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Hemostatic resuscitation is an essential aspect of treating traumatic bleeding. Trauma-induced coagulopathy is a multifactorial disorder that can lead to increased transfusion requirements. However, little is known about the interplay between coagulopathies and stored blood products used for hemostatic resuscitation, which themselves acquire dysfunction in the form of a storage lesion. Physiologically relevant models can aid in the study of trauma and hemostatic resuscitation by incorporating important aspects such as biological surfaces and flow regimes that mimic injury. This study aims to evaluate the contribution of platelet products under varying storage conditions in coagulopathic states. This study utilized microfluidic platforms of high shear, a flow regime relevant to injury, including a stenotic straight channel and a severe transected vessel injury device. Apheresis platelet products were collected from healthy volunteers, stored at room temperature (RT) or coldstored (CS)  $(1^{\circ}C-6^{\circ}C)$ , and tested for product cell count and intrinsic product function in a high-shear stenotic microfluidic device across storage days (D2, D5, and D7 for RT; D2, D5, D7, D14, and D21 for CS). Hemostatic resuscitation efficacy of products was assessed using induced coagulopathy models of dilution and thrombocytopenia (TP). In vitro hemostatic resuscitation was assessed in both the stenotic straight channel for kinetic platelet contributions and the transectedvessel injury device, using blood loss and clot composition as endpoints. CS products conserved inherent function despite decreasing platelet counts through storage D7. When mixed with coagulopathic blood, D2 RT products did not show hemostatic benefit in the dilutional coagulopathy (DC) model. However, both D2 RT and CS showed hemostatic benefits in the thrombocytopenia model. CS products (D5 and D7) also showed an enhanced ability to recruit recipient platelets in the thrombocytopenia model compared to RT. Overall, this study highlights disparate responses associated with product storage duration and

temperature, indicating the need to further evaluate hemostatic resuscitation efficacy under flow in pathologically relevant models to guide transfusion practices.

KEYWORDS

platelets, resuscitation, coagulopathy, hemostasis, cold-stored platelets

# **1** Introduction

Hemorrhagic shock due to excessive blood loss is a leading cause of death in trauma patients, accounting for up to 1.5 million deaths worldwide each year (Lozano et al., 2012). The traumatic injury response is complex [reviewed by Moore et al. (2021) and Vulliamy et al. (2021)], with both adaptive and maladaptive aspects. Consumption of clotting factors, hypocoagulability, hyperfibrinolysis, and iatrogenic resuscitation-associated coagulopathies (e.g., dilution) can perpetuate a lack of clotting response, leading to trauma-induced coagulopathy (Kushimoto et al., 2017; Moore et al., 2021). Additionally, platelet dysfunction after injury is a key component of trauma-induced coagulopathy (Kutcher et al., 2012; Vulliamy et al., 2020; Sloos et al., 2022).

Early hemostatic resuscitation following trauma is associated with improved survival (Sperry et al., 2018; Torres et al., 2024), and specifically, early platelet transfusion is critical (Gunter et al., 2008; Holcomb et al., 2008). However, stored blood components acquire a storage lesion, which results in products with their own unique coagulopathy and manifests in reduced hemostatic function as storage progresses (Cap, 2017; Shea et al., 2019). It remains to be studied how blood products, along with their acquired dysfunction during storage, interact with patient hemostatic function in the context of trauma-induced coagulopathy.

In vitro and ex vivo models that incorporate critical aspects of hemostasis are especially valuable for the functional evaluation of trauma-induced coagulopathies and blood product function. Fluid dynamics play a critical role in the mechanisms underlying hemostasis and thrombosis. Therefore, this study evaluated a severe injury model with a transected vascular channel for physiological relevance to the severely injured bleeding patient (Yakusheva et al., 2022). High-shear flow was evaluated throughout this study as cellular functions under high shear are of critical importance for hemostasis, especially for platelets undergoing shear-induced platelet activation and interaction with the von Willebrand factor (Andrews et al., 1997; Shankaran et al., 2003; Colace and Diamond, 2013; Zhang et al., 2022).

Cold-stored (CS) platelet products have logistical benefits compared to storage at room temperature (RT), including increased shelf life (Shea et al., 2024). CS platelets also may have better hemostatic function than RT products (Reddoch et al., 2014; Reddoch-Cardenas et al., 2019; D'Alessandro et al., 2020; Shea et al., 2022; George et al., 2023). The platelet storage lesion is modulated by temperature [reviewed by Hegde et al. (2018), Ng et al. (2018), and Shea et al. (2019)]. In RT-stored platelets, a progressive reduction in mitochondrial function occurs over time, along with the release of extracellular vesicles, granules, and other soluble mediators (e.g., CD40L) and increased CD62P expression (Shea et al., 2019). CS platelets have improved bioenergetics (Johnson et al., 2016; D'Alessandro et al., 2020; George et al., 2023; Shea et al., 2024); however, cold stimuli cause irreversible changes to the platelet cytoskeleton (Winokur and Hartwig, 1995; Hoffmeister et al., 2001; Hegde et al., 2024), resulting in increased surface expression of CD62P, GMP140, and CD40L and increased granule mobilization (Triulzi et al., 1992; Wood et al., 2016; Shea et al., 2019, 2024). Although CS results in the aforementioned improved *in vitro* hemostatic function and longer shelf life, the impact of the CS phenotype *in vivo* in hemostatic resuscitation remains unclear.

Simulated hemostatic resuscitation using platelet products stored under different durations and temperatures may help improve our understanding, thereby informing current transfusion practices and supporting the development of improved therapeutic approaches and novel therapies. This study evaluated platelet function over product storage duration and temperature in the context of trauma-induced coagulopathy. We hypothesized that platelet products used in clinical transfusion would rescue hemostatic function in models of trauma-induced coagulopathy, including increased platelet deposition and reduced blood loss, and CS platelets would have sustained efficacy over storage compared to RT platelets.

# 2 Materials and methods

The studies involving human participants were reviewed and approved by the University of Pittsburgh Human Research Protection Office (IRB 21110093 and 21100141). Participants provided their written informed consent to participate. Inclusion and exclusion criteria for apheresis platelet and whole blood (WB) samples are listed in supplementary materials.

### 2.1 Platelet unit collection

All platelet products were collected from healthy donor volunteers via apheresis, following the standards of the Association for the Advancement of Blood and Biotherapies (AABB) and US Food and Drug Administration (FDA), and suspended in anticoagulant citrate dextrose solution A (ACD-A) and plasma, using the Trima Accel automated blood collection system. Platelet units were randomly assigned to CS or RT storage. RT platelets were stored with gentle agitation. CS platelets were stored between 1°C and 6°C without agitation. The agitation of RT platelets and no agitation of CS platelets are consistent with current blood banking practices in the US, and we have previously demonstrated that agitation makes no difference in RT or CS storage with respect to functionality (Shea et al., 2022). Aseptic sampling was conducted on days D2, D5, and D7 for RT products and D2, D5, D7, D14, and D21 for CS products for subsequent testing (Figure 1A). A complete blood count (ADVIA 2120i Hematology System, Siemens) and high-shear stenotic microfluidic assays on products alone were performed prior to



paired and unmanipulated whole blood controls (WB). (B) Schematic representation of the stenotic straight channel microfluidic device with assembly, dimensions, and coating used to assess inherent product platelet function with growing thrombus in the stenotic region; increasing pressure monitored inline and upstream of the device. (C) Platelet counts in RT (red circles) and CS (blue squares) platelet products over their storage duration. (D) Occlusion time based on a pressure threshold of 75 mmHg from the stenotic straight channel device in both RT (red circles) and CS (blue squares) platelet products over their storage duration. Dotted line represents an assay cap of 60 min. (E) Representative pressure curves from RT and (F) CS products are shown. Data are presented as mean  $\pm$  standard deviation or individual values with bars representing mean  $\pm$  standard deviation. Occlusion time data were analyzed via multiple unpaired t-tests. \*p < 0.05.

*in vitro* resuscitation experiments. A total of eight biological replicate RT units were collected and tested on D2 with dilutional coagulopathy (DC). For extended storage studies, a total of four biological replicate RT units and three biological replicate CS units were collected and tested with thrombocytopenia (TP) coagulopathy. Sampling of each product over the storage period led to a sample size of 12 for RT products and 15 for CS products.

# 2.2 Whole blood collection for simulated *in vitro* hemostatic resuscitation with platelet products

Whole blood was collected from healthy volunteer donors via venipuncture into heparin, citrate, and EDTA vacutainers. Blood samples from these donors were used as a "recipient" for modeling transfusion through *in vitro* mixing with platelet products.

Complete blood counts were performed on the healthy sample using the EDTA aliquot prior to any further processing to confirm healthy volunteer donors had normal platelet counts. The high-shear stenotic microfluidic assay, also used on product alone, and a microfluidic transection injury assay were performed on mixed samples using citrated and heparinized whole blood respectively. Paired WB, induced coagulopathy [DC or TP], and induced coagulopathy mixed with platelet product samples were run on D2, D5, and D7 for RT products and D2, D5, D7, D14, and D21 for CS products. Dose responses of the coagulopathy models were conducted and assessed for platelet count, platelet aggregometry, and rotational thromboelastometry (ROTEM), according to the manufacturer's instructions for extrinsic pathway activation (EXTEM).

# 2.3 Stenotic microfluidic assay for the inherent platelet product function

A stenotic microfluidic device was fabricated as previously described (Mihalko et al., 2024). Channel height and width were measured on the resulting PDMS cast (Bruker DektakXT Surface Profiler and Zeiss Zen). Channel dimensions were 40  $\pm$  3  $\mu$ m in height and 462  $\pm$  3  $\mu$ m in width at the stenotic region and 137  $\pm$  4  $\mu$ m in height and  $462 \pm 3 \,\mu\text{m}$  in width at the inlet and outlet. The device was coated with collagen using a 5:1 volumetric ratio of normal saline and collagen (Chrono-par collagen reagent, Chrono-log Corporation) for 1 hour at RT. It was then rinsed with phosphate-buffered saline, incubated with 5% bovine serum albumin for 30 min, rinsed again with phosphate-buffered saline, and stored in a humid environment prior to use. Platelet products were infused through the channel at high shear rates (3,500 s<sup>-1</sup>) using a syringe pump (Harvard Apparatus, PHD Ultra), with upstream calcium addition using a second syringe pump (10 mM final concentration). Time to occlusion was determined using an upstream pressure monitor, with a 75 mmHg pressure increase set as the threshold for occlusion.

# 2.4 Transected injury microfluidic device fabrication

A transected vessel injury microfluidic device mold was fabricated using photolithography with a channel height of 100  $\mu$ m throughout and a channel width of 300  $\mu$ m at the vessel injury region, 1800  $\mu$ m at the inlet, and 2000  $\mu$ m at the outlet (i.e., extravascular region). An EDTA channel was positioned prior to the device outlet to quench downstream coagulation via a constant flow of EDTA (50 mM) using a syringe pump (8  $\mu$ L/min) to ensure legitimate occlusion is captured at the site of interest (Berry et al., 2021). The device was coated with collagen and tissue factor (Dade Innovin, Siemens) for 1 hour at RT, rinsed with phosphate-buffered saline, then incubated with 5% bovine serum albumin for 30 min, rinsed again with phosphate-buffered saline, and stored in a humid environment prior to use.

# 2.5 Functional assessment of simulated hemostatic resuscitation

For stenotic microfluidic experiments, platelet product aliquots were incubated with Fc receptor block (Biolegend; Human TruStain FcX; 422302; 1:600) and fluorescently tagged CD41 antibody (Janelia Fluor<sup>®</sup> 646) (Novus Biologicals; NB100-2614JF646; 1:600). Citrated whole blood was incubated with Fc receptor block (1:600) and a distinct fluorescently tagged CD41 antibody (Janelia Fluor<sup>®</sup> 549) (Novus Biologicals; NB100-2614JF549; 1:600). DC was induced by combining whole blood with sterile normal saline in a 2:3 volumetric ratio. TP samples were induced via centrifugation. In brief, whole blood was centrifuged at  $100 \times g$  for 10 min with no brake. The platelet-rich plasma (PRP) layer was then removed and further centrifuged at  $800 \times g$  for 10 min with no brake. Platelet-poor plasma (PPP) obtained from the second spin was mixed with red blood cells saved from the first spin to create a thrombocytopenic blood sample. The platelet product was mixed with coagulopathic blood in a 1:5 volumetric ratio, equivalent to the transfusion of four platelet units. A complete blood count was performed for TP samples and TP samples mixed with platelet products. All blood samples were perfused under constant flow using a withdrawal syringe pump at an initial wall shear rate of 3,500 s<sup>-1</sup> at the stenosis throat, consistent with high-shear injury (Yakusheva et al., 2022). Kinetic immunofluorescent images were captured using an Axio Observer inverted microscope (Zeiss) at 10× magnification as clot formation progressed (0.29 frames/ second) under room temperature conditions. MATLAB software was used to quantify platelet deposition. Mean fluorescent intensity (MFI) was determined for each image frame and each color channel to quantify the amount of corresponding fluorescently labeled platelets deposited in the channel. MFI curves generated demonstrate platelet kinetics over the length of the experiment.

For the microfluidic experiment modeling vessel transection hemostatic capacity, platelet product aliquots were incubated with Fc receptor block (1:600) and fluorescently tagged CD41 antibody (Janelia Fluor® 646) (Novus Biologicals; NB100-2614JF646; 1:600). Heparinized whole blood was incubated with Fc receptor block and a distinct fluorescently tagged CD41 antibody (Janelia Fluor<sup>®</sup> 549) (Novus Biologicals; NB100-2614JF549; 1:1,200). Coagulopathies were induced as mentioned above. Platelet products were mixed with coagulopathic blood in a 1:5 volumetric ratio, simulating a volumetric transfusion of approximately four platelet units in an adult. Blood samples were perfused under constant pressure (20 mmHg) via gravity, resulting in a pathologically high shear regime at the point of transection (~9,500 s<sup>-1</sup>), again consistent with high shear conditions associated with injury (Yakusheva et al., 2022). Device outflow was monitored using a scale and LabVIEW software, yielding a blood loss endpoint. Immunofluorescent images were captured at 10× magnification using an Axio Observer inverted microscope (Zeiss) (0.1 frames/ second) at room temperature conditions. ImageJ software was used for platelet area quantification.



### 2.6 Statistical analysis

All statistical analysis was performed using GraphPad Prism 10 (GraphPad, San Diego, CA). Data were analyzed using an unpaired t-test for inherent product function, a paired t-test for coagulopathy blood loss, and mixed-effects analysis or one-way analysis of variance (ANOVA) with correction for multiple comparisons using an Tukey's post hoc test with a 95% confidence interval for hemostatic resuscitation mixing studies. An unpaired t-test was conducted comparing early and late storage age blood loss. To identify outliers in platelet area data, the ROUT method—combining robust regression and outlier removal—was used, with the false discovery rate (Q) set at 1%. One outlier was identified and removed prior to analysis using an unpaired t-test. MFI fold-change curves are presented as mean  $\pm$  standard error of the mean. All other data are presented as mean  $\pm$  standard deviation. Data from product assessment and *in vitro* hemostatic resuscitation endpoints in the TP model were subjected to a Pearson's correlation coefficient analysis.

# **3** Results

# 3.1 Platelet product cell count and function over storage

Platelet counts from RT and CS platelet products are shown in Figure 1C. RT products had consistent platelet counts over storage, whereas CS products decreased platelet count following D2. Intrinsic product function evaluated in the straight stenotic microfluidic channel (Figure 1B) showed a significant reduction in occlusion time (i.e., faster

clot formation) with CS products compared to that with RT products at D7 (Figure 1D). Representative pressure curves from intrinsic product function testing (Figure 1E,F) illustrated conserved hemostatic function from CS products at D2, D5, and D7, which subsequently decreased at D14 and D21. Comparatively, RT products precipitously decreased in hemostatic activity over storage.

# 3.2 *In vitro* hemostatic resuscitation in a stenotic microfluidic device

Dose responses of dilutional coagulopathy revealed significantly impaired clotting parameters at a 2:3 volumetric ratio (i.e. 40% whole blood) on ROTEM and reduced platelet aggregometry (Supplementary Figure S1). Thrombocytopenia dose responses reached an average platelet count of  $70 \times 10^3$  cells/µL when 100% of platelets from isolated PRP were removed, with a less severe but statistically significant impairment in clotting parameters observed on ROTEM (Supplementary Figure S1).

The stenotic microfluidic device, which showed robust platelet deposition in the stenotic region in whole blood controls (Figure 2A), demonstrated substantial hemostatic dysfunction in DC and TP coagulopathic samples, as measured in fold change of CD41 MFI (Figure 2B). In paired WB and coagulopathy with or without hemostatic resuscitation experiments, RT D2 platelet products did not improve either the occurrence of substantial thrombus formations or recipient platelet deposition (CD41<sub>recipient</sub>) in the DC model (Figures 2C,D). Additionally, although RT products significantly enhanced platelet count



recovery upon *in vitro* hemostatic resuscitation in the TP model compared to CS products (Supplementary Figure S2), RT products did not improve thrombus formation occurrence (54% in TP versus 31% in TP + RT (D2-7)) or recipient platelet deposition (CD41<sub>recipient</sub>) (Figures 2E,F) in the TP coagulopathy model. A similar trend was observed with CS products in the TP model, with substantial thrombus formation in 56% of TP versus 22% of TP + CS (D2-7) and no improvement in recipient platelet deposition (CD41<sub>recipient</sub>) compared to coagulopathy (Figures 2G,H).

Platelet deposition of both CD41<sub>recipient</sub> and CD41<sub>product</sub> for TP recipient samples mixed with RT and CS platelet products are shown in Figure 3 from stenotic microfluidic experiments. When stratified by storage duration, both RT and CS CD41<sub>product</sub> were highest at D2, surpassing D5 and D7. Additionally, both RT and CS CD41<sub>recipient</sub> were highest at D2. Minimal kinetic MFI differences at D5 and D7 were observed.

# 3.3 *In vitro* hemostatic resuscitation in the transected injury microfluidic device

In the transected microfluidic device (Figure 4A), clots formed in the vascular channel portion of the device with a

high platelet content (Figure 4B). WB samples had an average blood loss of  $1.301 \pm 0.489$  g compared to DC with  $2.883 \pm 1.032$  g blood loss (paired samples, p < 0.01) and TP with  $1.540 \pm 0.374$  g blood loss (paired samples, p < 0.05) (Figure 4C). Mass outflow curves (Figure 4D) illustrated reduced flow over 20 min as a clot formed in WB samples. RT platelet products at D2 did not reduce DC blood loss ( $2.883 \pm 1.032$  g DC compared to  $2.661 \pm 0.8362$  g DC + RT), and both coagulopathy samples and coagulopathy samples mixed with platelet products had significantly higher blood loss than WB controls (p < 0.01 for both) (Figure 4E).

The ability of platelet products of varying storage age and temperature to elicit a hemostatic effect in a hemostatic resuscitation model was further evaluated in the transected injury microfluidic device with paired donor TP samples. Representative clot images illustrated robust clot formation with recipient platelets (CD41<sub>recipient</sub>, blue) in the microfluidic device that was persistent in the TP model (Figure 5A). Upon mixing platelet products with the TP samples, distinct populations of recipient platelets (CD41<sub>recipient</sub>, blue) and product platelets (CD41<sub>product</sub>, red) were observed in the formed clot. Together, RT and CS platelet products did not reduce TP blood loss (1.540  $\pm$  0.374 g TP



FIGURE 4

Transected injury microfluidic device assessed blood loss with coagulopathy models to evaluate hemostatic resuscitation. (A) Top-down view schematic representation of the transection injury microfluidic device with assembly, dimensions, and coatings used to assess *in vitro* hemostatic resuscitation. (B) Representative image of the clot formed in the vascular channel region of the microfluidic device (platelets, CD41, white). (C) Blood loss from healthy controls (WB) and DC and TP samples measured via endpoint microfluidic outflow. Data were analyzed via two paired t-tests comparing paired WB controls within each coagulopathy model. \*p < 0.05; \*\*p < 0.01. (D) Hemostatic resuscitation with RT platelet products at D2 were evaluated with mass outflow curves shown and (E) corresponding endpoint microfluidic outflow. Data were analyzed via mixed-effects analysis and Tukey's post hoc test using a 95% confidence interval. \*\*p < 0.01. All data are presented as mean  $\pm$  standard deviation or individual values with bars representing mean  $\pm$  standard deviation.

compared to 1.790  $\pm$  0.430 g TP + RT/CS), and both the coagulopathy sample and coagulopathy mixed with platelet product had significantly higher blood loss than WB controls (p < 0.05 and p < 0.001, respectively) (Figure 5B). TP + RT platelet product samples, compared to paired coagulopathic TP samples, did not have significantly different blood loss. However, TP + CS platelet product samples had significantly higher blood loss than paired coagulopathic TP samples (1.395  $\pm$  0.312 g TP compared to 1.838  $\pm$  0.320 g TP + CS (D2-21), p < 0.01) (Figures 5C,D). When comparing storage age, D2 products resulted in the lowest blood loss under both storage temperature conditions (1.378  $\pm$  0.492 g with D2 RT and CS products compared to 1.988  $\pm$  0.280 g with D5 and D7 RT and CS products, p < 0.01) (Figures 5E,F).

# 3.4 Recipient platelet and product platelet incorporation following *in vitro* hemostatic resuscitation

Endpoint clot composition in the microfluidic transection model is shown in Figure 6. A representative TP + RT (D2) z-stack image is shown (Figure 6A) with distinct populations from recipient and product platelets observed. When stratified by D5 and D7 where CS products had higher intrinsic hemostatic function on their own, no significant difference in platelet product area (CD41<sub>product</sub>) was observed (Figure 6B). However, a statistically significant increase in recipient platelet area (CD41<sub>recipient</sub>) was observed in CS platelets compared to the RT platelets (p < 0.001), along with an increased ratio of recipient



#### FIGURE 5

RT and CS products assessed in the thrombocytopenia model in the transected injury microfluidic device. (A) Representative images from paired healthy control (WB), TP sample, and TP sample mixed with platelet product are shown. TP sample platelets (CD41<sub>recipient</sub>, blue) and product platelets (CD41<sub>product</sub>, red). (B) Blood loss measured via endpoint microfluidic outflow from hemostatic resuscitation experiments combining storage temperature and age. Data were analyzed via mixed-effects analysis and Tukey's post hoc test using a 95% confidence interval. \*p < 0.05; \*\*\*p < 0.001. (C,D) Blood loss segmented by storage temperature. RT product data were analyzed via mixed-effects analyzed via aNOVA and Tukey's post hoc test using a 95% confidence interval. Cold-storage product data were analyzed via ANOVA and Tukey's post hoc test using a 95% confidence interval. \*\*p < 0.01. (E) Blood loss from TP + RT/CS samples stratified by storage age. (F) Blood loss compared in early-storage (D2) versus late-storage (D5 and D7) products. Early-versus late-storage age data were analyzed via an unpaired t-test. \*\*p < 0.01. All data are presented as mean  $\pm$  standard deviation or individual values, with bars representing mean  $\pm$  standard deviation.



#### FIGURE 6

Endpoint thrombus composition in the transected injury microfluidic device. (A) Representative image from the TP sample resuscitated with RT platelet products at D2 is shown. TP sample platelets ( $CD41_{recipient}$ , blue) and product platelets ( $CD41_{product}$ , red). (B)  $CD41_{product}$  area quantification and (C)  $CD41_{recipient}$  area quantification are shown highlighting storage at D5 and D7. (D) Calculated ratio of  $CD41_{recipient}$  over  $CD41_{product}$  area is shown for all storage days. \*\*\*p < 0.001. All data are presented as individual values, with bars representing mean  $\pm$  standard deviation.

platelets to product platelets across all storage days Figure 6 C, D. Both the recipient and product platelet areas from the transection device and recipient and product platelet MFI endpoints from the stenotic device positively correlated with each other and negatively correlated with transection device blood loss (Supplementary Figure S3).

### 4 Discussion

This study establishes microfluidic platforms that can be used to assess intrinsic product function and hemostatic resuscitation efficacy. In both a stenotic device and a transected injury device, disparate responses with product storage duration were observed. The stenotic device has a simpler design that could be considered closer to a point-ofcare possibility, while the transection model is a direct analog to vessel injury in trauma. Further probing of clot composition with respect to recipient and product platelets illustrates disparate responses with product storage temperature.

CS platelets showed increased intrinsic hemostatic function compared to RT platelets, regardless of decreasing platelet count in the product and reduced platelet count recovery in in vitro hemostatic resuscitation. This is consistent with a large number of studies in the literature demonstrating increased intrinsic platelet function due to the cold-induced cytoskeletal changes that result in a pro-hemostatic phenotype during CS (Reddoch et al., 2014; Reddoch-Cardenas et al., 2019; Shea et al., 2019; D'Alessandro et al., 2020; George et al., 2023), and specifically, our group (Shea et al., 2024) and others (Montgomery et al., 2013) have shown increased intrinsic product function under flow in CS versus RT platelets. There is little data regarding the direct effects of platelet storage on platelet-endothelial interactions and endothelial function; however, there is evidence that RT platelets can induce the release of soluble mediators from the endothelium and alter its surface marker expression in vitro, which increases with storage time (Urner et al., 2012; Baimukanova et al., 2016b; Sut et al., 2018). Some in vivo studies also demonstrated the protective effects of RT platelets, which again decrease over the course of storage (Sut et al., 2018). There are very few studies investigating CS platelet-endothelial interactions, although data generated so far show that CS platelets are less effective at preventing endothelial permeability in vivo than their RT counterparts (Baimukanova et al., 2016a, p. 22; Miyazawa et al., 2023). Future studies are essential to fully understand the effects of platelet manufacturing approaches and storage conditions on hemostatic, immune, and endothelial function.

The enhancement of *in vitro* hemostatic resuscitation function with CS platelet products was not clearly observed in the stenotic microfluidic device. However, a correlation of the product cell count to the ratio of recipient to product platelet area in the transection device was observed (Supplementary Figure S3). In addition, an enhancement in platelet count recovery, while positively correlated with the product cell count, was also positively correlated with intrinsic product occlusion time (i.e., enhanced platelet count recovery correlates with an increased clotting time or reduced platelet function under flow), supporting the need for further assessment of blood products to accurately evaluate or predict hemostatic function (Supplementary Figure S3). Overall, the direct assessment of blood products and their hemostatic resuscitation efficacy in this study, is a step toward precision transfusion medicine approaches. These data support the consideration of clinical platelet storage policies that prioritize early storage products, when hemostatic activity is at its peak, for trauma patients at risk of developing coagulopathy.

Limitations of this study include a lack of endothelial response. However, our focus was on platelet hemostatic dysfunction, and specifically high-shear hemostatic function under flow, relevant to traumatic injury. Future studies investigating concomitant endothelial and hemostatic effects are warranted, along with the critical roles of other blood cell types, including erythrocytes and immune cells such as neutrophils and monocytes. Additionally, validation of the microfluidic device against in vivo clot formation will be investigated in future work. Cold-storage effects on platelet signaling pathways in mixing studies (specifically GPVI and GPIba) and their implications for recipient hemostasis should also be explored. There is precedent for potential confounding factors in this study, such as platelet donor variability and high variability in assessing function under flow (Fiedler et al., 2020; Shea et al., 2024). Another limitation of this study is a lack of recovery toward healthy control responses upon platelet product mixing in the coagulopathic models examined. Whether this reflects a dilutional effect of product addition to an already coagulopathic blood sample or a deleterious storage lesion effect on hemostatic function remains to be determined.

Pathologically relevant models to assess hemostatic function and resuscitation strategies *in vitro/ex vivo* are critical for highthroughput preclinical investigations. Innovation in this space may ultimately improve outcomes related to trauma and transfusion medicine. A deeper understanding of platelet dysfunction in trauma and the effects of platelet-containing blood products will aid in more accurately modeling coagulopathies in future studies and the interpretation of model outputs. Disparate responses to product storage conditions evaluated in this study may help guide transfusion practices based on functional assessments of blood loss, which were lowest at early storage time points, along with the assessment of recruited recipient platelets in CS platelet products.

### Data availability statement

The original contributions presented in the study are included in the article/Supplementary Material, further inquiries can be directed to the corresponding author.

### Ethics statement

The studies involving humans were approved by the University of Pittsburgh Human Research Protection Office (IRB #21110093 and #21100141). The studies were conducted in accordance with the local legislation and institutional requirements. The participants provided their written informed consent to participate in this study.

# Author contributions

EM: conceptualization, formal analysis, investigation, methodology, project administration, supervision, visualization, writing – original draft, and writing – review and editing. RM: data curation, formal analysis, investigation, methodology, validation, and writing – review and editing. DD: data curation, formal analysis, investigation, methodology, validation, and writing – review and editing. SC: data curation, investigation, project administration, validation, and writing – review and editing. SS: conceptualization, funding acquisition, investigation, project administration, resources, supervision, visualization, writing – review and editing.

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# Conflict of interest

The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

# Generative AI statement

The author(s) declare that no Generative AI was used in the creation of this manuscript.

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# Supplementary material

The Supplementary Material for this article can be found online at https://www.frontiersin.org/articles/10.3389/fbioe.2025.1568113/ full#supplementary-material

#### SUPPLEMENTARY FIGURE S1

Coagulopathy model dose response. (A–G) Dilutional coagulopathy model dose response in citrated blood samples measured via (A) complete blood counts for platelet concentration, (B) whole blood impedance aggregometry with 10  $\mu$ M ADP agonist and ROTEM EXTEM (C) clotting time, (D) clot formation time, (E) maximum clot firmness, (F) alpha angle, and (G) lysis index at 60 min. Dilutions of WB in sterile normal saline were examined from 100% WB and 0% saline to 25% WB and 75% saline. (H–N) Thrombocytopenia model dose response in citrated blood samples measured via (H) complete blood counts for platelet concentration, (I) whole blood impedance aggregometry with 10  $\mu$ M ADP agonist and ROTEM EXTEM (J) clotting time, (K) clot formation time, (L) maximum clot firmness, (M) alpha angle, and (N) lysis index at 60 min. Various centrifugation preparations of PRP (25% of PRP platelets removed to 100% of PRP platelets removed) were conducted for the decreasing platelet count.

#### SUPPLEMENTARY FIGURE S2

Platelet count recovery. Platelet counts from citrated thrombocytopenia coagulopathy samples before and after simulated transfusion with RT (D2-7) and CS (D2-21) platelet products are shown. Data are presented as individual values with bars representing mean  $\pm$  standard deviation. Data were analyzed via one-way analysis of variance (ANOVA) and Tukey's post hoc test using a 95% confidence interval. \*p < 0.05; \*\*p < 0.01; \*\*\*\*p < 0.001; \*\*\*\*p < 0.001.

#### SUPPLEMENTARY FIGURE S3

Correlation analysis of platelet product assessment and *in vitro* resuscitation. The correlation matrix indicates positive (purple) and negative (orange) Pearson's correlation coefficient values. \*p < 0.05; \*\*p < 0.01; \*\*\*p < 0.001.

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