



## OPEN ACCESS

## EDITED BY

Rino Frisina,  
Guglielmo da Saliceto Hospital, Italy

## REVIEWED BY

Brian D. Lawrence,  
Silk Technologies, Ltd., United States  
Ignacio Alcalde,  
Instituto Universitario Fernández-Vega, Spain  
Giovanni Casini,  
University of Pisa, Italy

## \*CORRESPONDENCE

Daniel E. Savage  
✉ Daniel.Savage@hsc.utah.edu

<sup>†</sup>These authors have contributed equally to this work and share first authorship

<sup>‡</sup>Deceased

RECEIVED 19 October 2024

ACCEPTED 17 February 2025

PUBLISHED 20 May 2025

## CITATION

Savage DE, Tecse A, Zhou J, Germann JA, Buckley MR, Baratta RO, Del Buono BJ, Schlumpf E, Telias M and Marcos S (2025) Second-harmonic generation microscopy of murine scleral remodeling by collagenase and reparative collagen mimetic peptides. *Front. Med.* 12:1514073. doi: 10.3389/fmed.2025.1514073

## COPYRIGHT

© 2025 Savage, Tecse, Zhou, Germann, Buckley, Baratta, Del Buono, Schlumpf, Telias and Marcos. This is an open-access article distributed under the terms of the [Creative Commons Attribution License \(CC BY\)](https://creativecommons.org/licenses/by/4.0/). The use, distribution or reproduction in other forums is permitted, provided the original author(s) and the copyright owner(s) are credited and that the original publication in this journal is cited, in accordance with accepted academic practice. No use, distribution or reproduction is permitted which does not comply with these terms.

# Second-harmonic generation microscopy of murine scleral remodeling by collagenase and reparative collagen mimetic peptides

Daniel E. Savage<sup>1,2\*†</sup>, Aldo Tecse<sup>3,4†</sup>, Jiaxi Zhou<sup>4</sup>, James A. Germann<sup>4</sup>, Mark R. Buckley<sup>3,4</sup>, Robert O. Baratta<sup>5‡</sup>, Brian J. Del Buono<sup>5</sup>, Eric Schlumpf<sup>5</sup>, Michael Telias<sup>2,4</sup> and Susana Marcos<sup>4,5</sup>

<sup>1</sup>John A. Moran Eye Center, University of Utah, Salt Lake City, UT, United States, <sup>2</sup>Flaum Eye Institute, University of Rochester, Rochester, NY, United States, <sup>3</sup>Department of Biomedical Engineering, University of Rochester, Rochester, NY, United States, <sup>4</sup>Center for Visual Science, University of Rochester, Rochester, NY, United States, <sup>5</sup>The Institute of Optics, University of Rochester, Rochester, NY, United States

**Introduction:** Myopia, resulting from an excessive axial elongation of the eye, is increasing worldwide at alarming rates. This investigation is a pilot study to determine if a novel collagen mimetic peptide (CMP) has a reparative function for scleral collagen organization after collagenase digestion, a cause for scleral thinning and increased creep rates, as this may have application in the pharmacologic treatment of myopia.

**Methods:** Fresh, *ex vivo*, scleral tissue samples from 3 albino Sprague–Dawley rats (5 eyes) and from 8 C57/Black mice (8 eyes) underwent sequential collagenase digestion and treatment with a CMP solution. Full-thickness second-harmonic generation (SHG) microscopy was performed over a 200  $\mu\text{m}$   $\times$  200  $\mu\text{m}$  area through depth on each of the untreated samples (either scleral tissue samples or full intact eyes), and again after each sequential treatment. The organization of the collagen fibers at each tissue depth was quantified using a previously validated order coefficient (OC). This measure of collagen organization was then used to compare between the untreated, collagenase-digested, and CMP-treated tissue.

**Results:** SHG microscopy of the untreated scleral tissue showed a high degree of organization. Collagenase treatment resulted in a subjective straightening of the collagen fibers and a widening of the inter-fiber spacing with a statistically significant reduction of the OC ( $p < 0.05$ ). CMP treatment of digested sclera resulted in a collagen organization that was more similar (i.e., not significantly different) from untreated tissue at depths up to 60  $\mu\text{m}$  ( $p < 0.05$ ). The restoration of collagen organization was found both in the treated excised rat scleral samples (OC:  $0.30 \pm 0.01$  normal tissue,  $0.37 \pm 0.05$  collagenase-digested and  $0.28 \pm 0.03$  CMP-treated until 20  $\mu\text{m}$ ) and on intact mice eyes (OC:  $0.25 \pm 0.01$  normal tissue,  $0.30 \pm 0.05$  collagenase-digested and  $0.24 \pm 0.01$  CMP-treated).

**Discussion:** CMP treatment induced scleral collagen reorganization after collagenase digestion in murine models. These effects are consistent with inhibition or reversal of collagen enzymatic digestion. These results suggest that specific CMPs may have utility in the treatment of progressive myopia.

## KEYWORDS

myopia, collagen, sclera, collagen mimetic peptides, second-harmonic generation

## 1 Introduction

To address the visual complications associated with myopia and prevent its advancement into severe forms, there has been a growing interest in innovative therapeutic approaches. Myopia has emerged as a global health concern with a rising prevalence, presenting significant challenges to public healthcare systems (1). Progressive myopia, especially high myopia, carries an elevated risk of ocular complications, including retinal detachment, myopic maculopathy, and glaucoma, all of which can ultimately lead to vision impairment and blindness (2, 3).

Collagen, serving as the primary structural component of the sclera, plays a pivotal role in upholding the biomechanical integrity of the eye (4–6). Studies have shown an association between myopia and increased protease activity within the sclera (7–10). Consequently, interventions capable of modulating enzymatic collagen degradation within the sclera may hold promise as potential therapeutic avenues for myopia. Among these interventions, collagen mimetic peptides (CMPs) have emerged as potential agents for repairing and restoring collagen organization and structure (11, 12).

CMPs are synthetic peptides that mimic the structural and functional properties of natural collagen. CMPs are typically composed of amino acid sequences that resemble the repeating Gly-X-Y motif found in natural collagen, where Gly is glycine and X and Y can be any amino acid (typically proline or substituted proline residues) (13). CMPs have previously been used in tissue engineering and regenerative medicine applications to facilitate tissue repair and regeneration (13–15). The CMP investigated in the present study was similarly designed to attempt to repair helical collagen damaged by proteases, thus restoring the structural and functional properties of collagen to that seen in its undamaged state.

In this investigation, we employed second-harmonic generation (SHG) microscopy to evaluate how a novel CMP affects collagen in murine scleral tissue after collagenase treatment (16). Our primary objective was to assess the ability of this novel CMP to restore the organization of collagen that has undergone enzymatic digestion within rat scleral tissue. If successful, this endeavor could lead to innovative therapeutic approaches aimed at slowing the progression of myopia.

## 2 Materials and methods

### 2.1 Murine samples

Scleral tissue from albino Sprague–Dawley rats (Charles River Laboratories, Inc., Wilmington, MA, United States) and male C57BL/6 J mice (Jackson Laboratory, strain #000664) were used as the scleral collagen model. All animal use in this study conformed to the standards set in the Association for Research in Vision and Ophthalmology (ARVO) Statement for the Use of Animals in Ophthalmic and Vision Research and was approved by the University of Rochester University Committee on Animal Resources. The minimum number of samples deemed necessary for this pilot study were used in order to minimize animal sacrifice.

Fresh scleral tissue was obtained from 3 albino Sprague–Dawley rats euthanized by KCl injection. The 6 rat eyes were dissected, and the extra-scleral tissue, such as connective and muscle tissue, was removed using pulling it against the grain with angled forceps (17). Mice eyes ( $n = 8$ ) were obtained postmortem (P28–P49) following euthanasia by isoflurane overdose followed by cervical dislocation. The extra-scleral tissue was then meticulously removed similarly to the procedure for rat sclerae (17). The samples were preserved in phosphate-buffered saline (PBS) at 4°C when not in use and all experiments were done less than 12 h after euthanasia.

### 2.2 Imaging protocol

A custom-built SHG microscope was used to image the scleral tissue samples. The system was a new generation of a system previously described redundant (18), with some new features, including the illumination laser. Briefly, a femtosecond laser source (Fyla, Spain, 950–1150 nm, 20 fs, 80 MHz) was attenuated to 28.5 mW average power and focused into the sample plane using a high numerical aperture water-immersion microscope objective. The sample plane was mounted on an automated 3-axis XYZ translation stage. The backscattering signal ( $\lambda_0 = 550$  nm BW = 200 nm) from the sample plane was de-scanned by the same objective and focused onto a photomultiplier tube (Figure 1A). Calibrations of the system were performed using tissue from a single rat eye.

Each rat ( $n = 5$ ) scleral tissue sample had radial cuts made into it to allow it to be mounted flat on a standard microscope slide with a drop of a balanced saline solution (BSS) and a coverslip. Then, a series of 200  $\mu\text{m} \times 200 \mu\text{m}$  en face images (Lateral resolution: 0.375  $\mu\text{m}$ ) were taken at 5  $\mu\text{m}$  intervals through the full thicknesses of the sclerae approximately 2 mm from the optic nerve (Figure 1B).

For intact eye scleral imaging in mice, a compressive fixture was used to fix the cornea at base with cyanoacrylate, and to allow whole eye immersion in BSS (Figure 2A). The fixture consisted of two 3D printed pieces leaving a cuboidal space with a height of 3 mm (Figure 2B). This design enabled intact-eye imaging of the scleral tissue at the top (Figure 2C). Then, a series of 200  $\mu\text{m} \times 200 \mu\text{m}$  en face images (Lateral resolution: 0.375  $\mu\text{m}$ ) were acquired through the full thickness at 2- $\mu\text{m}$  intervals, and measured at 1 mm away from the optic nerve head.

### 2.3 Tissue treatment

After baseline SHG imaging, the tissue samples were partially digested on microscope slide (excised samples) or in the fixture (whole eyes) using a 200  $\mu\text{g}/\text{mL}$  solution of recombinant collagenase derived from *Clostridium histolyticum* with recombinant thermolysin (TDzyme® C/T; TDzyme, Inc., Dong-gu, Daegu, Republic of Korea) for 30 min. This was accomplished by removing the coverslip and placing 1 to 2 drops of the solution onto the surface of the tissue sample, enough to completely coat the apical surface of the sample. The samples were subsequently rinsed with BSS and re-imaged at

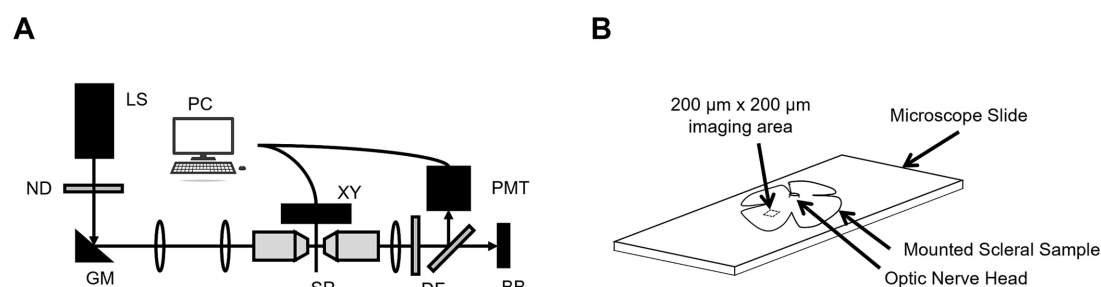


FIGURE 1

(A) The custom-built SHG microscope where LS = laser source, ND = neutral density, GM = galvanometer mirrors, PC = computer, XYZ = translation stage, SP = sample plane, DF = dichroic filters, PMT = photomultiplier tube, and BB = beam block. (B) A representative anatomical sketch of a scleral sample mounted on a microscope slide with the optic nerve head and SHG collection area illustrated (not to scale).

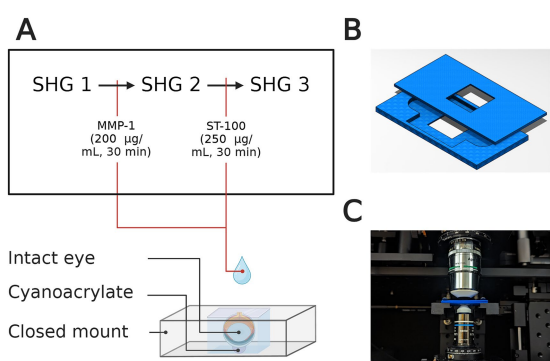


FIGURE 2

(A) Representative illustration of whole-eye setup for SHG imaging for untreated sample (SHG 1), after collagenase (MMP-1) treatment (SHG 2), and after CMP treatment (SHG 3). The cornea is fixed at the bottom using cyanoacrylate and the eye is immersed in BSS during imaging. (B) Top and bottom pieces of the intact-eye mount that were 3D-printed for each sample. (C) Representative image of the intact-eye mount with the custom-built confocal microscope before imaging.

approximately the same locations. The digested samples were then bathed in a 294 nM CMP solution (Stuart Therapeutics, Inc., Stuart, FL, United States) for 30 min again using 1 to 2 drops on the top surface of the tissue sample. The CMP solution “ST-100” provided by Stuart Therapeutics was composed of a linear, single-chain 21-mer collagen mimetic sequence with a (Gly-Pro-Pro)<sub>7</sub> motif. Lastly, the tissue samples were rinsed with BSS and underwent final SHG microscopy. It is important to note that all tissue treatments were performed without removing the tissue sample from the microscope slide or fixture, thus allowing for reasonable co-localization of pre- and post-treatment SHG images.

## 2.4 Image analysis

After collection, the SHG image stacks from each sample were analyzed using Matlab (MathWorks, Inc., Portola Valley, CA, United States). Two algorithms were used to estimate the collagen bundles orientation. Preprocessing of images for both algorithms included median filter for removing Poisson noise typical of SHG and

edge sharpener based on a Gaussian Low-pass filter ( $N = 10$ ,  $SD = 10$ ) was to use to enhance high spatial frequency contrast.

In the first algorithm, a two-dimensional Fourier algorithm was used to analyze the whole en face image and a Hanning window was used to remove the edge effect of image cropping. Then, the higher energy density peaks were selected as these represent more collagen bundles at a particular angle (Supplementary Figure S1). The angles at which these peaks are present were stored.

In the second algorithm, a gradient pyramid of the whole image is computed, and no windowing is required given that this algorithm does not require a spatial frequency analysis. Then, Principal Component Analysis (PCA) is used to estimate the local orientation for each overlapping square windows (sides of  $1.88 \mu\text{m}$ ). Assuming a constant orientation inside the windows, the gradient vector should be orthogonal to the orientation of the image pattern. So, an optimization task was defined to find the vector that maximizes orthogonality (19). Then, an intensity mask was used to preserve orientation information only where collagen signal was detected (Supplementary Figure S2) (20). Finally, the orientation information can be displayed spatially by color coding, with the intensity representing the presence of collagen at that particular depth (20, 21).

A previously validated metric, the order coefficient (OC), was used to quantify the collagen arrangement based on the orientation provided by each algorithm through depth. The OC represents a measurement of anisotropy of the scleral collagen fibers which ranges from 0 to 1. Increasing magnitude of the OC indicates increasing uniformity in the direction collagen fibers run in each SHG image. Collagen orientation information is transformed into polar coordinates and its distribution is analyzed using angular windows of  $7.5^\circ$  with shifts of  $1^\circ$  (22). A control test on 5 samples and 3 simulated fiber distributions demonstrated the equivalency between the two described algorithms in the estimation of OC.

## 2.5 Statistical analysis

The OC for each of the rat samples was calculated at each depth position then averaged across all 5 samples over sequential  $20 \mu\text{m}$  depth intervals. This  $20 \mu\text{m}$  depth interval average OC was statistically compared using a paired Student's two-tail t-test between the tissue samples in different experimental states: the untreated and post-collagenase states, the untreated and post-CMP treatment states, and



the post-collagenase and post-CMP treatment states. A paired test was utilized as data was comprised of measurements taken on a given sample before and after the various interventions and thus were treated as dependent variables in hypothesis testing using Excel (Microsoft, Inc., Redmond, WA, United States). The OC for each of the mice eyes was calculated over their entire depth, around 20  $\mu\text{m}$  thick (23), considering a single value average over the whole sample depth. One-way analysis of variance (ANOVA) with *post hoc* Tukey–Kramer analysis was used to test statistical significance in OC across treatments.

### 3 Results

Subjectively, SHG microscopy of the untreated scleral tissue revealed a high degree of collagen fiber curling and inter-fiber connectedness (Figure 3A). After collagenase treatment, the collagen fibers assumed a straightened configuration with widening of the inter-fiber spacing (Figure 3B). Tissue samples imaged after treatment with both collagenase and the CMP solution contained collagen fibers assuming a more interconnected and curled appearance compared to the collagenase treated tissue (Figure 3C).

The average OC in rat sclerae (from excised samples) across all 5 samples as a function of depth within the tissue samples is shown in Figure 4. The numerical OC and corresponding *p*-values are listed in Table 1. Collagenase digestion of the tissue samples resulted in a

statistically significant increase in the OC compared to the untreated tissue ( $p < 0.05$ ). CMP treatment of digested sclera resulted in a collagen organization that was more similar (i.e., not significantly different,  $p > 0.05$ ) from untreated tissue at all depths. The averages OC in mice sclerae (from whole eyes) along the sample depth, across all 8 eyes for the different treatments (Figure 5). Similarly, to experiment in rat sclerae, MMP-1 ( $0.30 \pm 0.05$ ) increased the alignment of collagen bundles ( $p < 0.05$ ) with respect to the virgin state ( $0.25 \pm 0.01$ ) in mice sclera. Also in this group, CMP ST-100 induced a significant reduction ( $p < 0.05$ ) of the OC ( $0.24 \pm 0.01$ ) (Figure 5).

### 4 Discussion

The present study used SHG microscopy to investigate the potential of a novel CMP (ST-100) with a (Gly-Pro-Pro)<sub>7</sub> motif to promote reparative changes in collagen organization within murine scleral tissue following collagenase digestion. The findings of this investigation are an important first step in elucidating a potential role for CMPs in addressing collagen degradation in the context of progressive myopia.

The effects of collagenase digestion on collagen fiber organization that we observed are consistent with the hypothesis that enzymatic degradation of the scleral extracellular matrix may play a role in the pathophysiology of progressive myopia (8). As

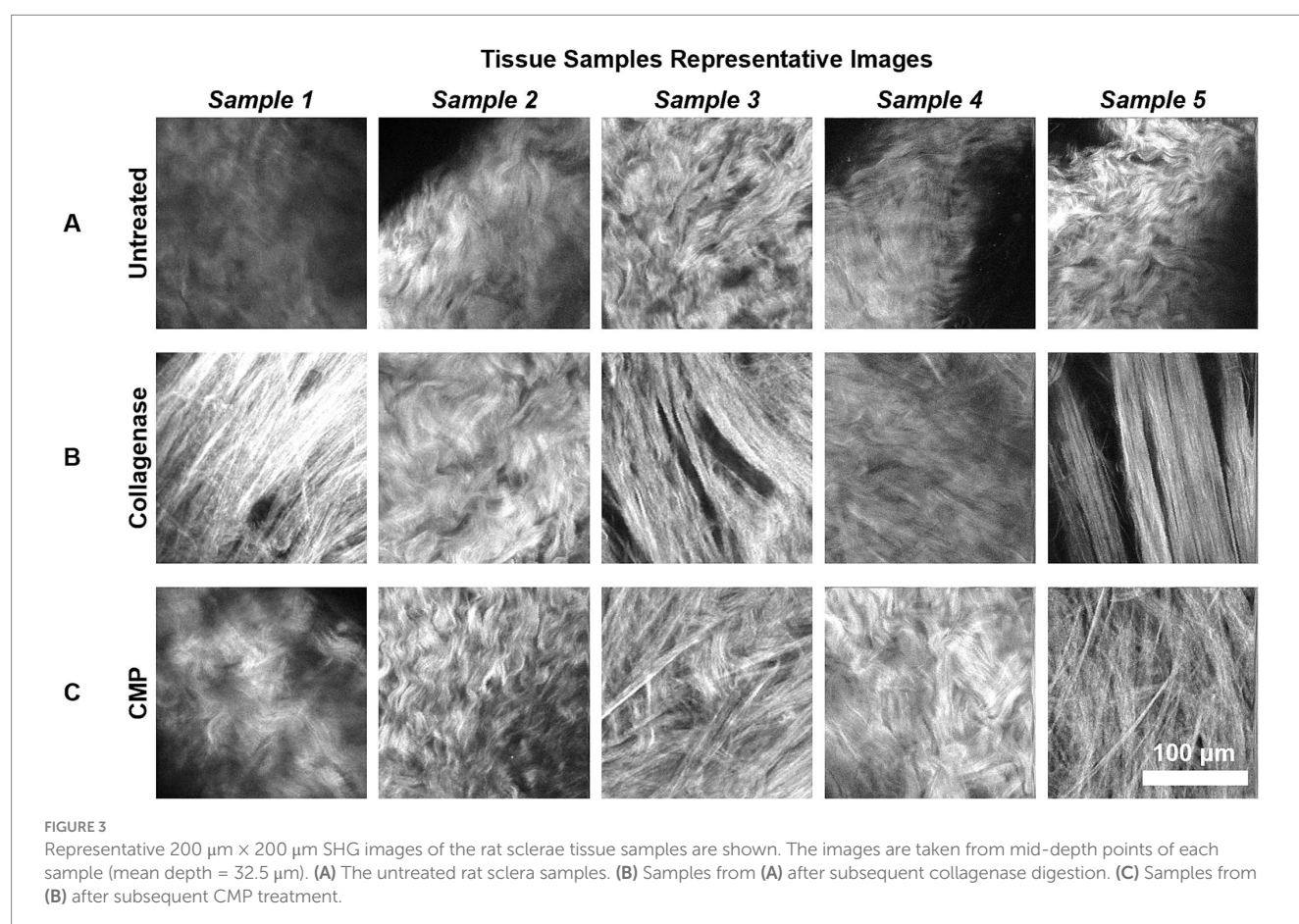
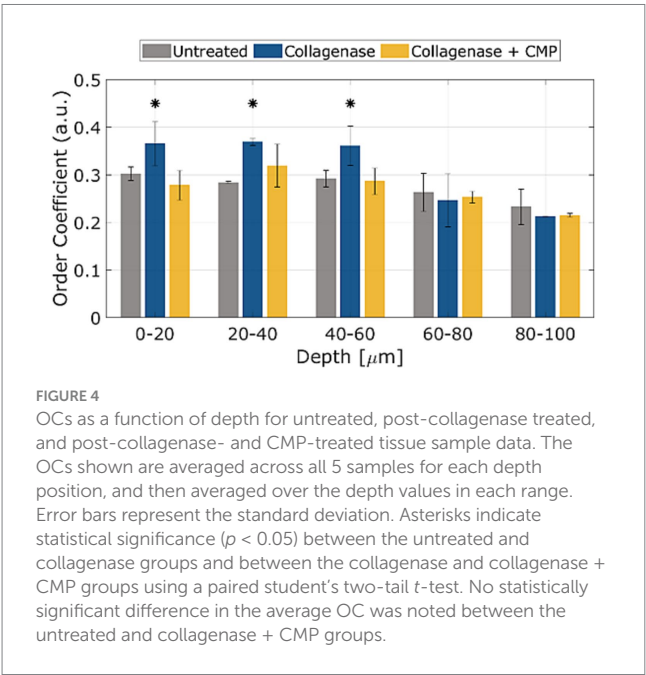


TABLE 1 The average OCs across all 5 samples as a function of depth ( $N = 20$  per depth interval) for untreated, post-collagenase treated, and post-collagenase- and CMP-treated tissue samples with standard deviations and  $p$ -values using a paired student's two-tail  $t$ -test.

Depth [ $\mu\text{m}$ ]	Average order coefficient						Paired $t$ -test-value		
	Untreated	SD	Collagenase	SD	CMP	SD	Untreated vs. collagenase	Collagenase vs. CMP	Untreated vs. CMP
0–20	0.302	0.014	0.365	0.046	0.278	0.031	0.020*	0.006*	0.060
20–40	0.284	0.002	0.369	0.007	0.319	0.045	0.005*	0.018*	0.074
40–60	0.292	0.018	0.361	0.041	0.286	0.028	0.003*	0.013*	0.782
60–80	0.263	0.040	0.246	0.056	0.253	0.012	0.273	0.670	0.228
80–100	0.232	0.037	0.212	0.001	0.215	0.004	0.233	0.651	0.095

SD, standard deviation; CMP, Collagen Mimetic Peptide, \*statistical significance ( $p < 0.05$ ).



noted, the untreated scleral tissue, as observed in our SHG microscopy images, exhibited a high degree of collagen fiber organization characterized by the typical curled appearance of scleral collagen fibers (24). However, collagenase treatment induced statistically significant changes in the collagen architecture consistent with a loss of collagen fiber interconnectedness, including straightening of the fibers and widening of the inter-fiber distances. These morphological changes may indicate a loss of scleral extracellular matrix strength and rigidity and may enable the elongation of the eye seen in progressive myopia (25–27).

Intriguingly, the application of CMP to the collagenase-digested scleral tissue samples appeared to have a reparative effect on collagen organization. The SHG microscopy images of tissue samples treated first with collagenase and then with CMP showed collagen fibers exhibited a more interconnected and curled appearance, which was visually distinct from the tissue after collagenase-only treatment. More importantly, the quantitative analysis using the OC revealed that CMP treatment of collagenase-treated tissue restored collagen

organization to a state that was not statistically different from the untreated tissue at depths up to 60  $\mu\text{m}$  in rat eyes, and over the full depth in mouse eyes. This finding suggests that CMPs have some potential to reverse the enzymatic degradation of collagen induced by collagenase, ultimately restoring the native collagen structure. It is possible that the CMPs may also have an inhibitory effect on the collagenase, however the present experiment was not designed to elucidate this.

Given that myopia is a progressive disease, further understanding of the mechanism by which CMPs impart their reparative effect is important for determining how effective CMP treatment may be over time. At least one other study has shown that CMPs are degraded by collagenase at a similar rate compared to natural collagen (28). Thus, the CMPs may act as a competitive antagonist to the collagenase enzyme, essentially preventing some quantity of the collagenase from binding to the scleral collagen. Alternatively, the CMPs may be intercalating into digested strands of damaged scleral collagen, effectively increasing crosslinking and fiber interconnectedness (29). A mixed mechanism is also possible. This study was not designed to elucidate the CMP reparative mechanism, but because it may inform the treatment potential of CMPs, it will be a subject of future investigations.

It is important to acknowledge that this study has certain limitations, including a small sample size, a study design that does not allow for differentiating the mechanism of the CMPs (i.e., enzymatic inhibition of the collagenase versus direct repair of the digested collagen fibers), and the use of *ex vivo* tissue. Further research is warranted to validate these preliminary results *in vivo* and to explore the long-term effects of CMP treatment on myopia progression and associated ocular complications. The experiment on intact mice eyes demonstrates that the finding holds when imaging is performed in a physiological setting more similar to *in vivo* conditions and in a backscattering mode. Additional next steps include studying the biomechanical properties of CMP-treated collagen to determine if there is a return to untreated levels of crosslinking and tensile strength.

In conclusion, this study provides initial evidence that CMP treatment can effectively restore collagen organization in collagenase-digested rat and mice scleral tissue. These findings suggest a potential role for CMPs in the development of innovative therapeutic strategies for the management of progressive myopia. Further research is needed to elucidate the precise mechanisms involved and to evaluate the clinical applicability of CMP-based interventions in myopia management.

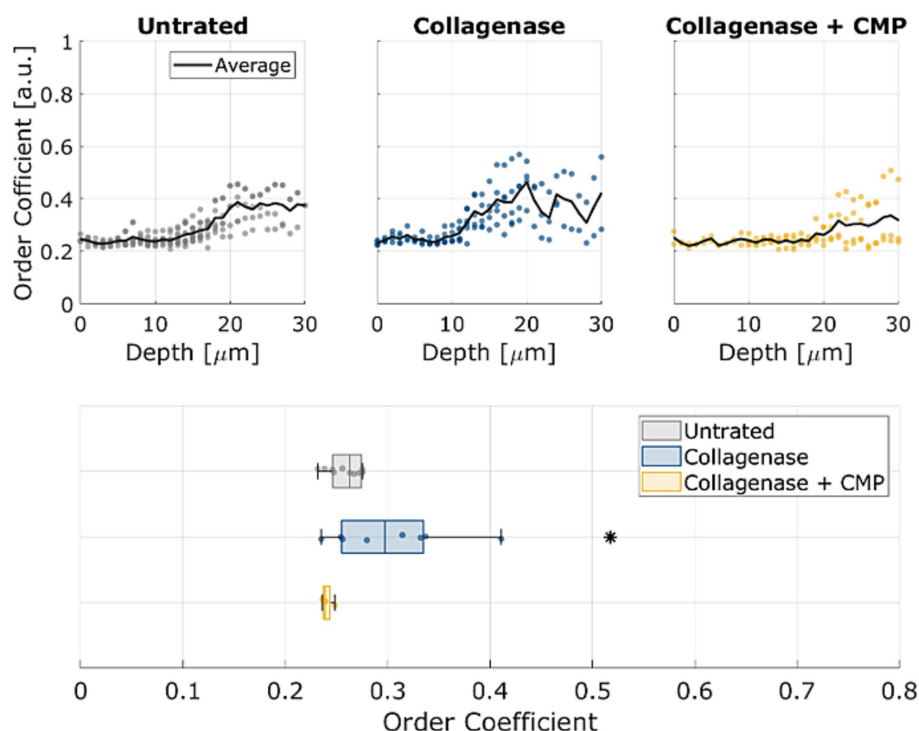


FIGURE 5

OCs as a function of depth for untreated, post-collagenase treated, and post-collagenase- and CMP-treated tissue sample data. The black line represents the average OC across all 8 samples through depth for each treatment. At the bottom, standard boxplots based on the average through the whole depth are shown. The asterisk indicates statistical significance ( $p < 0.05$ ) between the untreated and collagenase groups and between the collagenase and collagenase + CMP groups using ANOVA and a *post hoc* Tukey–Kramer analysis.

## Data availability statement

The raw data supporting the conclusions of this article will be made available by the authors, without undue reservation.

## Ethics statement

All animal use in this study conformed to the standards set in the Association for Research in Vision and Ophthalmology (ARVO) Statement for the Use of Animals in Ophthalmic and Vision Research and was approved by the University of Rochester University Committee on Animal Resources. The study was conducted in accordance with the local legislation and institutional requirements.

## Author contributions

DS: Data curation, Formal analysis, Methodology, Software, Visualization, Writing – original draft. AT: Data curation, Formal analysis, Methodology, Software, Visualization, Writing – review & editing. JZ: Data curation, Methodology, Writing – review & editing. JG: Data curation, Methodology, Software, Validation, Writing – review & editing. MRB: Resources, Methodology, Writing – review & editing. RB: Resources, Writing – review & editing. BD: Resources, Writing – review & editing. ES: Resources, Writing – review & editing. MT: Resources,

Methodology, Writing – review & editing. SM: Funding acquisition, Methodology, Project administration, Resources, Supervision, Writing – review & editing.

## Funding

The author(s) declare that financial support was received for the research and/or publication of this article. This work was supported in part by Stuart Therapeutics, Inc., a CVS Pilot Funds for Vision Research, National Institutes of Health – National Eye Institute P30 Core Grant EY001319-46, and an unrestricted grant from Research to Prevent Blindness (Flaum Eye Institute, University of Rochester, NY). The sponsor or funding organization participated in the review or approval of the manuscript.

## Acknowledgments

The authors would like to acknowledge Robert Baratta posthumously for his inspiration, mentorship, and many contributions to this project. Additionally, the authors would like to acknowledge Qian Wang for kindly providing the rats used in the present study and Jared Endres for help with the mice handling.

## Conflict of interest

RB, BD, ES, and SM have a financial stake in Stuart Therapeutics, Inc.

The authors declare that this study received funding from Stuart Therapeutics, Inc. The funder had the following involvement in the study: providing the collagen mimetic solutions free of charge.

## Generative AI statement

The authors declare that no Gen AI was used in the creation of this manuscript.

## References

- Morgan IG, Ohno-Matsui K, Saw S-M. Myopia. *Lancet*. (2012) 379:1739–48. doi: 10.1016/S0140-6736(12)60272-4
- Haarman AE, Enthoven CA, Tideman JWL, Tedja MS, Verhoeven VJ, Klaver CC. The complications of myopia: a review and meta-analysis. *Invest Ophthalmol Vis Sci*. (2020) 61:49. doi: 10.1167/iovs.61.4.49
- Flitcroft D. The complex interactions of retinal, optical and environmental factors in myopia aetiology. *Prog Retin Eye Res*. (2012) 31:622–60. doi: 10.1016/j.preteyeres.2012.06.004
- Keeley F, Morin J, Vesely S. Characterization of collagen from normal human sclera. *Exp Eye Res*. (1984) 39:533–42. doi: 10.1016/0014-4835(84)90053-8
- Avetisov E, Savitskaya N, Vinetskaya M, Iomdina E. A study of biochemical and biomechanical qualities of normal and myopic eye sclera in humans of different age groups. *Metab Pediatr Syst Ophthalmol*. (1983) 7:183–8.
- Norton TT, Rada JA. Reduced extracellular matrix in mammalian sclera with induced myopia. *Vis Res*. (1995) 35:1271–81. doi: 10.1016/0042-6989(94)00243-F
- Wride MA, Geatrell J, Guggenheim JA. Proteases in eye development and disease. *Birth Defects Res C Embryo Today*. (2006) 78:90–105. doi: 10.1002/bdrc.20063
- Zhao F, Zhou Q, Reinach PS, Yang J, Ma L, Wang X, et al. Cause and effect relationship between changes in scleral matrix metalloproteinase-2 expression and myopia development in mice. *Am J Pathol*. (2018) 188:1754–67. doi: 10.1016/j.ajpath.2018.04.011
- Guggenheim JA, McBrien NA. Form-deprivation myopia induces activation of scleral matrix metalloproteinase-2 in tree shrew. *Invest Ophthalmol Vis Sci*. (1996) 37:1380–95.
- Rada JA, Brenza HL. Increased latent gelatinase activity in the sclera of visually deprived chicks. *Invest Ophthalmol Vis Sci*. (1995) 36:1555–65.
- Baratta RO, Del Buono BJ, Schlumpf E, Ceresa BP, Calkins DJ. Collagen mimetic peptides promote corneal epithelial cell regeneration. *Front Pharmacol*. (2021) 12:705623. doi: 10.3389/fphar.2021.705623
- Baratta RO, Schlumpf E, Del Buono BJ, DeLorey S, Calkins DJ. Corneal collagen as a potential therapeutic target in dry eye disease. *Surv Ophthalmol*. (2022) 67:60–7. doi: 10.1016/j.survophthal.2021.04.006
- Yu SM, Li Y, Kim D. Collagen mimetic peptides: progress towards functional applications. *Soft Matter*. (2011) 7:7927–38. doi: 10.1039/C1SM05329A
- Xu Y, Kirchner M. Collagen mimetic peptides. *Bioengineering*. (2021) 8:5. doi: 10.3390/bioengineering8010005
- Huang NF, Zaitseva TS, Paukshto MV. Biomedical applications of collagen. *MDPI*. (2023) 10:90. doi: 10.3390/bioengineering10010090
- Chen X, Nadiarynk O, Plotnikov S, Campagnola PJ. Second harmonic generation microscopy for quantitative analysis of collagen fibrillar structure. *Nat Protoc*. (2012) 7:654–69. doi: 10.1038/nprot.2012.009
- Clayton A, Bishop AJR. Dissection of a mouse eye for a whole mount of the retinal pigment epithelium: 1940-087X. *J Vis Exp*. (2011) 48:2563. doi: 10.3791/2563
- Germann JA, Martínez-Enríquez E, Martínez-García MC, Kochevar IE, Marcos S. Corneal collagen ordering after in vivo rose bengal and riboflavin cross-linking. *Invest Ophthalmol Vis Sci*. (2020) 61:28. doi: 10.1167/iovs.61.3.28
- Xiao Guang F, Milanfar P, editors. Multiscale principal components analysis for image local orientation estimation. Conference record of the thirty-sixth Asilomar conference on signals, systems and computers (2002)
- Tecse A, Wozniak K, Germann JA, McMullen AJ, Buckley M, Baratta RO, et al. Scleral collagen remodeling and repair assessed in intact eyes through second harmonic generation. *Invest Ophthalmol Vis Sci*. (2024) 65:1167-.
- Kristen MT, Greene CA, Hetland RD, Zimmerle HM, DiMarco SF. True colors of oceanography: guidelines for effective and accurate Colormap selection. *Oceanography*. (2016) 29:9–13.
- Germann JA, Martínez-Enríquez E, Marcos S. Quantization of collagen organization in the stroma with a new order coefficient. *Biomed Opt Express*. (2018) 9:173–89. doi: 10.1364/BOE.9.000173
- Wen Y, Li Y, Zhu L, Tang T, Yan H, Hu J, et al. Nonlinear pathological trajectory of a high-myopia C57/BL6J mouse model induced by form deprivation. *Front Physiol*. (2024) 15:1442000. doi: 10.3389/fphys.2024.1442000
- Han M, Giese G, Bille JF. Second harmonic generation imaging of collagen fibrils in cornea and sclera. *Opt Express*. (2005) 13:5791–7. doi: 10.1364/OPEX.13.005791
- McBrien NA, Jobling AI, Gentle A. Biomechanics of the sclera in myopia: extracellular and cellular factors. *Optom Vis Sci*. (2009) 86:E23–30. doi: 10.1097/OPX.0b013e3181940669
- Harper AR, Summers JA. The dynamic sclera: extracellular matrix remodeling in normal ocular growth and myopia development. *Exp Eye Res*. (2015) 133:100–11. doi: 10.1016/j.exer.2014.07.015
- McBrien NA, Gentle A. Role of the sclera in the development and pathological complications of myopia. *Prog Retin Eye Res*. (2003) 22:307–38. doi: 10.1016/S1350-9462(02)00063-0
- O'leary LE, Fallas JA, Bakota EL, Kang MK, Hartgerink JD. Multi-hierarchical self-assembly of a collagen mimetic peptide from triple helix to nanofiber and hydrogel. *Nat Chem*. (2011) 3:821–8. doi: 10.1038/nchem.1123
- Chattopadhyay S, Raines RT. Collagen-based biomaterials for wound healing. *Biopolymers*. (2014) 101:821–33. doi: 10.1002/bip.22486

## Publisher's note

All claims expressed in this article are solely those of the authors and do not necessarily represent those of their affiliated organizations, or those of the publisher, the editors and the reviewers. Any product that may be evaluated in this article, or claim that may be made by its manufacturer, is not guaranteed or endorsed by the publisher.

## Supplementary material

The Supplementary material for this article can be found online at: <https://www.frontiersin.org/articles/10.3389/fmed.2025.1514073/full#supplementary-material>