



# Opportunities and Challenges for Nanotherapeutics for the Aging Population

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Nanotherapeutics utilize the properties of nanomaterials to alter the pharmacology of the drugs and therapies being transported, leading to changes in their biological disposition (absorption, distribution, cellular uptake, metabolism and elimination) and ultimately, their pharmacological effect. This provides an opportunity to optimize the pharmacology of drugs, particularly for those that are dependent on hepatic action. Old age is associated with changes in many pharmacokinetic processes which tend to impair drug efficacy and increase risk of toxicity. While these age-related changes are drug-specific they could be directly addressed using nanotechnology and precision targeting. The benefits of nanotherapeutics needs to be balanced against toxicity, with future use in humans dependent upon the gathering of information about the clearance and long-term safety of nanomaterials.

**Keywords:** drug delivery and targeting, ADME and toxicity, nano, ageing, clinical challenges, quantum dot, solid lipid nanoparticle, pharmaceutical

## INTRODUCTION

The use of nanotechnology in medicine is a rapidly emerging area. In 2016, Anselmo and Mitragotri (2016) highlighted the clinical landscape of nanotherapeutics which included over 25 FDA approved nanotechnologies and 45 that were in clinical trials. By 2019, there were 50 nanotherapeutic formulations available for patient care, including cancer treatments, iron-replacement therapies, contrast agents and vaccines (Anselmo and Mitragotri, 2019). In addition, there were 90 clinical trials of nanomedicines which included 15 new nanotechnologies (Anselmo and Mitragotri, 2019). Following this, the emergence of lipid nanoparticles (NPs) for vaccine delivery in response to COVID-19 (Shin et al., 2020; Khurana et al., 2021) has delivered the shot-in-the-arm nanotherapeutics needed to demonstrate their broader potential.

The goal of nanotherapeutics or nano-drug delivery is to develop next generation therapies that have increased: safety; biocompatibility; bioavailability; therapeutic action and bio-adherence; and

**Abbreviations:** Alb, albumin; ABC, ATP-binding cassette; DC, dendritic cell; FSA, formaldehyde treated serum albumin; GI, gastrointestinal; GFR, glomerular filtration rate; KC, Kupffer cells; LSEC, liver sinusoidal endothelial cells; MPS, mononuclear phagocytic system; NP, nanoparticle; P-gp, P-glycoprotein; QD, quantum dot; SLC, solute carriers; SLCO, solute carrier organic anion; SLN, solid lipid nanoparticles.

**TABLE 1** | Summary of the changes with aging on drug deposition and the effect on nanotherapeutics.

Feature	Change with aging	Effect on nanotherapeutics
Absorption		
Gastric acid	Decreased secretion Hilmer. (2008)	Reduced degradation Bi et al. (2020)
Gut motility	Delayed gastric emptying Klotz. (2009)	Increased absorption time Bi et al. (2020)
Microbiota	Reduced diversity and leaky gut Walrath et al. (2021)	Potential increase in toxicity Bi et al. (2020)
Injectable	Injection absorbance unaffected Heise et al. (2017)	Injectable NPs are unaffected Pardi et al. (2015)
Permeability		
Passive	Unaffected Yuasa et al. (1997)	Unaffected Bi et al. (2020), Hunt et al. (2021)
Solute transporters	Reduction in OCT transporters, P-gp unaffected in gut Warrington et al. (2004), Jang et al. (2016)	NPs are absorbed by a broader range of transporters Hunt et al. (2020), Hunt et al. (2021)
1st pass metabolism	Decreased due to reduced blood flow Mclean and Le Couteur. (2004)	Prolonged circulation time Hunt et al. (2021)
Distribution		
Plasma proteins	Reduced circulating albumin Klotz. (2009)	May reduce protein corona
Body composition	Decreased water content, increased fat content Mclean and Le Couteur. (2004)	May reduced distribution of water-soluble NPs, increased distribution of fat-soluble NPs
Cell uptake		
Complement proteins	Reduced circulating IgG, increased classical and alternative complement cascades Gaya Da Costa et al. (2018), Gudelj et al. (2018)	Potential change in NP opsonisation in elderly La-Beck et al. (2021)
Phagocytosis	Reduced clearance, but with increased number and circulating inflammatory markers Hunt et al. (2019)	Unaffected MPS uptake Pomatto et al. (2018)
Endocytosis	By LSECs is slightly reduced Simon-Santamaria et al. (2010)	Largely unaffected Hunt et al. (2020)
Transcytosis	By LSECs is unaffected Simionescu et al. (2009)	Unaffected Hunt et al. (2020)
Passive uptake	Decreased due to pseudocapillarization Le Couteur et al. (2008)	Reduced NP uptake Hunt et al. (2021)
Metabolism		
Phase I	Reduced (due to hepatic blood flow) Mclean and Le Couteur. (2004)	Prolonged circulation time Hunt et al. (2021)
Phase II	Reduced Mclean and Le Couteur. (2004)	Unaffected Pomatto et al. (2018)
Clearance		
Passive renal elimination	Decreased GFR and increased renal vascular resistance Mclean and Le Couteur. (2004)	Potentially unaffected Pinheiro et al. (2019)
Active renal elimination	Decreased P-gp, OCT2 and MATE soluble transport Warrington et al. (2004), Xu et al. (2017)	May decreased NP clearance via P-gp and MATE
Biliary elimination	Decreased xenobiotic elimination due to decreased soluble transporters (Xu et al., 2017)	Decreased NP clearance Pinheiro et al. (2019)

reduced: dosage, clearance and metabolism (Sahoo et al., 2007). Nanoscale formulations have facilitated advanced engineering of drug pharmacology in order to optimize drug release, absorption, site-directed distribution, metabolism and excretion, and drug residence time (Suk et al., 2016; Patra et al., 2018). These advances have been strongly mediated by PEGylation of nanotherapeutics and drugs to prolong their circulation time, and delay immune recognition and metabolism (Suk et al., 2016).

Next generation advances include sensor-based drug release, targeting to intracellular compartments, improved modelling and screening of nanotechnology platforms, and the application of nanotechnology to a broader range of therapeutic classes including proteins, DNA, siRNA and miRNA (Sindhvani and Chan, 2021). These recent advances have highlighted that nanomaterials have broad impacts on drug absorption, distribution, metabolism and excretion, and the importance of framework for their regulation (Zolnik and Sadrieh, 2009). However, these studies have also highlighted that nanotherapeutics in aged cohorts are rarely investigated.

This presents a critical problem as the most common user of drug therapeutics are the older (60+ years) population (Martin et al., 2019). This problem exists for many drug therapeutics with older patients rarely participating in clinical trials and proposed to limit the efficacy once translated to the clinic (Shenoy and

Harugeri, 2015). With 85% of adults over 60 years taking at least one medication (Martin et al., 2019) and two-thirds of these using 4 or more drugs (Elliott, 2006) this highlights that therapeutics, including nanotherapeutics, will primarily be given to this older age bracket.

Aging promotes changes in the pharmacokinetics and pharmacodynamics of nearly all medications in a drug dependent way (Klotz, 2009; Reeve et al., 2015; Khan and Roberts, 2018). In the case of nanotherapeutics this may impede the advantages that a nanomaterial might have on the disposition of a therapeutic agent. On the other hand, nanotherapeutics could be designed to overcome age-related changes in pharmacokinetics that can impair the efficacy of drugs in older people. The aim of this review is to provide an overview of the broad changes in drug absorption, distribution, cellular uptake, metabolism, drug action and removal facilitated by nanomaterials (summarized in **Table 1**). Then, we describe how these effects may offset age-related changes in the disposition of drugs and mitigate off target effects by precision drug delivery.

Administrative route of nanotherapeutic studies: mixed (Pardi et al., 2015); oral (Bi et al., 2020; Hunt et al., 2020; Hunt et al., 2021), IP injection (Weitzmann et al., 2015; Pinheiro et al., 2019) and inhalation: (Pomatto et al., 2018).

## ABSORPTION

Nanotherapeutics administration can occur in several ways. When given orally, absorption occurs *via* the stomach and gastrointestinal (GI) tract. Subcutaneous or intraperitoneal delivered therapeutics are taken up *via* the circulation, and those that are intravenously injected are placed directly into the systemic circulation. Bioavailability is the fraction that reaches the systemic circulation—by definition drugs given *via* intravenous injection will have 100% bioavailability.

The kinetics of lipid NPs with a payload of mRNA were studied when given *via* multiple injection techniques (intramuscular, subcutaneous, intraperitoneal, intravenous or intradermal) (Pardi et al., 2015). Systemic uptake and distribution were rapid with all these routes of administration. A key difference, was that intravenous injections recorded a  $C_{max}$  (peak concentration) 10-fold higher than all other injection methods with  $T_{max}$  (time to reach peak) occurring at the same time point for all methods of administration. Intravenous injections demonstrated the shortest half-life by 2-fold compared to subcutaneous and intraperitoneal and 3-fold compared to intramuscular and intradermal injections (Pardi et al., 2015).

The evaluation of the oral absorption of nanotherapeutics has been performed with *in vitro* and *in vivo* methods. The results show that it is important to perform multiple methods to determine the bioavailability fraction within initial nanomedicine research (Faria et al., 2018). The absorption of orally administered nanomaterials through the GI tract is facilitated by Peyer's Patches or aggregated lymphoid nodules, M cells and enterocytes (Schimpel et al., 2014). Lymph draining patches have been observed to promote uptake of a range of different sized nanomaterials (alginate coated chitosan NPs and polymeric NPs) from 50 nm to 200  $\mu$ m and have been investigated for immune modulation strategies, however, absorption *via* lymphatics doesn't equate to improved bioavailability (Borges et al., 2006; Des Rieux et al., 2006). Finally, Yao et al. (2015) used Au NPs to demonstrated intestinal enterocytes can take up more limited range of nanomaterials (50–500 nm) with uptake increasing with reductions in NP size.

Enterocyte uptake has been extensively evaluated using Caco-2 cells for metal NPs (Imai et al., 2017), organics (Behrens et al., 2002; Coyuco et al., 2011), dendrimers (Kitchens et al., 2007) and solid lipid nanoparticles (SLN) (Chai et al., 2016). Caco-2 cells and co-cultures of Caco-2/HT29-MTX (enterocyte, mucus-secreting goblet and M cells) are utilized to visualize and measure the dynamics of NP transfer (Schimpel et al., 2014). To further understand these pathways the use of endocytosis inhibitors has demonstrated that the uptake of metals, organics, dendrimers and SLN is *via* multiple specific and non-specific pathways. For example, the uptake of SLN and dendrimers, are mediated by macropinocytosis, clathrin- and caveolin-mediated endocytosis (Kitchens et al., 2007; Chai et al., 2016). These endocytosis and transcytosis pathways are forms of active transport within the GI tract but also the liver; here they are

responsible for the direct remove of systemically circulating nanomaterials (discussed in *Distribution*).

In our previously study, Hunt et al. (2020) utilized small intestine explants to study the uptake of NPs. Explants allow uptake to be studied with the ease and flexibility of *in vitro* cell cultures but have greater similarity to the *in vivo* environment (Kothari and Rajagopalan, 2019). Using explants, we found that metal ( $Ag_2S$ ) quantum dots (QDs) were non-specifically taken up into small intestine explants and were blocked by inhibitors acting on macropinocytosis, and clathrin- and caveolin-mediated endocytosis (Hunt et al., 2020). Coating the surface of these QDs with various polymers facilitated receptor specific endocytosis pathways. We subsequently determined the *in vivo* bioavailability of conventional and polymer coated QDs, and found that these results reflected those found in the explant studies (Hunt et al., 2020).

These studies highlight that nanomaterials are not passively absorbed, but actively taken up by multiple transporters. This pathway is not unique to nanomaterials with drugs, and more broadly xenobiotics are heavily dependent on active transport channels, particularly solute carriers (SLC) and solute carrier organic anion (SLCO) superfamilies of membrane transporters (Döring and Petzinger, 2014).

Targeting of specific nutrient transporters (SLC5A6, SCL10A2, and SLC22A5) *via* the use of surface coatings, NP formulations and selective dendrimers has been extensively investigated to improve the oral bioavailability of nanotherapeutic drug delivery platforms (Kou et al., 2018). Utilizing biotin, deoxycholic acid, tetra DOCA, taurocholic acid and L-carnitine multiple groups have shown improved bioavailability of oral insulins and heparin (Lee et al., 2001; Lee et al., 2005; Lee et al., 2006; Kim et al., 2007; Khatun et al., 2013; Alam et al., 2014; Zhang et al., 2014). These groups observed that both the drug delivered, and the materials used are rapidly distributed to the liver and metabolized following absorption. This critically demonstrates the potential use of these drug delivery platforms for targeting hepatic drug receptors.

Recently there has been increasing interest in the effects of the gut microbiota on the metabolism of xenobiotics (including NPs). Microbiota facilitate metabolism *via* azo reduction, amide formation, hydrolysis, acetylation, nitro reduction, deamination, sulfoxide/oxide reduction and thiazide ring formation (Jourova et al., 2016). Degradation of Ag NPs has been extensively examined and dependent on gastric pH and the microbiome (Bi et al., 2020). There are complex multi-directional relationships between Ag NPs (particularly those with a diameter less than 10 nm), the intestinal microbiota, and the epithelial mucus. NPs increase mucosal secretions which limit their interactions between the cell membrane and inhibit uptake. Ag NPs may also directly impact on the composition of the microbiome, decreasing *Firmicutes* and *Lactobacillus* populations (Bi et al., 2020).

## Absorption and Aging

Aging is associated with impeded oral absorption of drugs and changes in their pharmacokinetic profile (Vinarov et al., 2021).

This is due to several factors, primarily due to decreased blood flow to most organs including the mesenteric system which contributes to the delayed absorption of drugs and metabolites observed in elderly patients. Critically for injected materials, older patients demonstrate similar pharmacodynamic responses to younger patients (e.g., fast acting insulin), which indicates there are no age-related changes in injectable absorption (Heise et al., 2017).

Modification of GI metabolism in older patients delays absorption of drugs, metabolites and xenobiotics. Passive intestinal transport of most substances is not considered to be affected by aging (Yuasa et al., 1997; Saltzman and Russell, 1998), yet active transportation *via* solute transporters (SLCs and SLCOs) has been shown to be impacted by aging. As reviewed by Hilmer (2008) the active transportation of glucose, calcium and Vitamin B12 are all observed to decrease with aging in rats.

Active transport of drugs, NPs and xenobiotics are heavily dependent on solute carriers and mucin-adhesion (Döring and Petzinger, 2014; Marczynski et al., 2021) with age-related reduction in secretory mucins and altered glycan profiles impede transport *via* solute carriers (Kameyama et al., 2021). In the rodent GI tract old age is not associated with changes in enzyme P450 (CYP3A4) or the soluble transporter p-glycoprotein (P-gp/ABCB1/MDR1) (Warrington et al., 2004). Together these results suggest that those drugs and xenobiotics that are actively transported by SLCOs such as OCT1 (e.g., metformin) have impaired absorption in older patients (Jang et al., 2016). Comparatively, carbon NPs coated with carboxylic acid demonstrate uptake *via* P-gp (Coyuco et al., 2011) and may not be affected by changes with age. Finally, Hunt et al. (2021) investigated the uptake of QD capped with carboxylic acid and conjugated metformin in aging mice. In old mice there was a decreased uptake of metformin, with attachment to QDs preventing this decline. Inhibitor studies showed there were age-related changes in the soluble transporters that mediated absorption of metformin.

Drug absorption can also be influenced by age-related changes in gastric pH. There is a 20–25% reduction in gastric acid secretion in old age, leading to increased gastric pH. These aging changes are compounded by age-related changes in diet and increased use of medications such as protein pump inhibitors (Hilmer, 2008; Reeve et al., 2017; An et al., 2018). Gastric acid is a critical barrier for nanotherapeutics due to the risk of degradation of the transported drug (Tyagi et al., 2018). Improved yields for nanotherapeutics may occur in older people secondary to the reduction in gastric acid secretions. In mice, pretreatment with a protein pump inhibitor to increase gastric pH, increased 3-fold the oral bioavailability of growth hormone in liposomes (Parmentier et al., 2014). As well as changes in gastric pH, there is age-related reduction in gut motility that delays gastric emptying, generally prolonging  $T_{max}$  and decreasing  $C_{max}$  rather than altering overall absorption (Holt, 2007; Saffrey, 2014).

Aging is associated with increased leakiness of the gastrointestinal epithelial barrier and changes in the microbiota (Walrath et al., 2021). In humans, there is a high

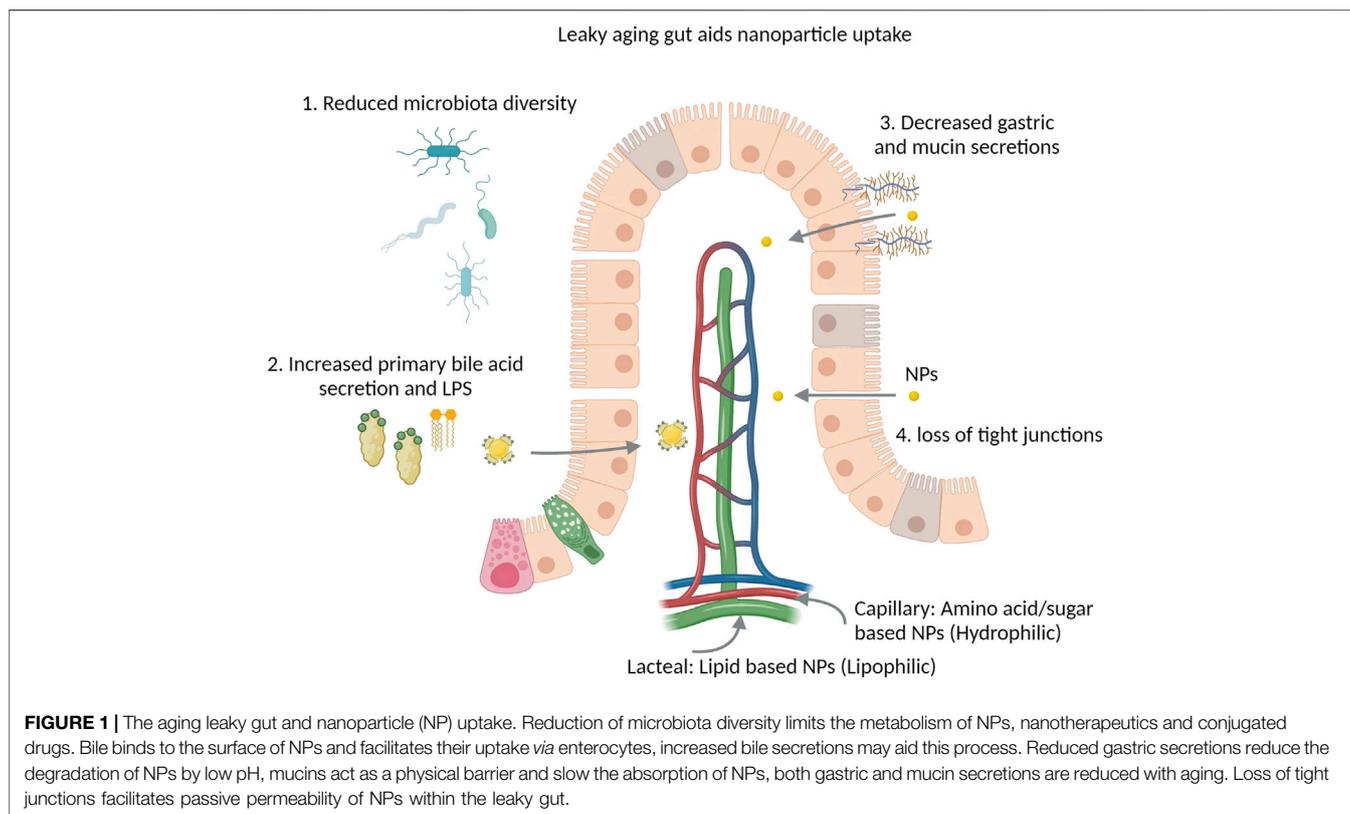
degree of variability due to diet and drugs (Claesson et al., 2011), however it has usually been reported that old age is associated with reduced microbial diversity (Bischoff, 2016), decreased Firmicutes and increased Proteobacteria (Walrath et al., 2021). Changes in gut microbiome contribute to decreased bacterial short chain fatty acids, increased lipopolysaccharides and decreased secondary bile acid production. This leads to degradation of the intestinal barrier observed with aging, called the leaky gut model of aging and inflammation (Mäkivuokko et al., 2009; Bischoff, 2016; Walrath et al., 2021). The 'leaky gut' may pose a broader challenge to orally administered nanotherapeutics due to its potential effects on passive diffusion and inflammation within the gut wall and lumen (Figure 1).

## DISTRIBUTION

Distribution refers to the accumulation within peripheral compartments or the steady state concentration at the site of action relative to the concentration in the circulation. The effect of drug distribution on blood levels of a drug is usually seen after the effects of absorption, bioavailability and 1st pass metabolism have occurred (Doogue and Polasek, 2013).

Distribution poses a challenge for nanotherapeutics. Conventional metal based or uncoated NPs have very poor distribution and bioavailability as they are generally cleared from the blood circulation within 10 min of systemic administration regardless of their composition (Moghimi et al., 2001; Yoo et al., 2010; Suk et al., 2016). This rapid uptake and accumulation occurs primarily within the liver and is the product of 1st pass metabolism and the liver's exceptional clearance rate of xenobiotics, including nanomaterials, and the mononuclear phagocytic system (MPS). To limit this uptake into the liver, and bypass 1st pass metabolism and MPS, the most effective strategy has been PEGylation, with sub 100 nm PEGylated NPs having a longer circulating time than conventional NPs as reviewed by Alexis et al. (2008); Suk et al. (2016).

NP uptake by the liver and MPS is discussed in the *cellular uptake* section, nevertheless, it is important to discuss the role of the circulatory system in aiding these clearance pathways. Circulating proteins such as serum albumin, complement, glycoproteins, lipoproteins, coagulants and immunoglobulins bind readily to NPs (Madathiparambil Visalakshan et al., 2020). This leads to the formation of soft and hard protein coronas composed of 10–1,000 s of proteins within minutes of entering the circulatory system (Ke et al., 2017). There are vast differences in the number of proteins that can bind to NPs based on their composition, shapes and surface chemistry with differences in hard and soft protein coronas directing circulation time and differential cellular uptake (García-Álvarez et al., 2018; Richtering et al., 2020). Cloaking NPs from protein corona formation is a key strategy for targeted drug delivery (Oh et al., 2018; Alberg et al., 2020). The prefabricated attachment of serum albumin to NPs is one method utilized to avoid MPS uptake (Pitek et al., 2016).



## Distribution and Aging

Aging is associated with decreased muscle mass, body water and organ mass and increased fat mass. At very advanced ages (>85 years) there is often a decrease in fat mass associated with frailty (Hilmer et al., 2019). Each year after the age of 50, body fat increases 1% and body water decreases by 1% (Hilmer, 2008). This increases the volume of distribution of lipophilic drugs and decreases the volume of distribution of hydrophilic drugs (Mclean and Le Couteur, 2004; Klotz, 2009). This may affect the distribution of lipophilic and hydrophilic NPs in aging animals, however this has not been investigated to date. Finally, tissue perfusion decreases with age particularly to muscle and splanchnic tissues (Payne and Bearden, 2006).

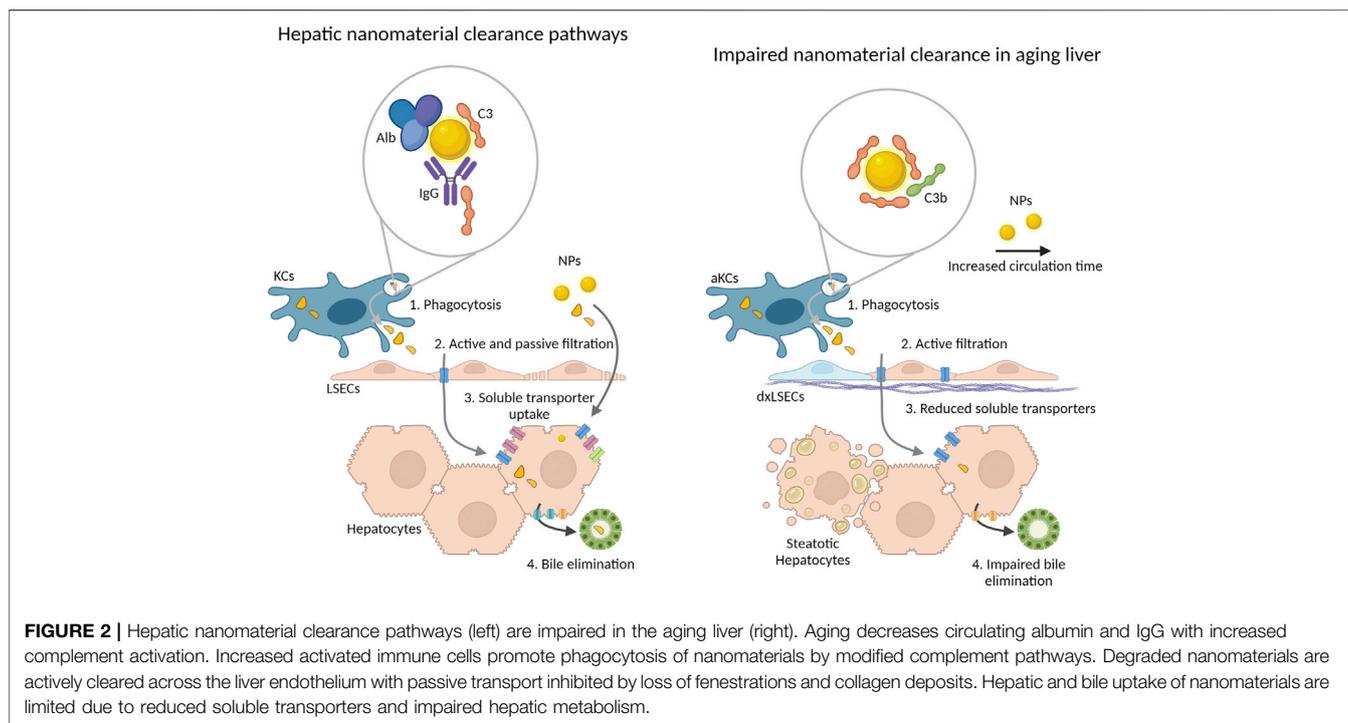
NPs are composed of a broad range of materials, with ranging solubility, surface reactivity, and lipophilic, zwitterion and hydrophobic surface chemistries (Date et al., 2016). They also have broad ranging interactions with circulating materials demonstrating high and low affinity for circulating proteins (Ke et al., 2017). Collectively NPs present many characteristics of drugs, and it may be suggested that NPs may have as broad ranging level of effectiveness as drugs collectively do in aging populations.

Circulating proteins also demonstrate changes with age.  $\alpha 1$  acid glycoprotein increases with age (Hilmer, 2008), decreasing the free fraction of basic drugs binding to albumin, particularly high affinity drugs such as levodopa, warfarin and phenytoin (Israïli and Dayton, 2001). Similarly, serum albumin decreases with age (15–20%) but rarely impacts on drug effects (Klotz, 2009) as bound drugs are inactive and drugs that have high

affinity for albumin are often given at lower dosages in older patients (Reeve et al., 2015). The key risk factor in these drug formulations is increased drug availability due to reduced circulating albumin, correlating with greater side effect profiles (Reeve et al., 2015).

The protein corona may also render the transported drug inactive, because the drug can bind to non-specific sites in the proteins that make up the protein corona. Nanotherapeutics with a protein corona can release the drug or therapeutic release, but this may be limited by the scale of the protein corona (Ke et al., 2017). Ascertaining dosages of nanotherapeutics in older patients is complex because the dose of the therapeutic agent, the nanomaterial and possibly the protein corona must be considered. Aging is associated with increased inflammatory markers and complement (Singh and Newman, 2011) yet little evidence on how age-related changes in circulating proteins influence the formation of coronas on NPs, or whether this necessitates any change in dosing in older people.

The uptake and distribution of nanotherapeutics into target cells by transporters can be impeded with aging. Recently, Hunt et al. (2021) investigated the hepatic delivery of Ag<sub>2</sub>S QD-nicotinamide mononucleotide (NMN) in young and old mice. NMN acts within the liver but has poor bioavailability in young mice and impaired efficacy in old mice (Hunt et al., 2021). NMN is transported by SLC12A8 (Grozio et al., 2019) with QD conjugation facilitating a 10-fold increase in its transportation by pinocytosis and clathrin-mediated endocytosis *in vitro* (Hunt et al., 2021). In young animals a 10,000-fold reduction in dosage was required to induce changes in glucose sensitivity *in vivo*. QD-NMN treatment in old



animals led to improved glucose and insulin sensitivity with no effect observed with NMN treatment alone (Hunt et al., 2021). QDs increased the potency of NMN in young mice and overcame the lack of responsiveness to NMN in old mice.

## CELLULAR UPTAKE

The MPS consists of splenic and lymph derived monocytes and macrophages along with KCs in the liver. The KCs are the first barrier that NPs must overcome in order to enter the systemic circulation with the second barrier being the scavenger endothelial cells of the liver or LSECs (Poon et al., 2019). NP uptake is primarily performed by MPS cell types and LSECs following optimization or complement attachment, however other passive and active transporters also have a role in NP clearance (**Figure 2**). Passive clearance of NPs from the blood is performed *via* nanopores in the LSECs called fenestrations (sub 120 nm); these NPs enter the Space of Disse and may then be taken up by hepatocytes and directed towards to bile (Cogger et al., 2020) (discussed in *Metabolism* and *Urinary and Biliary Elimination*).

KCs are the major cells involved with the uptake of NPs by phagocytosis (Tsoi et al., 2016), yet they perform multiple other functions, some of which can influence nanotherapeutics. They have a role in tolerogenic regulation *via* suppression of T regulatory cells and stimulation of IL-10 release (Breous et al., 2009). KCs also facilitate cross talk between dendritic cells (DCs), natural killer cells and natural killer T cells (Nguyen-Lefebvre and Horuzsko, 2015). KCs are strongly activated by C3

complement products which activates phagocytosis and increases uptake of NPs (Helmy et al., 2006; Nguyen-Lefebvre and Horuzsko, 2015). On the other hand CD47-mediated immune suppression leads to a reduction of NP uptake by macrophages including KCs (Yong et al., 2017).

C3a and C3b are common components of protein coronas that encapsulate NPs. In a recent study the attachment of C3a and C3b to NPs was shown to be dependent on primary immunoglobulin binding to NPs, particularly IgG (Vu et al., 2019). IgG provided a scaffolding for C3b binding, with the epitope for NP attachment still to be identified (Vu et al., 2019). This is not surprising as IgG can naturally absorb non-specifically onto multiple pathogens, antigens, surfaces, proteins and is used as a control in flow cytometry for this property. IgG can attach to SPIONs, liposomes, Fe NPs and Au NPs (Bell et al., 2013; Vu et al., 2019). Macrophages also recognize NPs by the attachment of Fc or fibronectin (Neuberger et al., 2005). In addition, opsonin-independent scavenger receptors on macrophages also facilitate NP clearance (Walkey et al., 2012). Similarly, this is also performed by LSECs (Monopoli et al., 2012; Tenzer et al., 2013). The LSEC receptors involved in NP uptake remain to be identified, it is likely that several receptors facilitate uptake with varying effectiveness, of particular interest is stabilin-2 given that liposome based NPs are endocytosed by stabilin-2 in zebra fish (Campbell et al., 2018).

The role of the scavenger endothelium, and how scavenging fits in relative to phagocytosis needs to be discussed in the context of NP clearance. Phagocytosis is performed by KCs, DCs and mononuclear cells while clathrin-mediated scavenging is a form of pinocytosis (cellular drinking) and transcytosis/endocytosis which facilitates uptake of soluble sub-200 nm materials

(Sørensen et al., 2012). This difference is critical as NPs retained within phagocytic cells (particularly non-degradable NPs) have long term retention (months to years) while NPs scavenged by clathrin-mediated-endocytosis are degraded, exocytosed and cleared within the urine or bile within days to weeks (Zhang et al., 2016; Hunt et al., 2021). This provides a rationale for designing nanomedicines that are preferentially targeted by scavenging rather than phagocytosis.

Endothelial transcytosis and endocytosis are mediated by clathrin coated pits. Visualization of this process was performed by Kishimoto and Tavassoli (1987) using an Fe-transferrin complex labelled with nano-sized colloidal gold. This complex was internalized and transported *via* tubules and vesicles followed by exocytosis into the space of Disse, the space between the LSECs and hepatocytes. Transcytosis and endocytosis are either receptor mediated or independent. Independent transcytosis occurs for plasma solutes and macromolecules (limited to 70 nm by the size of clathrin-coated pits) such as glycogen, dextran and ferritin (Simionescu et al., 2009). Clathrin-mediated transcytosis facilitates the transport LDL, transferrin, ceruloplasmin, insulin and albumin (alb) (Simionescu et al., 2009). Recently included in this list are chemokines CXCL10 and MCP-1, and glycated proteins (Li et al., 2013; Neumann et al., 2015; Shetty et al., 2018). The clathrin-coated pits contain receptors of IL-1, p75 (death receptors), insulin, AGE, CP, Tf, Alb, EGF, HDL and LDL receptors for receptor mediated transcytosis (Simionescu et al., 2009).

Endocytosis by LSECs involves the degradation and metabolism of blood borne waste proteins and xenobiotics *via* lysosomal formation; this property is also referred to as scavenging. There are five scavenging receptor classes expressed on LSECs (A, B, E, H and L) that mediate this process. In two recent reviews, Pandey et al. (2020) and Bhandari et al. (2021) highlighted the scope of molecules that are scavenged by these receptors. These receptors mediate the LSECs uptake and degradation of blood borne waste molecules and colloids under 200 nm. Previously we investigated whether it was possible to target specific clearance pathways *in vitro* and *in vivo* using biopolymer coatings to facilitates endocytosis or avoidance of liver phagocytic cells and scavenger endothelial cells with hepatocyte-only uptake (Hunt et al., 2020). Coating with formaldehyde-treated serum albumin (FSA) was increased scavenger endothelial cell uptake *in vitro* and *in vivo via* stabilins 1 and 2. In the *in vivo* context, heparin coating facilitated uptake by hepatocytes but not KCs or LSECs (Hunt et al., 2020).

## Cellular Uptake and Aging

Hepatic cellular uptake of many drugs and NPs is dependent on the rate of supply to the liver. This is influenced by hepatic blood flow, the rate of transfer from blood to hepatocytes (involving both passive and active transcytosis across the endothelium), and the metabolic rate or 'intrinsic clearance' of hepatocytes (i.e., flow capacity, dissolution capacity and metabolism capacity respectively) (McClean and Le Couteur, 2004).

Aging is associated with a 20–50% reduction in hepatic blood flow which will reduce the hepatic clearance and first pass metabolism of flow-dependent substrates (McClean and Le

Couteur, 2004). The passive transfer from the blood to hepatocytes is affected by defenestration of LSECs, endothelial thickening and collagen deposition, collectively referred to as pseudocapillarization (Le Couteur et al., 2008). These aging changes also reduce the hepatic clearance of flow-limited substrates. This may be an advantage for orally administered NPs given in old age, because lower doses will generate similar concentrations as obtained at younger ages. For example, we observed that old mice had double the systemic concentration of orally administered Ag<sub>2</sub>S QDs than young mice despite the same dose (Hunt et al., 2020; Hunt et al., 2021). The hepatic clearance of substrates that undergo capacity-limited clearance will also be reduced in old age as a result of reductions in liver mass and enzyme activity (Le Couteur et al., 2002; Le Couteur et al., 2008).

Active transporters are affected by aging within the liver. Decreased activity of P-gp has been shown in the liver, but not the endothelium or intestines (Warrington et al., 2004). The expression of LSEC SRH-2 (stabilin-2), the main scavenger receptor on LSECs, remains largely unchanged with age, but LSECs have a slightly reduced ability to endocytose ligands *via* this receptor in LSECs from old rats (Simon-Santamaria et al., 2010). The SLC transporters OCTs, OCTNs, NPTs, OATPs and APTs are decreased with age (Fu et al., 2012; Cogger et al., 2013; Hou et al., 2014; Wu and Lin, 2019). Broad inhibition of these soluble transporters inhibits PLGA NPs, QD uptake into hepatocytes (Press et al., 2014; Zhang et al., 2018; Hunt et al., 2021). Overall, aging may impair NP uptake and clearance by the MPS and liver resulting in greater bioavailability in older patients.

## METABOLISM

Drug metabolism usually results in an active drug becoming inactive and water soluble, therefore able to be excreted in urine or bile. Drug metabolism occurs *via* two pathways: phase I pathways (oxidation and reduction, hydrolysis) and phase II pathways (conjugation with water soluble substrates such as glutathione, sulfate, acetate and glucuronide) (Klotz, 2009). While the majority of metabolism occurs in the liver, CYP3A4 is also present in the intestine, kidneys, lung, brain, placenta and lymphocytes (Anzenbacher and Anzenbacherova, 2001). The majority of hepatic metabolism is *via* P450 enzymes CYP3A4 (52%), CYP2D6 (30%) and CYP2C9/10/19 (11%) (Anzenbacher and Anzenbacherova, 2001).

Nanotherapeutics and NPs present a different challenge in terms of their metabolism as they have rapid cellular uptake *via* the MPS (phagocytic cells) and LSECs, followed by phagolysosome/lysosome mediated degradation. Enzymatic metabolism also occurs during this process and NPs are oxidized and reduced to improve their solubility for renal and biliary clearance.

Degradation of nanomaterials by phagocytic cells (MPS) is promoted following opsonization facilitated by C3b or/and IgG. Phagocytosis is promoted these opsonins proteins *via* either complement receptor or FcγR signaling in KCs, neutrophils and macrophages. The formation of the phagosome differs

between the two signaling cascade. Complement receptor signaling facilitating activation of Rho GTPase, ROCK, Arp 2/3 complexes and mDia (Uribe-Querol and Rosales, 2020), while FcγR signaling activates the Src family kinases leading to the activation of PI3K, PKC, Rac and ERK (Uribe-Querol and Rosales, 2020). The phagosome facilitate internalization *via* modification to the actin cytoskeleton. Once internalized the phagosome transitions to a phagolysosome *via* the accumulation of V-ATPase, NADPH oxidase complexes, myeloperoxidase and hydrolytic enzymes, lysozymes and lipases (Uribe-Querol and Rosales, 2020). V-ATPase promotes an acidic environment (pH 4.5) (Marshansky and Futai, 2008), oxidase complexes produce reactive oxygen species (ROS) and superoxide (O<sub>2</sub><sup>-</sup>) (Babior, 2004; Minakami and Sumimoto, 2006). O<sub>2</sub><sup>-</sup> dismutates to hydrogen peroxide, which based on co-enzymes (myeloperoxidase) can produce other radical ions (Cl<sup>-</sup>) (Nauseef, 2014). In addition to the phagolysosome, phagocytic cells also engender an inflammatory environment *via* ROS generation, secretion of inflammatory mediators, degranulation of antimicrobial molecules and production of cytokines (Uribe-Querol and Rosales, 2020).

The degradation *via* phagolysosomes of different NP materials has been reported. Degradation of carbon nanotubes is mediated *via* hypochlorite and peroxydinitrite (myeloperoxidase-induced) pathways (Ding et al., 2017). MnO<sub>2</sub> NPs are completely decomposed to form free Mn<sup>2+</sup> ions that are readily excreted *via* the kidneys (Liu et al., 2017). Calcium based NPs are stable under neutral pH but disintegrate at pH 5.0 (Ueno et al., 2005). Polystyrene and TiO<sub>2</sub> NPs activate the production myeloperoxidases for ROS mediated degradation (Sanfins et al., 2018).

Comparatively, Au NPs present a challenge for degradation as chemically Au is inert; yet it has been shown to promote a localised inflammatory response (Oh and Park, 2014). This inflammatory response is mediated by the phagocytic cell attempting to degrade Au NPs. Exocytosis of non-degraded Au NPs from macrophages is mediated by the presence of surface coatings (e.g., PEGylation) or, as is the case with conventional Au NPs, they have a long retention within the phagocytic cell (Oh and Park, 2014). To examine the long term retention, Kolosnjaj-Tabi et al. (2015) examined the 1 year fate of Au and Fe coated Au NPs *in vivo*. Conventional Au NPs demonstrated a 30% retention 1 day after injection that reduced to 12% after 1 year within the liver; comparatively Fe coatings demonstrated 80% retainment for up to 1 week and 7% retainment over 1 year. Fe NPs are degraded by phagocytic cells and are used clinically in the form of ferric carboxymaltose, Fe sucrose and Fe dextran as therapeutics for Iron deficiency (Lyseng-Williamson and Keating, 2009). Differences in their cellular uptake into phagocytic cells have been observed with Fe sucrose demonstrating complement mediated uptake (Faria et al., 2019). These studies highlight the importance of degradability of the metal NPs.

Metal NPs also present toxicity challenges highlighted by a recent review (Egorova and Ananikov, 2017). It was concluded that the toxicity of a metal NP depends on multiple factors (oxidation state, ligand, solubility and morphology) that

contribute to potential toxic effects on both humans and the environment (Egorova and Ananikov, 2017). During the course of absorption-distribution-metabolism-excretion (ADME), metal NPs will have multiple modifications and should be considered holistically. Heavy metal poisoning in humans is due to aluminium, arsenic, beryllium, cadmium, copper, chromium, iron, lead, lithium, manganese, mercury, nickel, silver, thallium, tin and zinc (Ibrahim et al., 2006). To address the risk of heavy metal poisoning there are standardised guidelines about the concentration of each metal that can be present in water, air and food products. These guidelines should be considered when developing metal based nanotherapeutics, with alternative materials to be used even for very low clinical risk metals.

LSECs have a critical role in degradation of nanomaterials (Poon et al., 2019) due to their immense endocytic capacity (Sørensen et al., 2012). Using a variety of receptors [mannose receptor, stabilins 1/2 (a.k.a. SRH1/2), and endocytic Fcγ2B receptor] LSECs recognize and internalize pathogen associated molecular patterns, cellular debris and immune complexes [including small circulating IgG complexes (Malovic et al., 2007)]. For example, LSEC clear gram amounts of denatured collagen and procollagen I N-terminal peptides arising from bone turnover *via* the mannose receptor (Mousavi et al., 2007) and stabilin-2/SRH-2 (Mccourt et al., 1999), respectively. LSECs also clear BK polyoma virus (Simon-Santamaria et al., 2014), bacteriophages (Øie et al., 2020) and adenoviruses (Ganesan et al., 2011). The degradation capacity of LSECs is dependent on the circulating lysosomal enzymes that are taken up by LSECs *via* mannose receptor mediated endocytosis for the hydrolysis of endocytosed proteins, lipids and nucleic acids (Elvevold et al., 2008). We have shown selective targeting of LSECs for degradation of Ag<sub>2</sub>S QDs conjugated to a scavenger receptor binding ligand *in vivo* (Hunt et al., 2020). Attachment of this ligand lead to a 5-fold increase in the endocytic uptake rate compared to unconjugated Ag<sub>2</sub>S QDs, with no differences in whole animal excretion rate or volume observed.

An important point is that phagocytic cells and LSECs degrade or solubilize NPs with the aim of creating a soluble and excretable product that may be cleared by the kidneys or transported by soluble carriers (SLCs and SLCOs) to the bile. Problematically, even if the base nanomaterial is degraded it may still be reactive and able to promote cellular stress and damage. This action is most clearly identified with metal NPs and highlighted by the spectrum of metals that induce toxicity. For example, CeSe/ZnS cause high levels of oxidative stress, cellular damage and DNA damage compared to Ag and carbon-based NPs (Malaviya et al., 2019).

## Metabolism and Aging

Aging affects phagocytic cells of the MPS, LSECs, IgG and complement pathways. KCs and macrophages have increased cell numbers, reduced phagocytosis capacity but increased production of cytokines, particularly IL-6 (Hunt et al., 2019). Within the liver this local inflammatory environment is coupled with senescence-associated secretions from hepatocytes to drive increased recruitment and activation

of immune cells (Hunt et al., 2019). LSECs undergo pseudocapillarization loss of fenestrations, deposition of a basement membrane and increased cell adhesion markers (facilitates increased KC attachment) (Hunt et al., 2019) which inhibits passive clearance leading to increased drug concentrations in systemic circulation (Mitchell et al., 2011).

Circulating IgG is substantially reduced with aging (Buckley and Dorsey, 1970) due to glycosylation of IgG impairing its function (Gudelj et al., 2018). This may reduce opsonization of NPs in aging animals but has not been investigated to date.

Complement pathways also demonstrated broad changes with aging. The complement cascades *via* the classical, mannan and alternative pathways both adapt and change with age (Gaya Da Costa et al., 2018). NPs, particularly >30 nm anionic liposomes, have been observed to act *via* all three pathways *via* different proteins within the protein corona. In the classical pathway IgG acting as the initiator; in the mannan pathway lectin proteins conjugate to mannose; and in the indirect pathway *via* direct C3b attachment to NPs (La-Beck et al., 2021). With age, classical and alternative pathways have increased activity (Gaya Da Costa et al., 2018). The mannan pathway has been shown to have decreased activity (Gaya Da Costa et al., 2018).

Overall, there are multiple factors that may affect the metabolism of nanotherapeutics in aging models and older patients. The reduction in phagocytosis by phagocytic cells and passive and active clearance by LSECs suggest prolonged circulation of nanotherapeutics may occur with aging. This conclusion is supported by our study showing a doubling of circulating concentrations of QD conjugated metformin in old mice compared to younger mice (Hunt et al., 2020; Hunt et al., 2021). Reduced circulating IgG and serum albumin will further aid this delay in optimization or conjugation of NPs *in vivo*. Given the broad changes in the complement cascade with aging, future studies need to investigate aged animal models with multi-morbidities to determine the efficacy of nanotherapeutics prior to clinical use particularly from an immunological focus.

## URINARY AND BILIARY ELIMINATION

Urinary clearance can occur *via* passive or active processes. Passive clearance occurs *via* glomerular filtration and is dependent on the drug/nanotherapeutic solubility, size (hydrodynamic diameter <6 nm) and protein binding status (albumin or corona coated materials are not readily excreted). Passive clearance is dependent on glomerular filtration rate (GFR) or the flow of plasma from the glomerulus into the Bowman's space.

Therapeutics may also enter the renal tubules by active secretion across the renal proximal tubule cells facilitated by SLC and adenosine triphosphate (ATP)-binding cassette (ABC) transporters (Yin and Wang, 2016). These transporters include OCT2, OCT 1/3, OAT2, OATP4C (SLCO4C), MATE1/2, OCTN1/2, P-gp, MRP2/4, OAT4, OAT10 and URAT1 (Yin and Wang, 2016). There is substantial overlap between active urinary secretion transporters and biliary excretion transporters.

Hepatic biliary transport is mediated by MDR1, MDRP, P-gp, ABCB11, ABCG2, aquaporin 8/9, BCRP and MATE1 to facilitate waste transportation into the bile cannula (Jetter and Kullak-Ublick, 2020). Hepatic bile is composed of water, bile salts, cholic acid and chenodeoxycholic acid produced from CYP450 mediated metabolism of cholesterol bilirubin and fats.

Collectively these channels contribute to the active excretion of drugs, xenobiotics and nanomaterials; the overlap between the two sites is due to the enzymatic breakdown occurring in a broad range of areas (intestine, kidneys, lung, brain, placenta and lymphocytes) with soluble blood born waste materials continuously being excreted (Anzenbacher and Anzenbacherova, 2001).

Urinary and biliary excretion of NPs has been shown to occur in a size dependent manner with Au NPs (Poon et al., 2019). Au NPs under 6 nm are more readily cleared *via* urinary excretion (Poon et al., 2019). NPs larger than this demonstrates a size dependent relationship with active excretion *via* biliary clearance with smaller NPs (down to 7–8 nm) having greater biliary clearance, because they have less KC uptake as well as undergo passive filtration through the fenestrated surface of the liver endothelium (Tsoi et al., 2016; Poon et al., 2019).

Several types of NPs have very high biliary clearance. Seo et al. (2015) showed that injected 38 nm oleic acid micelles capped with polysorbate 60 had 85% biliary clearance within 72 h. Souris et al. (2010) demonstrated high biliary clearance with mesoporous silica NPs conjugated with indocyanine. Lastly, we have demonstrated high biliary clearance with orally administered 7 nm Ag<sub>2</sub>S QDs (Hunt et al., 2020).

Active elimination *via* different transporters has been shown for nanotherapeutics and more broadly, for xenobiotics. P-gp also known as multi drug resistant protein 1 (MDR1) or ABCB1, is the most common xenobiotic transporter and is expressed in most tissues (Jetter and Kullak-Ublick, 2020). P-gp is also highly expressed in some cancer cells and there have been several strategies to overcome P-gp facilitated removal of nanotherapeutics from targeted cancers (Niazi et al., 2016). A potential side effect of these strategies may be reduced long-term clearance and broader distribution of these NPs. P-gp is expressed 7-fold higher in the GI tract and blood brain barrier compared to hepatocytes (Cascorbi, 2011). Impaired P-gp clearance may contribute to long term retention and toxicity of NPs.

Other transporters with demonstrable roles in biliary excretion include OAT2 (SLC22A7) MATE1 And Aq9. OAT2 mediates the uptake of xenobiotics (Jetter and Kullak-Ublick, 2020), while MATE1 (SLC47A1) acts as a scavenger for P-gp to facilitating its excretion into the bile (Jetter and Kullak-Ublick, 2020). Finally, Aq9 permits the diffusion of mannitol and critically PEG below 900 Da for urinary and biliary excretion (Javitt, 2014).

These active uptake pathways, particularly the SLC channels, are present throughout the body and most heavily in the GI tract and liver. This almost ubiquitous presence highlights a critical issue with targeting and utilizing these channels to improve bioavailability as there is likely increased clearance with greater precision targeting of these transporters. Still, this challenge presents an opportunity as drug delivery may be

facilitated during this rapid clearance if the therapeutic agent can be released during a short time frame.

## Clearance and Aging

With age GFR (passive filtration of ultra-particles from the plasma) is reduced by 15–40% (McClean and Le Couteur, 2004). Renal plasma flow also decreases with age at a faster rate than GFR as a result of increased renal vascular resistance (Fliser et al., 2005). Age-related changes in renal function are a very important consideration when calculating the drug dosage given to older people (such as aminoglycosides, digoxin, and dabigatran). This is further confounded by prevalent coexistent comorbidities (diabetes, hypertension and heart failure) or nephrotoxic drugs (non-steroid anti-inflammatory).

Active transporters (as highlighted in the *cellular uptake* section and above) decrease with age. Differences between renal and hepatic changes with age are evident for P-gp which showed decreased expression in kidneys and reduced activity in the liver (Warrington et al., 2004). Within the kidney, decreased expression in old age was observed for OCT2, OATP4C1, Mdr1b and MATE1; while OAT1 and 3, OCT1, BCRP, MRP2 and 4 and MATE2 show no changes with age (Xu et al., 2017). Within the liver, of the 101 xenobiotic-processing genes, 40–43% of transporters are downregulated with age (Fu et al., 2012). This was contributed to reduced phase 1 metabolism. Increased expression was only observed for OAT2 and GSTM2 within the liver (Fu et al., 2012). These studies highlight that organic cation transporters consistently demonstrated downregulation in multiple organs. As highlighted in the *absorption* section metformin is a primary drug candidate to demonstrate the benefits of nano-drug efficacy in aging. We demonstrated that there are improved pharmacokinetics and pharmacodynamics when metformin is conjugated to QDs aging animals (Hunt et al., 2020; Hunt et al., 2021). We suggest that other OCT1/2 transporter drugs (e.g., anti-viral medications: zidovudine, acyclovir and ganciclovir) are ideal candidates for nano-formulation to improve the efficacy of drug treatment in older patients. Previously we have also reviewed other potential drug therapeutics for hepatic specific targeting with nanotechnology (Hunt et al., 2018).

## NANOTHERAPEUTICS AND AGING

Even though older people are the major users of therapeutic agents, there are very few studies examining the effects of aging on the pharmacology of nanomedicines. One study reported the effects of aging on the biodistribution of citrate coated Fe NPs (10 nm). Old mice had greater Fe NP retention in the liver and kidney while young mice predominantly retained Fe NPs within the spleen. Comparing old and young mice, greater iron NP uptake was observed in the lung, brain, spleen and liver of older mice, however no differences in clinical or histological outcomes were observed between the age groups (Pinheiro et al., 2019). Another study examined silica NPs to limit age-related bone loss (Weitzmann et al., 2015). We studied the effects of aging on orally

administered metformin or NMN coated Ag<sub>2</sub>S QDs (Hunt et al., 2020; Hunt et al., 2021). Overall, these few studies have not detected any major age-related toxicity concerns. However, NP toxicity studies in 18 month old mice found a loss of stress responses in older animals (Zhang et al., 2012; Pomatto et al., 2018). Investigation into the effects of aging on the pharmacology of NPs and subsequent efficacy and safety in clinical trials will be critical for any nanotherapeutics that will be used in older patients.

## REGULATORY CONSIDERATIONS

Nanomaterials, similarly to linkers, antibodies, peptides and viral vectors, change the efficacy and toxicity of drugs. This is important because nanomaterial may address the efficacy and toxicity weaknesses of novel drug formulations that have failed in phase 2/3 clinical trials (Harrison, 2016). The limited translation of nanomedicines further highlights the difficulty in achieving this task (He et al., 2019). Regulatory issues with nanotechnology are currently addressed by classifying nanotherapeutics or nano-drugs as drugs themselves, regardless of whether the nanotechnology is proposed to be inactive or active in their actions within the body. FDA guidelines suggest, like for all drug formulations, that early phase *in vivo* studies require haematology, clinical chemistry, gross pathology, immune response, tissue weights and histological examination. These existing guidelines may create difficulties with a nano-drugs designed to have prolonged circulation and be resistant to metabolism and clearance. Potential accumulation in off target tissues and reduced biodegradability may be significant barriers to regulatory approval. Additionally, the use of nanomaterials that have a highly reactive surface chemistry may contribute to ROS generation, particularly with heavy metals (Malaviya et al., 2019). This presents great difficulty in regulatory assessments as nanomaterials, despite their advantages based on their size and reactivity, are effectively drugs themselves with a broad range of side effects. It is therefore of critical importance that nano absorption, distribution, cellular uptake, metabolism, drug action and removal be understood and potentially provided with separate regulatory processes specifically designed with the properties of nanomaterials in mind.

With the above considerations nanotechnology should be considered an enabling technology platform that can have broad applications from biotechnology, bio-medicine, information technology and cognitive technology. Previously, regulatory regimes worldwide were decentralized, fragmented and presented gaps and challenges (Devasahayam, 2019; Allan et al., 2021). On the other hand, as reviewed by Devasahayam (2019) the current legal metronomy within the global setting is adequate to respond to the measurements required for nanotechnology (nanometrometry). In a recent review Halamoda-Kenzaoui et al. (2021) described the regulatory framework and technical approaches required for safety and quality control of nanotherapeutics. Both the European Medicine Agency (EMA) and FDA have released several guidance documents that outline the parameters to consider,

including ICH guidelines for medical products and CEN/ISO standards (Halamoda-Kenzaoui et al., 2021). Due to the complex nature and propensity to interact with biological systems additional assessments are required. Of critical interest have been the key discussion points of this review, phagocytosis, inflammation and complement activation. Relating to ADME challenges for *in silico* and humanized biodistribution remain key areas to address. As highlighted by this review within older patients there will be additional changes in ADME that cannot be predicted by young animal models. Finally, additional studies must also be performed in aging animal models to aid existing PBPK models.

## CONCLUSION

The aim of this review was to provide an overview of the broad changes in drug absorption, distribution, cellular uptake, metabolism, drug action and removal facilitated by nanomaterials and how these systems are affected by aging. We have identified the areas of overlap and advantages for nanotherapeutics in aging (Table 1). Nanotherapeutics provide the opportunity to greatly enhance absorption of therapeutics in older people with impaired uptake of specific soluble transporter drugs, delayed uptake time and reduced absorption of weakly basic drugs. These benefits are afforded because nanotherapeutics are broadly absorbed by multiple soluble transporters and utilize macropinocytosis and clathrin endocytosis to increase drug bioavailability. Additionally, nanotherapeutics demonstrate conventional and highly specific distribution and clearance by

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the liver, potentially bypassing recognized age-related impairments in first pass metabolism, reductions in serum albumin, blood flow and passive clearance pathways. Challenges for nanotherapeutics in older patients will be based on the local inflammatory profiles within the liver and in circulation. Broad differences in complement, IgG and protein binding may drastically shift the efficacy and long-term toxicity of nanotherapeutics in older patients and highlights the need to investigate aging animal models and relevant metabolic pathways in older people to better understand how nanotechnology will translate into patients and the clinic.

## AUTHOR CONTRIBUTIONS

NH composed the original draft; VC, DL, PM, and ZK revised and edited the draft. All authors have reviewed and approved submission.

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