



Preliminary Outcomes of Combined Treadmill and Overground High-Intensity Interval Training in Ambulatory Chronic Stroke

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Purpose: Locomotor high-intensity interval training (HIIT) is a promising intervention for stroke rehabilitation. However, overground translation of treadmill speed gains has been somewhat limited, some important outcomes have not been tested and baseline response predictors are poorly understood. This pilot study aimed to guide future research by assessing preliminary outcomes of combined overground and treadmill HIIT.

Materials and Methods: Ten participants >6 months post-stroke were assessed before and after a 4-week no-intervention control phase and a 4-week treatment phase involving 12 sessions of overground and treadmill HIIT.

Results: Overground and treadmill gait function both improved during the treatment phase relative to the control phase, with overground speed changes averaging 61% of treadmill speed changes (95% CI: 33–89%). Moderate or larger effect sizes were observed for measures of gait performance, balance, fitness, cognition, fatigue, perceived change and brain volume. Participants with baseline comfortable gait speed <0.4 m/s had less absolute improvement in walking capacity but similar proportional and perceived changes.

Conclusions: These findings reinforce the potential of locomotor HIIT research for stroke rehabilitation and provide guidance for more definitive studies. Based on the current results, future locomotor HIIT studies should consider including: (1) both overground and treadmill training; (2) measures of cognition, fatigue and brain volume, to complement typical motor and fitness assessment; and (3) baseline gait speed as a covariate.

Keywords: locomotion, gait, aerobic exercise, brain, magnetic resonance imaging

INTRODUCTION

Limited walking capacity (decreased speed and endurance) is a common and persistent problem after stroke (1–5), that can be caused by neurologic motor impairments and by aerobic deconditioning (6, 7). Stroke rehabilitation guidelines recommend walking exercise at higher intensities to address both of these issues and improve walking capacity (6, 8, 9).

Thus, locomotor high-intensity interval training (HIIT) is a promising new intervention for stroke rehabilitation (10, 11). This method involves bursts of fast walking alternated with recovery periods to enable vigorous aerobic intensities, using burst and recovery intervals ranging from short (e.g., 30 s) to long (e.g., 3–4 min) (12). Initial longitudinal stroke studies suggest that both short-interval and long-interval locomotor HIIT are feasible, can improve gait function and exercise capacity (13–20), and could be more efficacious than conventional moderate-intensity exercise (15, 16).

However, locomotor HIIT has only been tested on a treadmill, and treadmill-only exercise often has limited translation to overground gait improvements after stroke (15, 21, 22). Based on the neuroplasticity principle of task-specificity (23), we proposed combining overground and treadmill HIIT to improve overground translation (15, 24). This method showed feasibility in ambulatory chronic stroke (24), but no previous studies have reported outcome changes after a protocol involving overground HIIT. Such information could help determine whether further protocol refinement may be needed before considering an efficacy trial.

Another limitation to prior post-stroke HIIT studies is that they have mostly included only gait and exercise capacity outcomes. HIIT also has the theoretical potential to facilitate other important aspects stroke recovery, such as cognition, fatigue and brain health (25–27). In addition, there is reason to suspect that some of these potential HIIT effects could be greater than those elicited by moderate intensity exercise (25, 26). For example, HIIT has been shown to elicit greater acute increases in some circulating neurotrophins than moderate intensity exercise after stroke (28, 29). However, no longitudinal stroke studies have assessed changes in cognition, fatigue or brain volumes after locomotor HIIT. Thus, it remains unknown which outcome measures, if any, might be sufficiently responsive to consider including in future studies.

Additionally, there is limited available information about baseline patient characteristics associated with responsiveness to HIIT post-stroke. Previous studies have shown that stroke survivors with slower baseline walking speed tend to have less absolute improvement in gait function with various forms of training (30–33). Yet, it is uncertain if this generalizes to HIIT and whether proportional change or perception of improvement are similar between participants with different baseline walking speeds. This knowledge could help guide selection of eligibility criteria, stratification factors and covariates in future studies.

The primary aim of this pilot study was to assess overground translation of treadmill speed gains after combined overground and treadmill HIIT in chronic hemiparetic stroke. Participants >6 months post-stroke had a no-intervention control phase

followed by 12 sessions of combined overground and treadmill HIIT (using both short and long interval HIIT). We hypothesized that at least 50% of treadmill speed gains during the treatment phase would translate into overground gait, on average. The second aim of this study was to evaluate responsiveness of different outcome measures across various domains, including gait, balance, exercise capacity, cognitive, fatigue/subjective and brain volume measures, to guide selection of outcome measures for future trials. We hypothesized that standardized effect size estimates in each outcome domain would be ≥ 0.4 between the treatment and control phases, justifying further study (34). The third aim was to examine the potential for differences in responsiveness between participants with faster vs. slower baseline gait speed (34). Compared with participants who had baseline comfortable gait speed ≥ 0.4 m/s, we hypothesized that those with speed < 0.4 m/s would have less absolute improvement in 6-min walk distance (30), but similar proportional change and perception of improvement.

MATERIALS AND METHODS

The study providing data for this analysis was approved by institutional review boards, preregistered on ClinicalTrials.gov (NCT02858349) and performed in a cardiovascular stress laboratory, MRI research center and rehabilitation research laboratory from July 2016 to December 2017. Some of the methods and baseline data from this study have been previously described in manuscripts addressing different aims from the current report (24, 35).

Participants

Participants with ischemic or hemorrhagic stroke and control participants without stroke were recruited from the community and provided written informed consent. To be eligible, participants had to be 30–90 years old, MRI compatible, able to communicate with investigators and correctly answer consent comprehension questions, able to perform mental imagery (36), without recent history of drug/alcohol abuse or significant mental illness, and not pregnant. Participants with stroke had to meet the following additional criteria: unilateral stroke in middle cerebral artery territory experienced > 6 months prior to enrollment; walking speed < 1.0 m/s on the 10 m walk test (37); able to walk 10 m over ground with assistive devices as needed and no physical assistance; no evidence of significant arrhythmia or myocardial ischemia on treadmill ECG stress test, or significant baseline ECG abnormalities that would make an exercise ECG uninterpretable (38); no recent cardiopulmonary hospitalization; no significant ataxia or neglect (NIHSS item score > 1) (39); no severe lower extremity (LE) hypertonemia (Ashworth > 2) (40); no major post-stroke depression (PHQ-9 ≥ 10) (41) in the absence of management of the depression by a health care provider (42); not participating in physical therapy or another interventional research study; no recent paretic LE botulinum toxin injection; and no concurrent progressive neurologic disorder or other major conditions that would limit capacity for improvement. Control participants had to be a demographic match for a

participant with stroke (same sex, age difference ≤ 5 years) without any current neurologic, orthopedic or medical condition affecting gait.

Study Design

After baseline assessment, each participant with stroke had a 4-week control phase with no-intervention, followed by a 4-week treatment phase with 12 sessions of locomotor HIIT, approximately 3x/week. In alternating order, 6 of these sessions used short-interval HIIT while the other 6 used long-interval HIIT, with the first session randomized across participants. Outcome measures were assessed before the control phase (PRE), after the control phase (4WK), and after the 4-week treatment phase (8WK). Control participants had baseline testing (PRE) only.

Screening

Eligibility determination was based on medical history review and physical assessment. Participants with stroke also had treadmill acclimation and graded exercise testing (GXT) with electrocardiography for screening, as previously described (15, 43). For the GXT, treadmill speed was held constant at a pre-determined individualized value, while incline was increased 2–4% until volitional fatigue, severe gait instability or a cardiovascular safety limit (38, 44).

Outcome Testing

The following outcome measures were assessed for participants with stroke at PRE, 4WK and 8WK by a blinded physical therapist who had not been involved with the participant's treatment. For the 4WK and 8WK testing, the testing therapist did not know whether the participant had received any treatment in the previous phase. Participants used any habitual orthotic and assistive devices during gait testing and were guarded as needed, but only assisted if required to prevent a fall or injury. These measures were assessed for control participants one time only (PRE).

Gait Function

- The 10-m walk test (45) was performed twice at comfortable speed and twice at fastest speed with trial pairs averaged for analysis to calculate comfortable and fastest overground gait speeds.
- The 6-min walk test was performed and total distance was recorded (46).

Spatiotemporal Gait Parameters

- Two passes were performed at comfortable speed across a sensor-embedded electronic walkway (47, 48) and were combined for analysis, with parameters averaged across gait cycles, including: cadence, step time symmetry, step lengths and symmetry and single-limb support times and symmetry. Symmetry indices were calculated as: $(1 - |\text{Paretic} - \text{Nonparetic}| / (\text{Paretic} + \text{Nonparetic})) * 100\%$; with possible values ranging from 0 to 100%, where 0% means complete asymmetry and 100% means perfect symmetry.

The following outcome measures were assessed for participants with stroke by the treating physical therapist and a research assistant (both unblinded), on a separate day from the gait measures above, at each testing time point. Control participants were also assessed on these measures at PRE except as indicated below.

Treadmill Gait Function

- Fastest safe treadmill speed was evaluated with a rapid acceleration test, where speed was increased by 0.1 mph every 5 s until the participant could no longer maintain the speed or had severe gait instability. This test was not done for controls.

Standing Balance

- The NIH Toolbox Standing Balance Test Age 7+ (49) was performed using the NIH Toolbox iPad application and BalancePod iPod touch application with recommended equipment (49). Fully corrected T scores were used for analysis. These scores are referenced to persons with the same age, gender, race/ethnicity and educational attainment as the participant from the NIH Toolbox nationally representative normative sample (50–52), with a mean of 50 and a standard deviation of 10. Thus, a score of 40 would represent worse balance than the average American with similar demographics, one standard deviation below the mean.

Exercise Capacity

These assessments were done only for participants with stroke. A GXT was performed following the same protocol as the screening GXT, but with a metabolic cart and facemask for gas exchange analysis (53). This was done on a separate day from the screening GXT at PRE. Fifteen minutes after the GXT, participants performed another exercise test for verification of peak exercise capacity. This test started at the participant's pre-determined fastest safe speed and 2–4% grade. Incremental grade then speed decreases were done as little as needed to enable continued walking as fast as possible for 3 min, with close guarding.

- The oxygen consumption rate (VO_2) at the ventilatory threshold during the GXT was determined using a combination of the V-slope and ventilatory equivalents methods, as previously described (54).
- The highest VO_2 and heart rate (HR) values from either the GXT or 3-min test were recorded as $\text{VO}_{2\text{peak}}$ and HR_{peak} .

Cognition

- The Free and Cued Selective Reminding Test (FCSRT) (55, 56) was administered and the free recall score was used to assess episodic memory. The FCSRT was found to be the most accurate clinical test for identifying prodromal Alzheimer's disease among patients with mild cognitive impairment and had an optimal free recall cutoff score of <17 (on a scale from 0 to 48) (57). This test was not done for controls.
- The following tests from the NIH Toolbox Cognition Battery (58) were administered using the NIH Toolbox iPad application: Flanker inhibitory control and attention test (assesses attention and executive functioning), picture

sequence memory test (episodic memory), list sorting working memory test (working memory), dimensional change card sort test (executive function) and pattern comparison processing speed test (processing speed). The NIH Toolbox also provides a fluid cognition composite score combining the results from each of these tests. Fully corrected T scores were used for analysis.

Subjective Measures

These assessments were done only for participants with stroke.

- The Patient Reported Outcomes Measurement Information System (PROMIS®) Fatigue (59, 60) short form 8a v1.0 (PROMIS-Fatigue) was administered, and raw scores were converted to T scores according to the scoring manual. These T scores are referenced to the entire U.S. general population PROMIS calibration sample (61), with a mean of 50 and a standard deviation of 10. Thus, a score of 60 would represent greater fatigue than the average American, one standard deviation above the mean.
- The Stroke and Aphasia Quality of Life Scale 39 (62) was administered and a total score from 1 to 5 was calculated by averaging all items, where a score of 1 on each item strongly endorses (definitely yes) and a score of 5 strongly denies (definitely no) a particular problem or difficulty.
- Global Ratings of Change (GROC) (63) for overall stroke recovery, walking ability and fitness were administered at 4WK and 8WK (rating *change* is not applicable at PRE). Participants were asked to rate the change in each characteristic from the time that they began the study until that testing session, using a 15-point scale ranging from -7 (a very great deal worse) to 0 (about the same) to $+7$ (a very great deal better) (63). Scores of $+1$ (hardly any better at all) to $+3$ (somewhat better) are considered to represent small improvement, while scores of $+4$ (moderately better) to $+5$ (a good deal better) represent moderate improvement and scores of $+6$ (a great deal better) and $+7$ represent large improvement (63).

Brain Volume

Structural MRI acquisition and preprocessing has been previously described in detail (35). Briefly, T1-weighted (T1w) brain images were obtained with a 3.0T Philips Ingenia MRI system (1 mm isotropic resolution; TR, 8.1 ms; TE, 3.7 ms; flip angle, 8° ; SENSE factor 2). FSL software (64) was used for bias field correction, tissue type segmentation and non-linear registration to the MNI152 template, using a lesion mask to improve registration for participants with stroke. Lesioned voxels in the native-space T1w image were temporarily filled with MNI template voxels (65) to enable automated structure labeling with FreeSurfer software (66). Lesioned voxels were then masked out of any structure labels.

- Supratentorial brain volume (excluding brainstem and cerebellum) was calculated bilaterally and for the ipsilesional and contralesional hemibrain by summing the number of voxels in gray and white matter structure labels and multiplying by the voxel size. These volumes were adjusted for head size by first calculating the scaling factor from

the participant's skull to the MNI152 template skull (larger scaling factor = smaller participant skull) (67), then effectively regressing the scaling factor out of the volumetric data (68, 69). This adjustment used the formula: $Adjusted\ Volume_i = Volume_i - \beta_{control} \left(Scaling\ Factor_i - \overline{Scaling\ Factor}_{control} \right)$; where the subscript "i" represents values from the individual participant scan, $\beta_{control}$ is the slope of the regression line from using the scaling factor to predict the volume of interest in the control group, and $\overline{Scaling\ Factor}_{control}$ is the mean scaling factor in the control group (69). For bilateral, ipsilesional and contralesional (supratentorial) brain volumes, $\beta_{control}$ values were -712.7 , -358.4 , and -354.3 , respectively (all $p < 0.0001$). $\overline{Scaling\ Factor}_{control}$ was 1.27.

Locomotor HIIT Treatment Protocol

The treatment protocol and training intensity data have been previously reported in detail (24). Briefly, each session included a 3-min warm up (overground walking at $\sim 40\%$ HR reserve [HRR]), 10 min of overground HIIT, then 20 min of treadmill HIIT, followed by another 10 min of overground HIIT and a 2-min cool down (overground walking at $\sim 40\%$ HRR). HRR bpm targets were calculated by: $(HR_{peak} - HR_{resting}) \times \%HRR\ target + HR_{resting}$ (38). Participants wore habitual orthotic devices, started with habitual assistive devices during overground training and used a fall protection harness during treadmill training. Physical assistance was only provided if needed to avoid a fall or injury. During overground training, participants walked back and forth in a corridor, using visual feedback about distance covered and verbal encouragement to maximize speed each burst. Assistive device and/or pattern were progressed if it enabled achievement of faster speeds.

Each participant alternated between short and long-interval HIIT sessions. Short-interval HIIT sessions involved 30 s bursts at maximum safe speed alternated with 30–60 s resting recovery periods (15). Burst speed was progressed as able throughout the session to maintain constant challenge. Long interval HIIT sessions involved 3–4 min bursts at a target HR of $90\% HR_{peak}$ alternated with 2–3 min active recovery periods at a target of $70\% HR_{peak}$. Speed was continually adjusted as needed to achieve and maintain the target HR.

During short-interval HIIT sessions, actual mean training speed was 0.75 m/s overground and 0.90 m/s on the treadmill, while mean training HR was 78 and $83\% HR_{peak}$, respectively (24). During long-interval HIIT sessions, mean speed was 0.67 m/s overground and 0.51 m/s on the treadmill, while mean training HR was 81 and $82\% HR_{peak}$, respectively (24).

Safety Monitoring

Adverse events (AEs) were defined as any undesirable change in participant health (regardless of severity or suspected relationship with the study procedures) and were systematically assessed. Participants with stroke were asked about AEs at each visit, were specifically queried about soreness/pain, fatigue, nausea, lightheadedness, falls and injuries, and were continuously monitored for AEs throughout each testing and treatment session.

Data Analysis

Baseline measures were compared between stroke survivors and controls using independent *t*-tests and Fisher exact tests. Baseline values were also expressed as a percentage of normative demographic-predicted values for comfortable gait speed (37), 6-min walk test (70), HR_{peak} (71, 72), and VO_{2peak} (73). AEs were categorized by relationship to the intervention, type, and severity (74). To estimate group-level outcome changes within and between phases for the stroke group, mixed effects general linear models were used with the outcome of interest (e.g., comfortable gait speed) as the dependent variable, a fixed (categorical) effect for time (PRE, 4WK, 8WK) and an unstructured covariance matrix to account for repeated measures within the same participant. SAS version 9.4 was used for analysis.

For hypothesis 1 (at least 50% of treadmill speed gains would translate into overground gait), we calculated change in fastest 10-m walk test speed during the treatment phase, expressed it as a percentage of change in fastest treadmill speed and averaged across participants.

For hypothesis 2 (standardized effect sizes in each outcome domain would be ≥ 0.4), we calculated Cohen's *d* effect sizes (75) for each outcome measure during the treatment phase by dividing the mean change by the standard deviation of change and multiplying by $\sqrt{2}$. We also performed the same calculation for the treatment vs. control phase comparison using individual values for treatment phase change minus control phase change.

For hypothesis 3 (faster walkers at baseline would have greater absolute improvement in 6-min walk distance, but similar proportional change and perception of improvement), we used the mixed effects model described above and added fixed effects for baseline comfortable gait speed subgroup (<0.4 vs. ≥ 0.4 m/s) (30) and its interaction with time. Preliminary subgroup estimates were calculated for treatment phase changes in gait function (absolute and percent changes) and subjective measures. For comparison with the gait speed subgroup effect, we also used the same modeling approach to test whether treatment phase change in 6-min walk distance was moderated by age (dichotomized using a median split) or sex.

Target Sample Size

Based on previous study aims (35), the target sample size was 10 stroke survivors and 10 controls with complete data. At the 0.05 significance level, this sample size provides 80% power to detect a within-group change Cohen's *d* effect size as small as 1.00 (very large) and a between group (stroke vs. control) Cohen's *d* effect size as small as 1.32. Therefore, this pilot study was only powered to statistically detect very large or greater effects.

RESULTS

Ten participants with stroke and 10 healthy controls were enrolled (Figure 1). All participants completed the trial, with no missing visits. Compared with controls, participants with stroke were significantly less independent with ambulation, used more orthotic and assistive devices and had lower gait speed and 6-min walk distance (Table 1). Participants with stroke also had significantly lower values for various spatiotemporal gait

parameters, standing balance, fluid cognition, and brain volume (Table 2). No serious AEs occurred throughout the study. Mild and moderate AEs are reported in Table 3.

During the control phase, participants with stroke showed no significant change in gait function measures, spatiotemporal gait parameters, standing balance, peak heart rate, most cognitive measures, all subjective measures, and brain volume (Table 2). Meanwhile, significant increases were found in ventilatory threshold, VO₂-peak, and Flanker scores. During the treatment phase, participants with stroke showed significant improvements in all gait function measures, paretic step length, paretic single support time, single-support time symmetry, ventilatory threshold, VO₂-peak, FCSRT score, PROMIS-Fatigue score and most subjective change ratings (Table 2 and Figure 2). Compared with the control phase, treatment phase changes were significantly greater for all gait function measures, paretic single support time, PROMIS-Fatigue score, and most subjective change ratings (Table 2).

When testing hypothesis 1, improvement in fastest overground gait speed during the treatment phase (+0.16 m/s [95% CI: 0.08–0.25 m/s]) averaged 61% [33–89%] of the improvement in fastest treadmill speed (+0.29 m/s [0.16–0.42 m/s]).

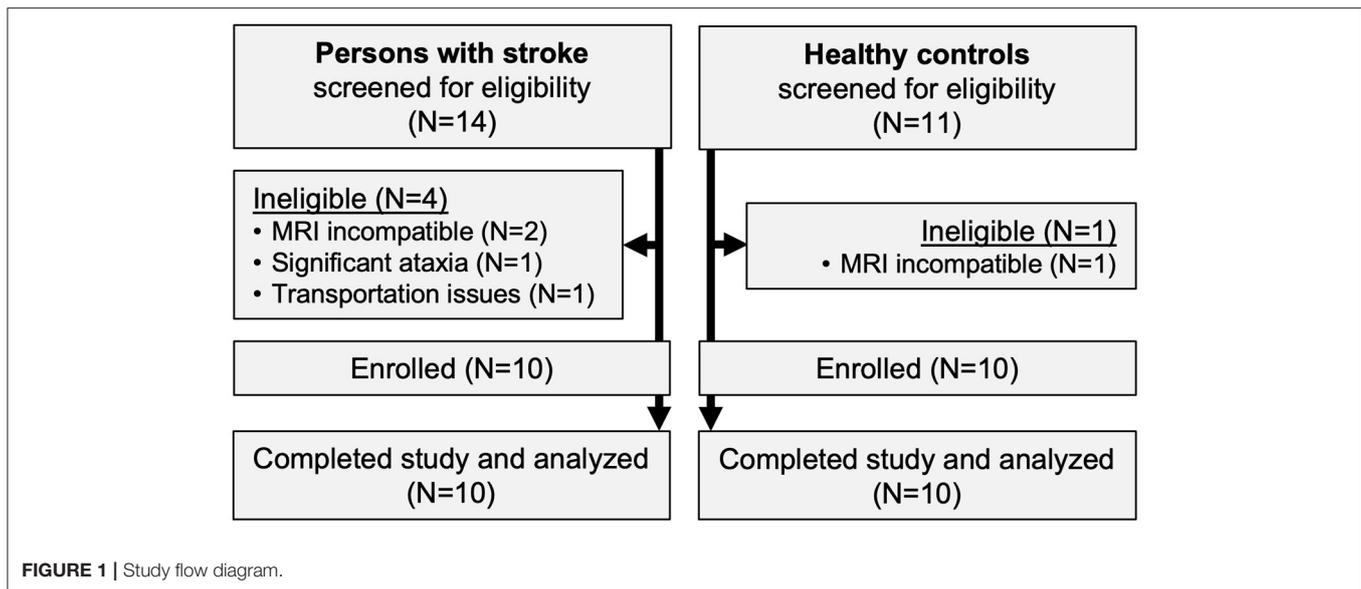
When testing hypothesis 2, the following outcome measures had standardized effect sizes ≥ 0.4 for both the treatment phase and the treatment vs. control phase comparison (Table 4): all gait function measures, cadence, paretic, and non-paretic step length, paretic single-support time, single support symmetry, NIH Toolbox standing balance test, ventilatory threshold, FCRST free recall, NIH Toolbox pattern comparison processing speed test, PROMIS-Fatigue, all subjective measures and all brain volumes.

When testing hypothesis 3, participants with baseline comfortable gait speed ≥ 0.4 m/s had significantly greater absolute improvement in 6-min walk distance than participants with baseline speed <0.4 m/s (Table 5). Mean percent change in 6-min walk distance was greater in the slower baseline subgroup, but not significantly different. The slower baseline subgroup also had a significantly greater percent improvement in fastest treadmill speed. Both subgroups reported similar levels of improvement on subjective measures.

Age and sex did not significantly moderate change in 6-min walk distance ($p = 0.33$ and 0.81 , respectively). When subgrouping based on a median split of age, participants <60 years old improved by +38 m [16–60 m] and participants ≥ 60 years old improved by +24 m [2–46 m]. When subgrouping based on sex, females improved by +29 m [3–55 m] and males improved by +33 m [11–54 m].

DISCUSSION

This pilot study aimed to guide future locomotor HIIT research in chronic hemiparetic stroke by: (1) assessing overground translation of treadmill speed gains with a refined treatment protocol that included both overground and treadmill training; (2) evaluating responsiveness of different outcome measures across domains, including gait, balance, fitness, cognition,



fatigue/subjective, and brain volume; and (3) examining the potential for moderation by baseline gait speed. Non-stroke control participants were also included to facilitate interpretation of baseline measures. Participants with stroke showed expected differences from controls, with lower function or greater impairment in each domain tested. Consistent with our hypotheses, we found that: (1) improvement in fastest overground gait speed averaged $>50\%$ of the improvement in fastest treadmill speed (61%); (2) some outcome measures in each domain showed standardized effect sizes ≥ 0.4 ; and (3) participants with faster baseline gait speed appeared to have greater absolute improvement in 6-min walk distance, yet similar proportional change and perceived improvement. Due to very large observed effect sizes, some variables also exhibited statistically significant improvement during the treatment phase, significant effect moderation by baseline gait speed and significant treatment vs. control phase comparisons.

Using combined treadmill and overground HIIT, the percentage of treadmill speed gains that translated into overground gait in this study was double that observed in our previous study using treadmill-only HIIT (15) (61 vs. 30%). While comparisons across studies can be misleading (e.g., due to differences in prognosis or treatment delivery between study samples), these likely sources of confounding should have mostly worked against the current study. For example, the current sample had lower mean baseline comfortable gait speed than our previous study (0.41 vs. 0.63 m/s), indicative of worse prognosis for overground gait improvement. Also, the current treatment protocol did not attempt to reduce treadmill handrail support to approximate the dynamic balance challenge of overground gait as we had done previously. Thus, the magnitude of the between-study difference and the likely direction of potential confounding suggest that overground HIIT may have been an important addition to the intervention protocol to continue in future studies. While translation was still not complete (i.e.,

100%), we suspect that it may be close to the feasible limit, because the fixed balance and posture support provided by an optimally-positioned treadmill handrail cannot be entirely replicated with an assistive device during overground gait.

Our findings may also be useful for guiding selection of outcome measures in future post-stroke HIIT research and related intervention studies. It has been suggested that only interventions and outcome measures with preliminary Cohen's d effect sizes $\geq |0.4|$ should be advanced toward efficacy trials in neurologic rehabilitation (34). Based on this criterion, the results in **Table 4** indicate that some outcomes in each domain (gait function, spatiotemporal gait parameters, balance, exercise capacity, cognition, subjective measures, and brain volume) had sufficient responsiveness to consider including in future related studies. Large effect sizes ($\geq |0.8|$) were observed for both the treatment phase and treatment vs. control phase comparison for all gait function measures, select gait parameters (paretic step length, paretic single support time, and single support symmetry), ventilatory threshold, PROMIS-Fatigue, and subjective change ratings. Moderately large effect sizes ($\geq |0.6|$) were found for cadence, NIH Toolbox standing balance test, FCSRT free recall, and brain volume. The estimated effect sizes should be viewed with caution due to the small sample size, which makes them more prone to fluctuate with the addition of more data. However, these preliminary results may assist with prioritization of outcome measures in future studies. They also provide justification for adding cognitive, fatigue and brain volume measures to the typical motor function and fitness assessment batteries used in locomotor HIIT research.

Unexpectedly, a few outcome measures had significant changes during the no-intervention control phase, when participants were expected to be stable. This included ventilatory threshold, VO_2 peak, and the NIH Toolbox Flanker inhibitory control and attention test. While these results could plausibly be false positives due to the number of variables tested,

TABLE 1 | Participant characteristics.

	Control participants (N = 10)	Participants with stroke (N = 10)	Stroke vs. control p-value
Age, years	58.9 (7.8)	59.8 (6.8)	0.79
Females, N (%)	4 (40%)	4 (40%)	1.00
Body mass index (kg/m ²)	30.8 (4.2)	30.2 (4.2)	0.76
Left hemispheric stroke, N (%)	N/A	5 (50%)	
Stroke chronicity, years	N/A	2.4 (1.7)	
Lesion volume, mL	N/A	121.7 (105.0)	
Comorbid conditions, N (%)			
Diabetes mellitus	2 (20%)	1 (10%)	1.00
Hypertension	4 (40%)	6 (60%)	0.66
History of percutaneous coronary intervention	0 (0%)	2 (20%)	0.47
History of myocardial infarction	0 (0%)	1 (10%)	1.00
History of seizure	0 (0%)	2 (20%)	0.47
Functional ambulation category, N (%)			0.003
2: Dependent, Level I	0 (0%)	5 (50%)	
3: Dependent, Supervision	0 (0%)	2 (20%)	
≥4: Independent, Level Surfaces	10 (100%)	3 (30%)	
Used ankle foot orthosis, N (%)	0 (0%)	8 (80%)	0.0007
Assistive device, N (%)			0.003
None	10 (100%)	3 (30%)	
Narrow-based quad cane	0 (0%)	2 (20%)	
Wide-based quad cane	0 (0%)	4 (40%)	
Pyramid cane/hemi-walker	0 (0%)	1 (10%)	
Comfortable overground gait speed, m/s	1.36 (0.16)	0.41 (0.33)	<0.0001
Comfortable overground gait speed, % predicted	100.5 (7.3)	30.4 (24.2)	<0.0001
6-min walk test, m	537 (77)	156 (147)	<0.0001
6-min walk test, % predicted	101.6 (15.7)	28.2 (24.8)	<0.0001
Peak oxygen consumption rate, mL/kg/min	N/T	13.1 (2.8)	
Peak oxygen consumption rate, % predicted	N/T	54.4 (14.0)	

Values are mean (SD) or N (%). P-values are from independent T-tests or Fisher exact tests. N/A, not applicable; N/T, not tested.

they could also indicate learning or conditioning effects from repeated testing. This emphasizes the importance of appropriate control groups in future studies, even in chronic stroke.

The current findings also suggest that future locomotor HIIT studies should consider baseline gait speed as a potential stratification factor for randomization and/or a potential covariate in statistical models. Consistent with previous gait training research post-stroke (30–33), we found significantly greater absolute improvement in 6-min walk distance among participants with baseline gait speed ≥0.4 m/s vs. <0.4 m/s, despite having extremely low power to test for such interactions. Further, this subgroup effect is not likely to be explained

TABLE 2 | Adverse events (AEs) among participants with stroke (N = 10; total visits = 200)*.

	No. (%) of participants with AE	Total number of AEs
All	8 (80%)	55
Related to intervention	5 (50%)	18
-Grade 1 (mild)	4 (40%)	15
-Grade 2 (moderate)	3 (30%)	3
-Grade 3–5 (severe-death)	0 (0%)	0
-Cardiac disorder	0 (0%)	0
-Soreness/pain	4 (40%)	10
-Fatigue	2 (20%)	3
-Nausea	0 (0%)	0
-Lightheadedness	2 (20%)	5
-Other nervous system	0 (0%)	0
-Fall	0 (0%)	0
-Other	0 (0%)	0
Possibly related or unrelated to intervention	8 (80%)	37
-Grade 1 (mild)	8 (80%)	34
-Grade 2 (moderate)	3 (30%)	3
-Grade 3–5 (severe-death)	0 (0%)	0
-Cardiac disorder	0 (0%)	0
-Soreness/pain	7 (70%)	14
-Fatigue	0 (0%)	0
-Nausea	0 (0%)	0
-Lightheadedness	3 (30%)	6
-Other nervous system	0 (0%)	0
-Fall	5 (50%)	11
-Headache	2 (20%)	2
-Increased knee hyperextension	1 (10%)	1
-Joint stiffness	1 (10%)	1
-Infection (common cold)	1 (10%)	1
-Excision of ingrown toenail	1 (10%)	1
-Other	0 (0%)	0

*There were no adverse events among control participants.

by age or sex, which showed weaker and non-significant subgroup effects.

Based on these results, it could be argued that future studies should exclude persons with speed <0.4 m/s. However, we would advocate against this for several reasons. First, the 95% confidence interval for change in 6-min walk distance included the possibility of a meaningful effect even in this subgroup. Proportional changes and perceived changes in this subgroup were also comparable or better than the faster walking subgroup. In addition, the treatment protocol had a relatively short 4-week duration, and it remains unknown whether persons with baseline speed <0.4 m/s may be more responsive with a longer locomotor HIIT protocol. Finally, there are limited available interventions with evidence of efficacy for persons with severe gait impairment in chronic stroke. Thus, we would recommend continued inclusion of persons

TABLE 3 | Baseline measures and outcome changes.

	Control data (N = 10)	Stroke baseline (N = 10)	Stroke control phase change	Stroke treatment phase change
Gait function				
Comfortable overground gait speed, m/s	1.36 (0.16)	0.41 (0.33)*	0.00 [−0.05, 0.05]	0.13 [0.05, 0.21]†
Fastest overground gait speed, m/s	1.94 (0.24)	0.57 (0.56)*	0.00 [−0.03, 0.04]	0.16 [0.08, 0.25]†
Fastest treadmill speed, m/s	N/T	0.72 (0.51)	−0.01 [−0.07, 0.05]	0.29 [0.16, 0.42]†
6-minute walk test, m	537 (77)	156 (147)*	−2 [−13, 9]	31 [16, 47]†
Spatiotemporal gait parameters				
Cadence, steps per minute	109.0 (7.4)	62.9 (31.5)*	−0.5 [−5.8, 4.8]	12.6 [−2.2, 27.4]
Step time symmetry, %	98.9 (0.8)	74.8 (18.3)*	−7.5 [−22.4, 7.4]	3.6 [−10.6, 17.8]
Paretic [‡] step length, cm	71.7 (9.5)	39.0 (11.8)*	−3.6 [−9.7, 2.5]	7.5 [2.1, 12.8]
Non-paretic [‡] step length, cm	70.4 (10.4)	30.5 (15.9)*	−0.4 [−4.4, 3.5]	2.4 [−1.2, 6.0]
Step length symmetry, %	98.1 (1.5)	81.4 (22.7)*	−7.0 [−28.8, 14.8]	6.0 [−12.9, 25.0]
Paretic [‡] single support, % gait cycle	35.6 (2.2)	17.3 (9.1)*	−1.4 [−3.9, 1.2]	3.1 [0.4, 5.8]†
Non-paretic [‡] single support, % gait cycle	35.1 (2.1)	26.7 (9.8)*	1.7 [−5.4, 8.8]	2.5 [−3.2, 8.2]
Single-support symmetry, %	98.1 (3.4)	77.2 (16.3)*	−8.2 [−20.9, 4.4]	6.4 [1.0, 11.8]
Standing balance , NIH Toolbox T score	40.8 (4.5)	29.1 (7.4)*	−1.0 [−4.5, 2.5]	2.3 [−0.1, 4.7]
Exercise capacity				
Ventilatory threshold, mL/kg/min	N/T	9.8 (2.6)	0.6 [0.1, 1.1]	1.8 [0.6, 3.0]
Peak oxygen consumption rate, mL/kg/min	N/T	13.1 (2.8)	1.4 [0.1, 2.7]	1.8 [1.2, 2.4]
Peak heart rate, bpm	N/T	142 (18)	6 [−4, 16]	0 [−10, 10]
Cognition				
FCSRT free recall, 0–48	N/T	24.2 (13.6)	−0.8 [−3.9, 2.3]	2.5 [0.1, 4.9]
NIH Toolbox fluid cognition composite, T score	47.9 (5.8)	27.6 (10.9)*	1.4 [−1.2, 4.0]	1.3 [−1.5, 4.1]
Flanker inhibitory control and attention, T score	45.8 (6.9)	33.0 (6.1)*	2.7 [0.2, 5.2]	−0.9 [−5.9, 4.1]
Picture sequence memory, T score	49.5 (12.2)	42.6 (9.1)	1.6 [−4.0, 7.2]	3.3 [−1.9, 8.5]
List sorting working memory, T score	48.9 (6.1)	38.4 (13.6)*	2.0 [−5.8, 9.8]	−0.5 [−8.4, 7.4]
Dimensional change card sort, T score	49.3 (6.2)	38.2 (10.6)*	−1.6 [−5.7, 2.5]	0.1 [−7.1, 7.3]
Pattern comparison processing speed, T score	50.3 (11.6)	25.1 (9.7)*	−0.3 [−4.7, 4.1]	2.6 [−0.2, 5.4]
Subjective measures				
PROMIS-Fatigue, T score [§]	N/T	51.1 (8.8)	2.9 [−0.4, 6.2]	−4.8 [−9.1, −0.6]†
Stroke and Aphasia Quality of Life Scale, 1–5	N/T	3.3 (1.0)	0.0 [−0.3, 0.3]	0.4 [−0.1, 0.9]
GROC-Overall stroke recovery, −7 to +7	N/A	N/A	1.0 [−1.2, 3.2]	3.9 [2.8, 5.0]†
GROC-Walking ability, −7 to +7	N/A	N/A	0.5 [−1.9, 2.9]	4.4 [2.7, 6.1]†
GROC-Fitness, −7 to +7	N/A	N/A	0.5 [−1.5, 2.5]	4.1 [2.8, 5.4]†
Supratentorial brain volume, mL[^]				
Ipsilesional hemibrain [‡]	1,004 (40)	856 (88)*	−4.8 [−17.3, 7.7]	7.4 [−3.5, 18.4]
Ipsilesional hemibrain [‡]	503 (21)	370 (79)*	−1.9 [−9.7, 6.0]	3.1 [−2.7, 9.0]
Contralesional hemibrain [‡]	501 (20)	486 (32)	−2.9 [−8.4, 2.6]	4.3 [−1.3, 9.8]

Values are mean (SD) or estimate [95% CI]. *Significant ($p < 0.05$) difference between stroke and control participants. †Significant difference between intervention and control phases. ‡Matched side for control group. §Lower score = less fatigue. ^Adjusted for head size. PROMIS, Patient Reported Outcomes Measurement Information System; GROC, global rating of change; FCSRT, free and cued selective reminding test; N/A, not applicable; N/T, not tested.

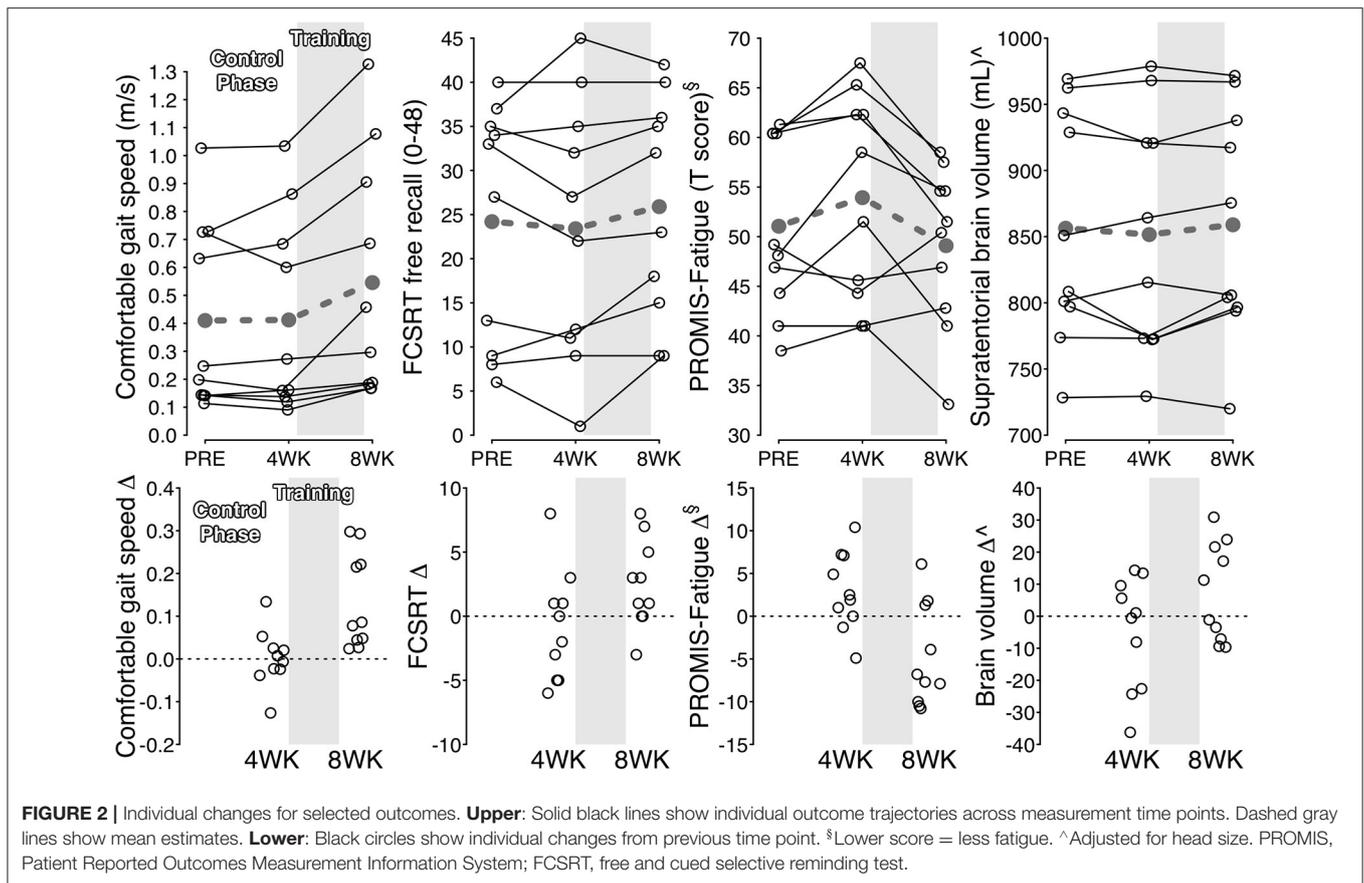
with comfortable gait speed <0.4 m/s in future studies, while incorporating baseline gait speed as a stratification factor and covariate.

The observed safety data in this study were similar to our previous research on locomotor HIIT and moderate-intensity exercise in chronic stroke (15). No serious AEs occurred and the frequency and type of mild/moderate AEs were consistent with expectations for exercise testing and training in a population with substantial pre-existing health conditions (76). When considering the current results in combination with previous studies, the safety profile of locomotor HIIT appears to be

reasonable to date, but continued monitoring is needed given the relatively low numbers of participants tested and the generally unsystematic collection and reporting of AE data in the literature.

Strengths and Limitations

Strengths of this study include: recruitment of a well-defined sample of stroke survivors with substantial gait limitations (representative of clinical rehabilitation) and well-matched controls; systematic refinement of the treatment protocol; use of a control phase before treatment to address spontaneous



recovery or repeated testing effects; detailed assessment of many outcome domains at multiple time points, including several novel measures for this area of research; systematic progression toward efficacy and effectiveness trials with early consideration of optimal outcome measures and covariates; complete follow up of all participants without any missing visits; and systematic safety data collection and reporting.

The main limitation is that this study was not designed to test treatment efficacy or effectiveness, but rather to guide future research on locomotor HIIT post-stroke. All results should be viewed as preliminary in light of the small sample size, lack of a randomized crossover order or control group, lack of an active control intervention and lack of adjustment for multiple statistical comparisons. The small sample size and intentional homogeneity of some participant characteristics also make it difficult to know how well the results may generalize to the broader population of stroke survivors (e.g., persons with stroke outside of the middle cerebral artery distribution). Another limitation was that we were unable to assess any potential outcome differences between short-interval and long-interval HIIT, since each participant performed both types in alternating sessions. This was done to increase the validity of short vs. long-interval HIIT intensity comparisons for a previous analysis (24). The lack of rater blinding for some outcome measures also increases risk of bias. This was partially mitigated by using standardized protocols and automated procedures where

feasible. For the subjective outcomes, participants were asked to answer as honestly as possible even if they perceived no changes or negative changes, and were told that our priority was getting accurate information to guide future research. However, we cannot rule out the possibility that some may have still reported more positive results to avoid social discomfort.

Summary of Implications for Future Studies

The current findings add to a growing body of evidence showing promising potential for locomotor HIIT to improve stroke rehabilitation outcomes (13–20). Powered randomized trials with clinically representative samples are now needed to definitively test the efficacy and effectiveness of locomotor HIIT in comparison with alternative strategies for optimizing recovery. It is also important for these studies to systematically collect and report adverse event data, so that the risk-benefit ratio of post-stroke HIIT can be appropriately assessed. Our team is currently conducting an early-phase multi-center trial toward this end (77).

The results of the present report suggest that future locomotor HIIT studies should consider adding overground HIIT rather than solely training on the treadmill. For overground gait testing, the 6-min walk test was the most responsive measure and is recommended as a primary outcome. For exercise capacity testing, ventilatory threshold was the most responsive (for treatment vs. control phase comparisons) and is recommended as a secondary outcome. Several novel outcomes now also

TABLE 4 | Cohen's d standardized effect size estimates (N = 10).

	Treatment phase	Treatment – control phase
Gait function		
Comfortable overground gait speed	1.70	1.61
Fastest overground gait speed	1.91	1.60
Fastest treadmill speed	2.33	2.01
6-min walk test	2.03	1.90
Spatiotemporal gait parameters		
Cadence	0.86	0.73
Step time symmetry	0.26	0.48
Paretic [‡] step length	1.42	1.01
Non-paretic [‡] step length	0.67	0.44
Step length symmetry	0.32	0.33
Paretic [‡] single support	1.18	1.07
Non-paretic [‡] single support	0.45	0.07
Single-support symmetry	1.20	0.93
Standing balance, NIH Toolbox	0.98	0.66
Exercise capacity		
Ventilatory threshold	1.55	0.91
Peak oxygen consumption rate	2.92	0.28
Peak heart rate	0.02	–0.57
Cognition		
FCSRT free recall	1.04	0.66
NIH Toolbox fluid cognition composite	0.47	–0.03
Flanker inhibitory control and attention	–0.18	–0.55
Picture sequence memory	0.64	0.19
List sorting working memory	–0.06	–0.18
Dimensional change card sort	0.01	0.18
Pattern comparison processing speed	0.94	0.49
Subjective measures		
PROMIS-Fatigue [§]	–1.15	–1.14
Stroke and Aphasia Quality of Life Scale	0.73	0.55
GROC-Overall stroke recovery	3.46	1.26
GROC-Walking ability	2.63	1.72
GROC-Fitness	3.13	1.57
Supratentorial brain volume		
Ipsilesional hemibrain [‡]	0.54	0.43
Contralesional hemibrain [‡]	0.78	0.78

[‡]Matched side for control group. [§]Lower score = less fatigue. [∧]Adjusted for head size. PROMIS, Patient Reported Outcomes Measurement Information System; GROC, global rating of change; FCSRT, free and cued selective reminding test.

appear to warrant further consideration, including measures of balance (NIH Toolbox standing balance test), memory (FCSRT free recall), processing speed (NIH Toolbox pattern comparison processing speed test), fatigue (PROMIS-Fatigue), quality of life (Stroke and Aphasia Quality of Life Scale), perceived change (in overall stroke recovery, walking ability and fitness) and brain volume (ipsilesional and contralesional). Of course, adding outcome measures also increases study burden (for participants, study teams and funding bodies), so the current preliminary effect sizes may also be useful to assist with prioritization.

TABLE 5 | Treatment phase changes by baseline comfortable gait speed subgroup.

	<0.4 m/s (N = 6)	≥0.4 m/s (N = 4)
Gait function		
Comfortable overground gait speed, m/s	0.09 [–0.01, 0.18]	0.20 [0.09, 0.32]
Comfortable overground gait speed, % baseline	61.8 [11.9, 111.7]	25.0 [–36.1, 86.1]
Fastest overground gait speed, m/s	0.11 [0.01, 0.21]	0.25 [0.13, 0.37]
Fastest overground gait speed, % baseline	62.8 [14.1, 111.5]	24.3 [–35.4, 83.9]
Fastest treadmill speed, m/s	0.28 [0.10, 0.45]	0.31 [0.10, 0.53]
Fastest treadmill speed, % baseline	81.2 [46.9, 115.5]	26.2 [–15.8, 68.2]*
6-min walk test, m	17 [6, 28]	53 [39, 66]*
6-min walk test, % baseline	37.1 [23.5, 50.7]	18.8 [2.2, 35.5]
Subjective measures		
PROMIS-Fatigue, T score [§]	–5.5 [–11.4, 0.4]	–3.8 [–11.0, 3.4]
Stroke and Aphasia Quality of Life Scale, 1–5	0.5 [–0.1, 1.2]	0.1 [–0.7, 0.9]
GROC-Overall stroke recovery, –7 to +7	4.5 [3.1, 5.9]	3.0 [1.3, 4.7]
GROC-Walking ability, –7 to +7	4.8 [2.5, 7.1]	3.8 [0.9, 6.6]
GROC-Fitness, –7 to +7	3.7 [1.9, 5.4]	4.8 [2.6, 6.9]

Values are the mean estimate [95% CI]. *Significant difference between gait speed subgroups. [§]Lower score = less fatigue. PROMIS, Patient Reported Outcomes Measurement Information System; GROC, global rating of change.

Lastly, the present results suggest that persons with severe gait limitations (comfortable speed <0.4 m/s) should continue to be included in future locomotor HIIT studies, while stratifying the randomization and/or analysis by baseline gait speed.

CONCLUSIONS

Locomotor HIIT is a promising intervention for stroke rehabilitation. Future studies on this topic should consider: (1) including both overground and treadmill training; (2) measuring cognition, fatigue and brain volume, in addition to typical gait and fitness assessment; and (3) stratifying randomization by baseline gait speed and including it as a covariate in statistical models.

DATA AVAILABILITY STATEMENT

The original contributions presented in the study are included in the article/**Supplementary Material**, further inquiries can be directed to the corresponding author/s.

ETHICS STATEMENT

The studies involving human participants were reviewed and approved by University of Cincinnati IRB. The patients/participants provided their written informed consent to participate in this study.

AUTHOR CONTRIBUTIONS

PB, JV, KD, and BK: conceptualization, funding acquisition, and supervision. PB: data curation, formal analysis, software, visualization, and writing—original draft. PB, SD, VS, ES, and DW: investigation. PB and JV: project administration. PB, JV, KD, BK, RSa, and DC: resources. All authors: methodology and writing—review and editing. All authors contributed to the article and approved the submitted version.

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SUPPLEMENTARY MATERIAL

The Supplementary Material for this article can be found online at: <https://www.frontiersin.org/articles/10.3389/fneur.2022.812875/full#supplementary-material>

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