higher than that (3.5°C) for the tumor received PBS (Figure 6b). Thus, the Cu₇S₄@SiO₂/DOX within tumor remain high photothermal conversion effect, which can convert 1064 nm NIR laser energy into enough heat to thermally ablate cancer cells.

After different treatments, mice in all groups were raised under the standard condition for the long-term observation of cancer treatment efficacy. The tumor sizes and body weights were recorded. The change of relative tumor volumes is demonstrated in **Figure 7A**. Obviously, the tumor volume in the control group increases greatly which was five times the initial volume. For the tumors in the DOX group and Cu₇S₄@SiO₂+NIR group, their growth has been inhibited, due to the cytotoxicity of DOX for DOX group and the photothermal therapy for Cu₇S₄@SiO₂+NIR group. Interestingly, in the case of the tumors in the Cu₇S₄@SiO₂/DOX+NIR group, their volume goes down continuously with the significant inhibition efficiency compared to the other three groups. The high inhibition efficiency should be due to the synergistic photothermal-chemo effect from the combination of Cu₇S₄@SiO₂/DOX and NIR laser irradiation. On the one side, the photothermal therapy can instantly kill part of cancer cells through high temperature, and on the other side, the load DOX within Cu₇S₄@SiO₂/DOX can continuous release to kill the remaining cancer cells, thus achieving the synergistic effect on melanoma tumors. In addition, there was no any sign of loss in body weight for all groups (Figure 7B). Therefore, the satisfactory inhibition efficiency can be realized from the synergistic photothermal-chemo therapy by the combination of Cu₇S₄@SiO₂/DOX and 1064 nm NIR laser, while no obvious side effect for mice.

Furthermore, mice in all groups were sacrificed when a tumor size was beyond 1.0 cm (Figure 7C). The tumors were extracted for the sacrificed mice, which were embedded in paraffin and crysectioned into slices. After stained with H&E assay, the tumor slices were imaged for histological examination. Figure 8 manifests the typical morphology of tumor cells, and the cancer cells shows the normal and complete morphology in regard to the cell size, shape and nuclear. The significant cell damage is noticed for Cu₇S₄@SiO₂/DOX+NIR group (Figure 8a), including the destroyed cell membranes and the condensed nucleus. For the tumor cells in the Cu7S4@SiO₂+NIR group (Figure 8b) and DOX group (Figure 8c), there are some cells showing the destroyed morphology, indicating the limited therapeutical effect through photothermal therapy or chemotherapy. On the contrary, the cell size and shape showed no difference in the control group (Figure 8d). The above histological examination solidly verifies the higher therapeutical effect of photothermalchemo therapy than photothermal therapy or chemotherapy.

CONCLUSION

In summary, we prepared the $Cu_7S_4@SiO_2/DOX$ and used them as efficient nanoplatforms for synergistic photothermalchemo therapy on melanoma tumors. The $Cu_7S_4@SiO_2/DOX$ was prepared by firstly synthesizing Cu_7S_4 nanocrystals, then *in situ* growing SiO_2 shell on the surface of Cu_7S_4 nanocrystals, and finally loading DOX. The $Cu_7S_4@SiO_2$ consisted of Cu_7S_4 core with the average diameter of 50 nm and SiO_2 shell with the average thickness of 25 nm. The $Cu_7S_4@SiO_2$ nanoplatforms

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Cheng, L., Wang, C., Feng, L., Yang, K., and Liu, Z. (2014). Functional nanomaterials for phototherapies of cancer. *Chem. Rev.* 114, 10869–10939. doi: 10.1021/cr400532z exhibited the strong and broad NIR absorption and rapidly converted 1064 nm laser energy into heat, and they also demonstrated high specific surface area and a large amount of pores with high DOX-loading content of 59.8%. Importantly, under the irradiation of 1064 nm laser, $Cu_7S_4@SiO_2/DOX$ simultaneous generated heat and accelerated the DOX release. Give these advantages, mice were intratumorally injected with $Cu_7S_4@SiO_2/DOX$ and irradiated with1064 nm laser, which achieved the highest therapeutical effect through synergistic photothermal-chemo therapy compared to photothermal therapy or chemotherapy alone. Therefore, the $Cu_7S_4@SiO_2/DOX$ can be served as novel and efficient photothermal-chemo nanoagents for efficient tumor therapy.

DATA AVAILABILITY STATEMENT

All datasets presented in this study are included in the article/**Supplementary Material**.

ETHICS STATEMENT

The animal study was reviewed and approved by the Ninth People's Hospital, Shanghai Jiao Tong University School of Medicine.

AUTHOR CONTRIBUTIONS

LZ and HP contributed equally to this work. LZ, HP, and XH designed the project and wrote the manuscript. LZ, HP, and YL carried out the experiment. LZ and FL performed the experimental data analysis. All the authors contributed to discussion of the results.

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SUPPLEMENTARY MATERIAL

The Supplementary Material for this article can be found online at: https://www.frontiersin.org/articles/10.3389/fbioe. 2020.579439/full#supplementary-material

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Conflict of Interest: The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

The reviewer XH declared a shared affiliation, with no collaboration, with the authors to the handling editor.

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