



Astragalus Polysaccharides/Chitosan Microspheres for Nasal Delivery: Preparation, Optimization, Characterization, and Pharmacodynamics

OPEN ACCESS

Saisai Wang^{1†}, Yuqing Sun^{2†}, Jingjing Zhang³, Xiaoming Cui¹, Zhilu Xu¹, Dejun Ding^{1,4,5}, Limin Zhao^{6*}, Wentong Li^{4,5,7*} and Weifen Zhang^{1,4,5*}

Edited by:

Apostolos Zarros,
University of Glasgow,
United Kingdom

Reviewed by:

Jessica Amber Jennings,
The University of Memphis,
United States

Nadeem Irfan Bukhari,
University of the Punjab, Pakistan

*Correspondence:

Limin Zhao
13869651631@163.com
Wentong Li
liwentong11@163.com
Weifen Zhang
zhangwf@wfmcc.edu.cn

[†]These authors have contributed
equally to this work

Specialty section:

This article was submitted to
Experimental Pharmacology
and Drug Discovery,
a section of the journal
Frontiers in Pharmacology

Received: 14 October 2019

Accepted: 20 February 2020

Published: 18 March 2020

Citation:

Wang S, Sun Y, Zhang J, Cui X,
Xu Z, Ding D, Zhao L, Li W and
Zhang W (2020) Astragalus
Polysaccharides/Chitosan
Microspheres for Nasal Delivery:
Preparation, Optimization,
Characterization,
and Pharmacodynamics.
Front. Pharmacol. 11:230.
doi: 10.3389/fphar.2020.00230

¹ School of Pharmacy, Weifang Medical University, Weifang, China, ² Department of Otolaryngology, Head and Neck Surgery, Central Hospital of Zibo, Zibo, China, ³ College of Basic Medical, Qingdao Binhai University, Qingdao, China, ⁴ Shandong Engineering Research Center for Smart Materials and Regenerative Medicine, Weifang Medical University, Weifang, China, ⁵ Institute for Smart Materials and Regenerative Medicine, Weifang Medical University, Weifang, China, ⁶ Department of Otolaryngology, Head and Neck Surgery, Affiliated Hospital of Weifang Medical University, Weifang, China, ⁷ Department of Pathology, Weifang Medical University, Weifang, China

Chitosan (CTS) constitutes a promising area in treatment of nose-related diseases as a nasal drug delivery carrier. Astragalus polysaccharide (APS) significantly attenuates eosinophils and neutrophil-dominant airway inflammation, and it has a potential pharmaceutical application in the treatment of severe asthma. The purpose of this work was to prepare APS/CTS microspheres intended for nasal drug delivery by the spray-drying method. The characteristics of APS/CTS microspheres were evaluated by a scanning electron microscope, Fourier transform infrared spectroscopy, differential scanning calorimetry, and *in vitro* drug release. The effect of APS/CTS microspheres on rats with allergic rhinitis (AR) was investigated by eosinophil and neutrophil counts in nasal lavage fluid. Results of SEM showed that microspheres were spherical and wrinkled. *In vitro* release showed that 67.48–93.76% APS was released from APS/CTS microspheres at pH 6.8 within 24 h. The effects showed that APS/CTS microspheres alleviated allergic symptoms and reduced eosinophils infiltration and the expression of interleukin-4 in the nasal mucosa tissue of rats that had no liver and kidney toxicity by hematoxylin-eosin staining observation. In conclusion, these results indicated that APS/CTS microspheres had excellent characteristics for the treatment of AR.

Keywords: Chitosan, Astragalus polysaccharide, spray drying, microspheres, nasal drug delivery

INTRODUCTION

Allergic rhinitis (AR) is a persistent, inflammatory disease characterized by anterior or posterior rhinorrhoea, nasal itching, sneezing, and nasal congestion which reduces people's quality of life and work efficiency (Seidman et al., 2015; Brożek et al., 2017). Currently, antihistamines are the main clinical drugs for AR. However, long-term application of these drugs causes drug-induced rhinitis.

Some drugs are not suitable for children and adolescents. Budesonide suspension combined with terbutaline is less effective in treating asthma at night, and the symptoms easily return (Wang et al., 2019).

Astragalus polysaccharides (APS), a main active extract of *Astragalus membranaceus*, can enhance the immune response by increasing the serum antibody titer and enhancing the secretion of a wide range of cytokines (Tan et al., 2017; Zhou et al., 2017). APS can also regulate the balance of Th1/Th2 cells and inhibit the expression of inflammatory factors and inflammation injury (Liu, 2017; Ren et al., 2018). APS ameliorated palmitate-induced pro-inflammatory responses through AMP-activated protein kinase (AMPK) activity (Lu et al., 2013).

Because nasal mucociliary clearance can reduce the residence time of drugs, microspheres are being considered as a new type of spherical carrier delivery system to overcome rapid mucociliary clearance and increase drug absorption (Ghori et al., 2015; Pandey and Tripathi, 2016). The chitosan (CTS) microsphere is a potential drug carrier and enhances absorption by opening tight junctions between the epithelial cells (Abdel Moez et al., 2014). The CTS microsphere has been used as a promising carrier system for both vaccines and DNA (Islam et al., 2012).

Here, APS/CTS microspheres intended for nasal drug delivery were prepared by a spray-drying method, and characteristics of these microspheres were evaluated. We then explored the toxicity evaluation and therapeutic effects of APS/CTS microspheres on rats with AR.

MATERIALS AND METHODS

Materials

Astragalus polysaccharides (purity = 70%) was provided by Hong Sheng Bio-products Company (Xi'an, China). CTS (deacetylation degree = 96.1%) was obtained from Hai Debei Marine Biotechnology Company (Jinan, China). Glacial acetic acid was kindly supplied by Yantai Shuangshuang Chemical Co., Ltd. (Yantai, China). Ovalbumin (OVA) and phosphate buffered solution (PBS) were obtained from Shanghai Solarbio Biotechnology Co., Ltd. (Shanghai, China). Budesonide was purchased from Jiangsu AstraZeneca Pharmaceutical Co., Ltd. (Jiangsu, China). Pentobarbital sodium was supplied by Beijing Rui Ee Xin De Technology Co., Ltd. (Beijing, China). The DAB kit, Biotinylated goat anti-rabbit IgG kit, and interleukin-4 (IL-4) rabbit anti-rat kit were obtained from Wuhan Boster Biological Technology Co., Ltd. (Wuhan, China). All other chemicals and solvents were analytical reagent grade.

Preparation and Optimization of APS/CTS Microspheres

A predetermined amount of APS (2.831 g) and CTS (5 g) was dissolved in 1,000 mL of 0.5% acetic acid and stirred vigorously for 12 h under room temperature. The solution was filtrated by 0.45 μm micropore film and spray dried by a spray drier (Mini Spray-Dryer, B-290; Büchi Labortechnik AG, Flawil, Switzerland). The optimum parameters for the formulation of APS/CTS microspheres were determined using

an L_9 (3^4) orthogonal design with three levels of four factors: inlet temperature (120, 140, 160°C), feeding rate (3, 5, 7 mL/min), molecular weight of CTS (3.0×10^2 , 5.0×10^2 , and 1.3×10^3 KDa), and APS/CTS ratio (1:3, 1:5, 1:7). The exact compositions and processing parameters of individual samples were summarized in **Supplementary Table 1**. Subsequently, microspheres were collected and stored in desiccators for further analysis.

Characterization of APS/CTS Microspheres

The shape and surface morphology of microspheres were observed by a scanning electron microscope (SEM) (s4500n, Hitachi, Japan). The particle size was determined by a laser diffraction particle size analyzer (Malvern Mastersizer 2000, Malvern Instruments Ltd., United Kingdom). The sample was scanned for percent transmittance in the range of 4,000–500 cm^{-1} by Fourier transform infrared spectroscopy (FTIR) (Perkin-Elmer, Japan). The thermal behaviors of pure APS, CTS and APS/CTS microspheres were determined using differential scanning calorimetry 7020 (DSC 7020) (Hitachi High-tech Science Corporation, Japan). The DSC runs were conducted over a temperature range 25–300°C at a rate of 10°C/min under inert nitrogen atmosphere.

Determination of Yield (YD), Drug Loading (DL), and Encapsulation Efficiency (EE) of APS/CTS Microspheres

Spray-dried microspheres were dissolved in PBS, rotated for 30 min at room temperature, followed by filtering through a 0.45 μm micropore film. The supernatant was then assayed by Ultraviolet spectrophotometry (UV-vis with UV-8000A Spectrophotometer; Shanghai Puxi Instrument Factory, Shanghai, People's Republic of China) at 490 nm. The concentration of APS was calculated according to the standard curve equation (Liu et al., 2017). Each sample was assayed in triplicate. YD, DL, and EE were calculated:

$$\text{YD (\%)} = \frac{C_M}{C_S} \times 100\% \quad (1)$$

$$\text{DL (\%)} = \frac{C_D}{C_M} \times 100\% \quad (2)$$

$$\text{EE (\%)} = \frac{C_E}{C_T} \times 100\% \quad (3)$$

where C_M refers to the total mass of microspheres, C_S refers to total added solid content mass, C_D refers to the mass of APS in the microspheres, C_E refers to the mass of APS encapsulated in the microspheres, and C_T refers to total added APS mass.

In vitro APS Release Studies

The microspheres (25 mg) were suspended in 1 mL of release medium (PBS of pH 6.8) in a dialysis bag and shaken at 100 rpm/min at 37°C. At predetermined time intervals, 1 mL of release medium was withdrawn and replaced with fresh PBS. The amount of APS was measured at 490 nm with an UV-vis.

The cumulative release (CR) of APS was calculated using the equation below [13].

$$\text{CR (\%)} = \sum_{t=0}^{t=\infty} \frac{M_t}{M_0} \times 100\% \quad (4)$$

where M_t refers to the cumulative releases of APS in PBS (pH 6.8) at set time intervals, and M_0 refers to the APS content of APS/CTS microspheres.

Moisture Uptake and Moisture Content

The microspheres (20 mg, W_d) were dried to constant weight under vacuum and stored in desiccators at 40°C and 75% relative humidity (Zhang et al., 2008). The weights of microspheres (W_h) were recorded at the end of different predetermined intervals (0.5, 1, 2, 4, 6, 8, 12, and 24 h). The increase of weight represented the amount of moisture uptake. For moisture content, the samples (20 mg) were tested at a drying temperature of 105°C for 3 h until a constant weight was achieved. Weighing was performed using a digital balance in duplicate, and the moisture absorption rate and moisture content were calculated as below (Liu et al., 2017).

$$\text{Moisture absorption rate (\%)} = \frac{W_h - W_d}{W_h} \times 100\% \quad (5)$$

$$\text{Moisture content (\%)} = \frac{W - W'}{W} \times 100\% \quad (6)$$

where W refers to the mass of microspheres before tested, and W' refers to the mass of samples after drying until the weight difference is less than 0.3 mg in two successive measurements.

Swelling Ratio and Tap Density

The swelling behavior of microspheres was determined by assessing the water uptake. The dried microspheres were weighed (W_d) and immersed in 4 mL of PBS (pH 6.8). The resultant mixture was incubated for 12 h to achieve swelling equilibrium. Then the solution was centrifuged at 3,000 r/min for 30 min, the liquid on the surface of microspheres was removed, and the wetted microspheres were weighed immediately (W_s). The swelling ratio of microspheres was calculated as below (Liu et al., 2017).

$$\text{Swelling ratio (\%)} = \frac{W_s - W_d}{W_d} \times 100\% \quad (7)$$

where W_s represents the weight of swollen microspheres, and W_d represents the weight of dried microspheres.

The bulk density of the microspheres was determined by tap density measurements (Fiegel et al., 2004). Briefly, the microspheres (25–35 mg) were loaded into a glass tube, which was tapped from a predetermined height (14 mm) on a hard bench top for 20 times. The last constant volume of the microspheres was recorded. The density was then calculated as below (Liu et al., 2017).

$$\rho = \frac{m}{V} \quad (8)$$

where ρ refers to the tap density, m refers to the recorded mass of the microspheres, and V refers last constant volume of the microspheres.

Preparation of AR Model Rats and Administration of Test Drugs

All animal procedures were conducted in accordance with the US NIH Guidelines for the Care and Use of Laboratory Animals, and the animal study was approved by the Animal Ethical Committee of Weifang Medical University. A total of 60 healthy Wistar rats (female, 5–6 weeks old, 160–200 g, Shandong Lukang Animal Center, license no., Slxklu no. 2015002; Shandong, China) were obtained. Rats were randomly divided into six groups: the normal group, model group, budesonide group (20 µg/kg), APS/CTS microspheres (low-dose, 5 mg/kg) group, APS/CTS microspheres (medium-dose, 10 mg/kg) group, and the APS/CTS microspheres (high-dose, 15 mg/kg) group. In the sensitization phase, OVA (0.3 mg/mL) with aluminum hydroxide gel (30 mg) were administered to rats by intraperitoneal injection once every other day for a total of 14 days (Daoud et al., 2014). In the challenge phase (day 15–21), bilateral nasal cavities of rats were continuously instilled by 50 µL OVA (25 mg/mL) once a day. Sneezing and scratching were observed within 30 min after each nasal instillation, and rats were then administrated. Rats were administrated from day 22 to day 32. In the model group and normal group, rats were administrated with only sterile normal saline once a day. In the budesonide group, rats were administrated with budesonide at a dose of 20 µg/kg once a day. In the APS/CTS microspheres low, medium, and high-dose group, rats were separately administrated with APS/CTS microspheres at a dose of 5, 10, 15 mg/kg (APS/CTS microspheres suspended in normal saline and nasal dripped with pipette tips) once a day. Except for the normal group, rats of other groups maintained the OVA nasal drops once every other day and nasal administration was performed 20 min before each challenge.

Allergic Symptoms Evaluation of Rats

The allergic symptoms of rats were observed and scored. The rats were observed for sneezing, scratching, and rhinorrhea and scored within 30 min after each challenge or administration. The allergic rat model was considered to be successful when symptom scores were higher than 5 (Senturk et al., 2018). Score 1: the time of sneezing was 1–3 or scratching was 1–5 or reaching the anterior nostril; Score 2: the time of sneezing was 4–10 or scratching was 6–15 or over the anterior nostril; and Score 3: the time of sneezing was more than 10 or scratching was more than 15 or flowing all the face.

Eosinophil and Neutrophil Counts in Nasal Lavage Fluid

At 24 h after the last nasal drop, rats in each group were anesthetized with 0.3% sodium pentobarbital (40 mg/kg). A syringe (1 mL) was inserted into the nasal cavity of rats about 1.5 cm and was fixed, the frog wood anatomy board and rats were inverted, 3 mL sterile normal saline (1 mL/min) was slowly injected into one side of nasal cavity, and lavage fluid was

recovered in the other side. The nasal lavage fluid was centrifuged for 10 min at 4°C, 1,500 rpm/min, and the cell pellet was taken to count the eosinophils and neutrophils (Virtala et al., 2012).

Hematoxylin-Eosin (HE) Staining and Immunohistochemistry

These nasal mucosa tissue specimens and the livers, kidneys, and spleens of rats were fixed in 4% paraformaldehyde for 24 h and cut into suitable size, placed in the embedding box, dehydrated by a serial alcohol gradient, embedded in paraffin wax, and cooled in a refrigerator at 4°C to solidify. Nasal mucosa tissue and viscera specimens were cut into 4 μm thick slices, and these were then dewaxed in xylene, rehydrated by different concentrations of ethanol, washed in distilled water, and stained with HE. These slides were dehydrated with ethanol, incubated in 3% hydrogen peroxide methanol, and then incubated with IL-4 polyclonal antibody (1:100 dilution) overnight at 4°C. This was followed incubation with the horseradish peroxidase labeled secondary antibody. The slides were then stained with DAB kit.

Statistical Analysis

All experiments were performed three times, and the results were reported as mean \pm standard deviations. Statistical analysis was carried out using SPSS19.0 and all statistically significant differences were analyzed by one-way analysis of variance and Newman-Keuls test. In all cases, $p < 0.05$ was considered statistically significant.

RESULTS

Morphology and Particle Size

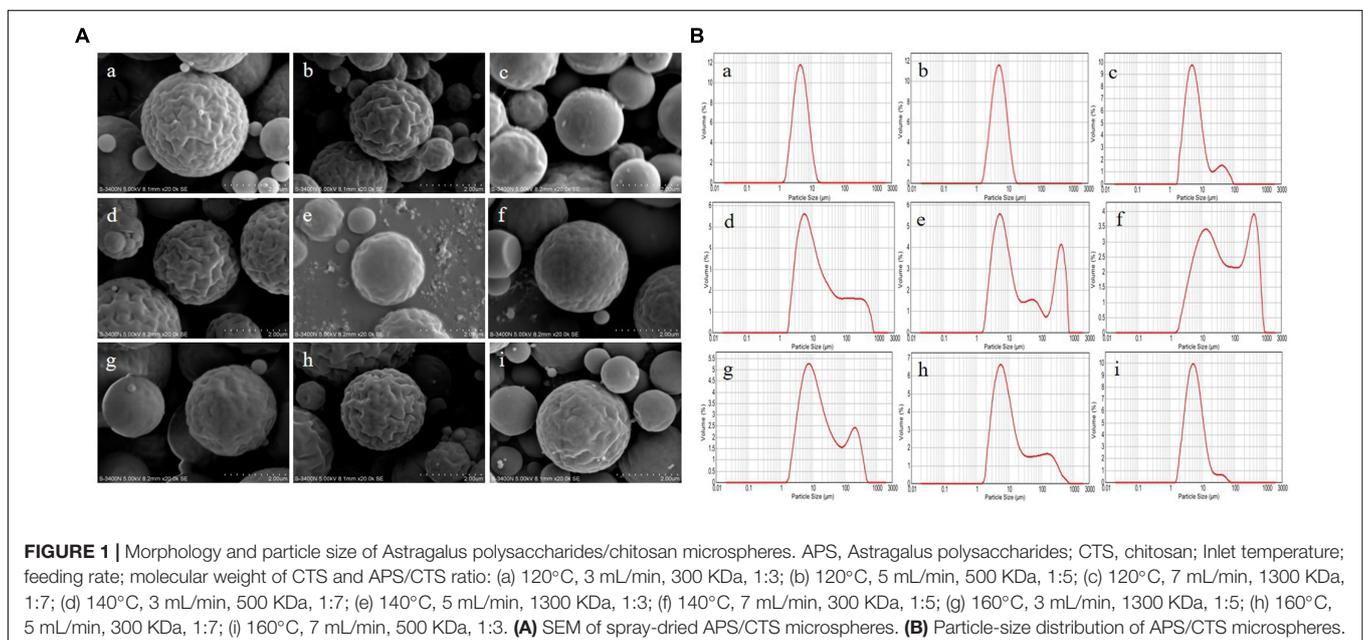
The optimization of experimental conditions was performed with regard to the DL. As shown in **Supplementary Table 2**,

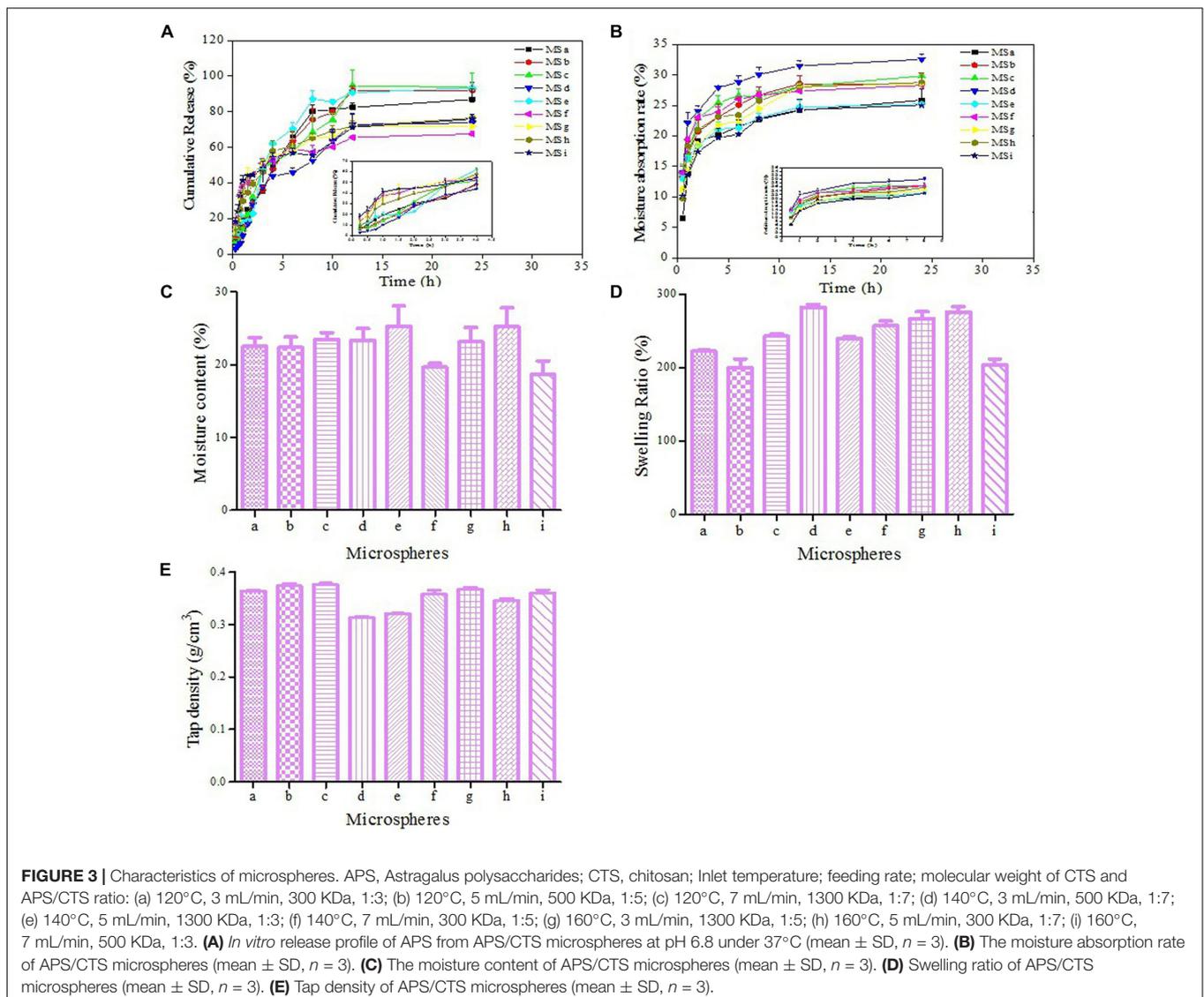
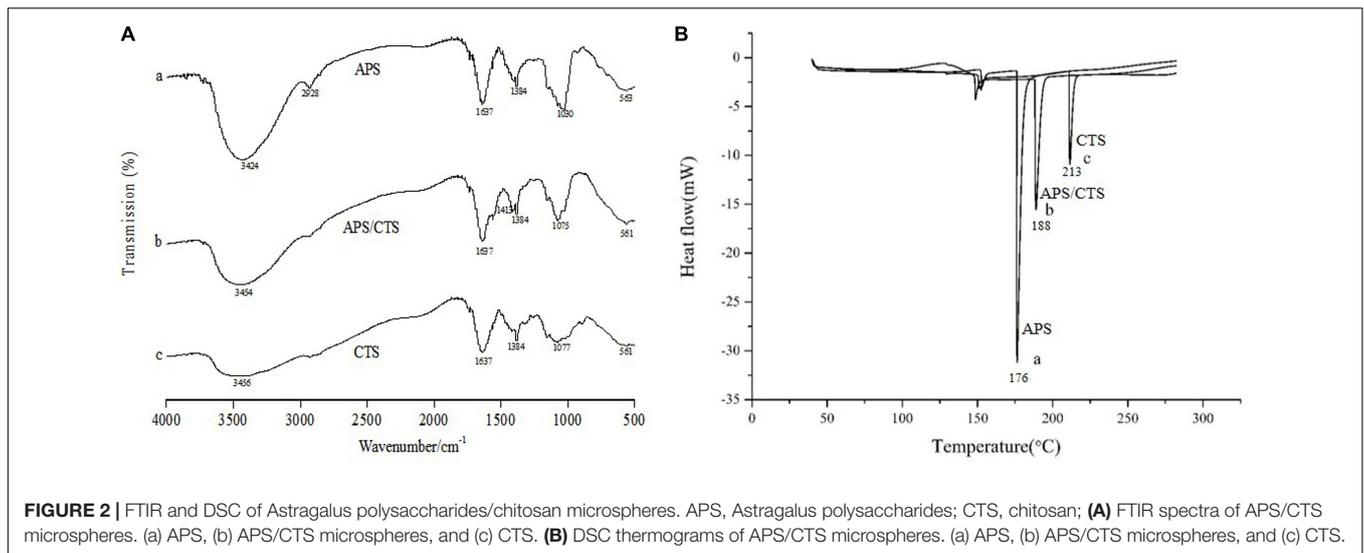
the optimal formulation was drawn: inlet temperature of 120°C, feeding rate of 3 mL/min, molecular weight of CTS of 5.0×10^2 KDa, and APS/CTS ratio of 1:3. The morphology of APS/CTS microspheres was confirmed via SEM imaging, as demonstrated in **Figure 1A**. The microspheres in every group displayed regular spherical shape and were presented in different sizes and different extents of surface roughness. The microsphere of a, b, d, and h presented considerably wrinkled surfaces; slightly wrinkled surfaces were found in microsphere e, f, g, and i; and microsphere c displayed a smooth surface. Adhesion phenomena were found in microsphere a, b, and c.

The volume size distributions of microspheres were shown in **Figure 1B**. The volume distribution of 50% [d (0.5)] of microsphere a, b, c, d, e, f, g, h, and i was 4.74, 5.28, 5.94, 11.97, 12.37, 42.02, 13.99, 8.88, and 5.68 μm , respectively. Among them, microsphere a, b, and i displayed narrow particle size distribution, and the other microspheres indicated that their size distributions were bimodal.

Results of FTIR and DSC

In **Figure 2A**, FTIR showed that spectra of pure CTS had a broad absorption band at $3,456 \text{ cm}^{-1}$ (O-H stretching vibration) and the characteristic absorptions of CTS were the bands at $1,637 \text{ cm}^{-1}$ (amide I, C-O stretching mode conjugated with -N-H deformation mode), at $1,384 \text{ cm}^{-1}$ (C-O-C stretching vibration) and at $1,077 \text{ cm}^{-1}$ (skeletal vibration involving C-O stretching). The FTIR spectra showed that the absorption peaks of APS were at $3,424 \text{ cm}^{-1}$ (O-H stretching vibration), which reflected the -inter and -intra molecular interactions of the polysaccharide, the absorptions at $2,928 \text{ cm}^{-1}$ (C-H stretching vibration) and $1,637 \text{ cm}^{-1}$ (COO^- stretching vibration). Compared with APS and CTS, the spectra of the APS/CTS microspheres showed a slight shift at 3,454 and $1,075 \text{ cm}^{-1}$. The change in the curve of the APS/CTS microspheres indicated that APS could react





with CTS (Jiang et al., 2013; Liu et al., 2017; Liao et al., 2018). The DSC thermograms of APS, CTS, and APS/CTS microspheres were shown in **Figure 2B**. A sharp endothermic peak of APS was at 176°C. The thermogram of CTS exhibited an endothermic peak at 213°C. For APS/CTS microspheres, a melting peak was observed at 188°C. These results indicated that APS and CTS had the properties of crystals. The DSC of the APS-loaded microspheres indicated a sharp endothermal peak at 188°C where no characteristic peak of APS was observed. The disappearance of the drug peak revealed that APS was entrapped or partially entrapped in the APS/CTS microspheres.

Characteristics of Microspheres

The cumulative release curves of APS were shown in **Figure 3A** and **Supplementary Table 3**. An obvious burst effect at the first 2 h was observed, and 67.48–93.76% APS was steadily released from APS/CTS microspheres at pH 6.8 within 24 h. Moisture absorption rates of all microspheres at 40°C and RH 75% were displayed in **Figure 3B**, and these were from 6.49 to 13.97% within 0.5 h. Microsphere i had the lowest moisture absorption rate at 12th h. **Figure 3C** showed that the moisture contents of all microspheres ranged from 18.59 to 25.28%. The swelling ratios of APS/CTS microspheres were revealed in **Figure 3D** and

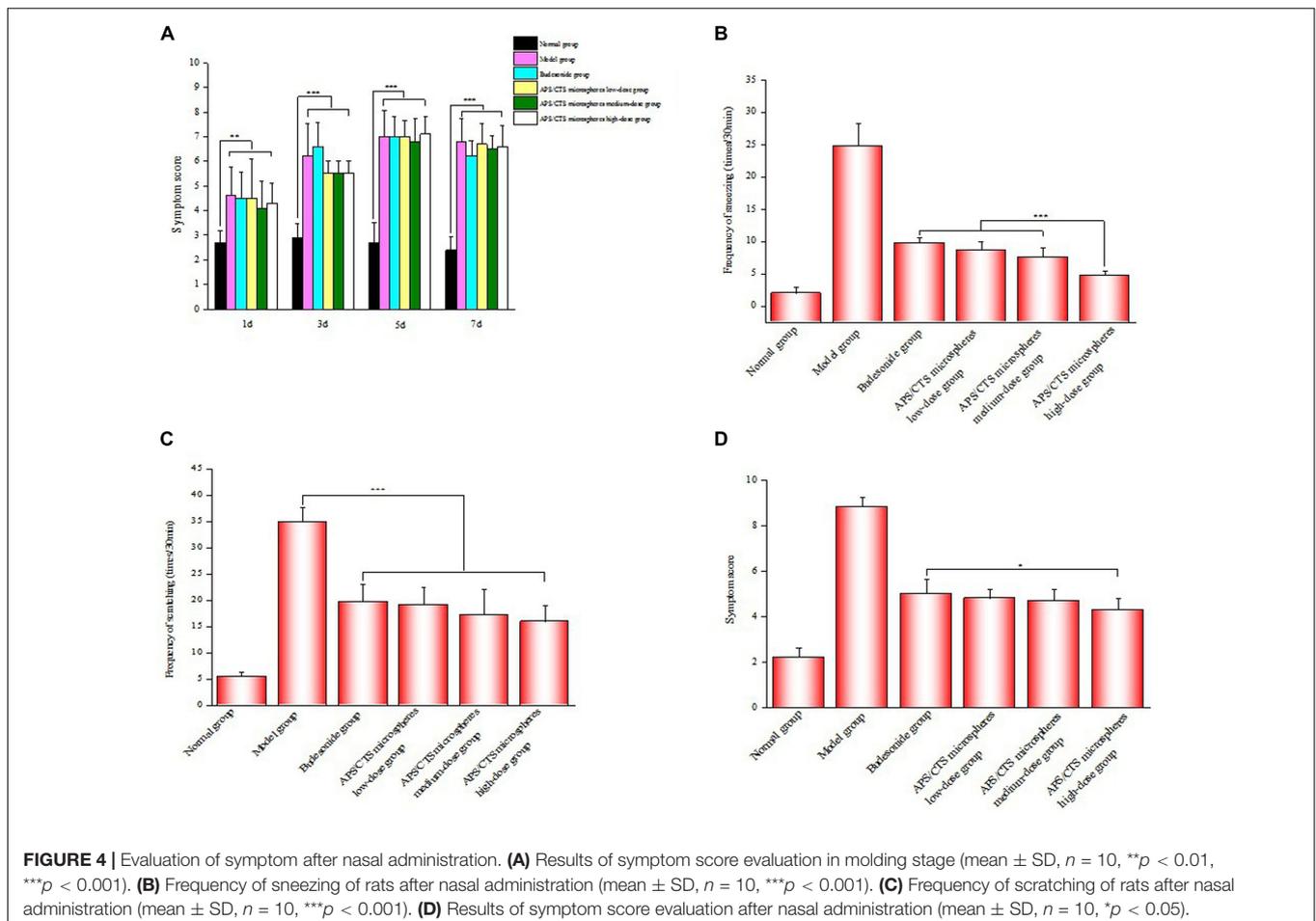
Supplementary Table 3, and they were from 200.22 to 282.22%. **Figure 3E** displayed tap densities of spray-dried microspheres ranged from 0.31 to 0.38 g/cm³.

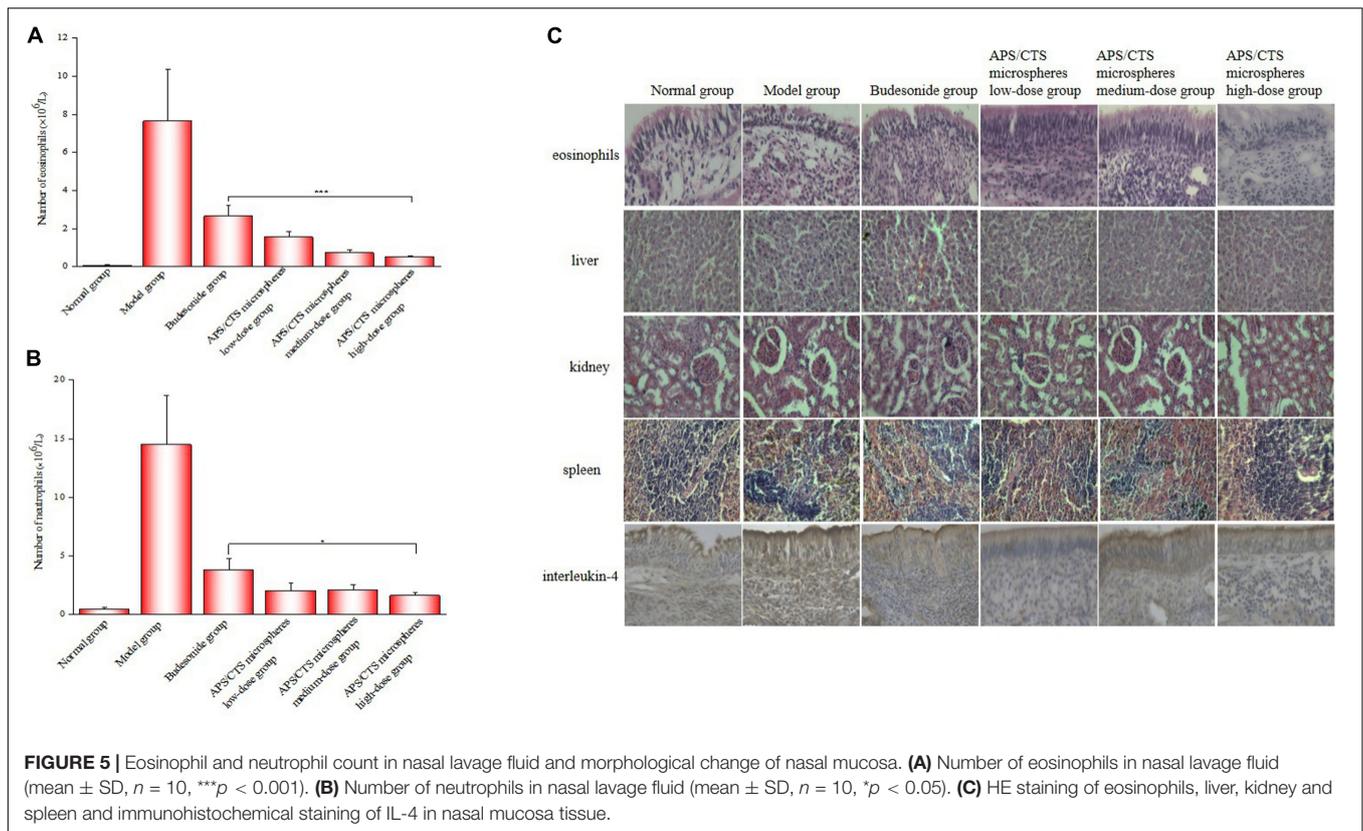
Evaluation of Symptom After Nasal Administration

The allergic symptoms of rats were scored on the 1st, 3rd, 5th, and 7th day of challenge phase (**Figure 4A**). There was a significant difference between APS/CTS microspheres (high-dose) group and budesonide group concerning the frequency of the sneezing of rats (**Figure 4B**). **Figure 4C** shows an evident difference between the budesonide group, the APS/CTS microsphere (low, medium, and high-dose) group, and the model group regarding the frequency of scratching in rats. In **Figure 4D**, an obvious difference between the APS/CTS microsphere (high-dose) group and the budesonide group about symptom score evaluation after nasal administration could be seen.

Eosinophils and Neutrophils Count in Nasal Lavage Fluid and Morphological Change of Nasal Mucosa

As was shown in **Figures 5A,B**, the APS/CTS microsphere (high-dose) group exhibited a lower number of eosinophils and





neutrophils in nasal lavage fluid compared to the budesonide group. In **Figure 5C**, a large number of eosinophils could be seen to have infiltrated into the subepithelial lamina propria, and there were submucosal vasodilation, congestion, and tissue edema in the model group; the nasal mucosa of the APS/CTS microsphere (high-dose) group displayed less infiltration of eosinophils compared to budesonide group. The structures of the liver, kidneys, and spleen treated with microspheres were normal. Compared to budesonide group, the expression of IL-4 in APS/CTS microspheres (medium, high-dose) group was significantly reduced.

DISCUSSION

Allergic rhinitis is a chronic inflammatory disease of the upper respiratory tract resulting from various environmental factors. APS can effectively correct the imbalance of Th1/Th2 cells and reduce inflammatory infiltration, and it has been widely used in the clinical treatment of AR (Liu et al., 2017; Ren et al., 2018). CTS microspheres can overcome rapid mucociliary clearance and provide longer contact time for drug transport. For example, Pandey et al. prepared and optimized CTS microspheres loaded with levocetirizine for nasal delivery with the aim to prolong residence time, increase local absorption of the drug, and improve therapeutic effects. Therefore, CTS microspheres have been extensively evaluated as a drug delivery system (Pandey and Tripathi, 2016).

In our study, APS/CTS microspheres were prepared by the spray-drying method to treat rats with AR. APS/CTS microspheres showed wrinkled surfaces, which could enable them adhere to nasal mucosal epithelial cells and prolong the drug treatment time (Liu et al., 2017). The rate of the heat transfer and water diffusion from the surface to the core of microspheres, as well as the intermediate air inlet temperature and feed flow rate, consequently influenced the microstructure of spray-dried microspheres (Behboudi-Jobbehdar et al., 2013). The size of microsphere f was 42.02 μm , and it could be administered through the nasal cavity. The DSC confirmed that APS was entrapped or partially entrapped in the APS/CTS microspheres. In terms of *in vitro* release, there was an obvious burst effect of all microspheres at the first 2 h, and 67.48–93.76% of the APS was then steadily released from APS/CTS microspheres at pH 6.8 within 24 h, which indicated that the APS/CTS microspheres were ideal for sustained-release preparations, which have the potential to prolong the action time of the drug in nasal mucosa, reduce the frequency of taking medicine, and improve patients compliance. The obvious burst effect was due to the release of APS adsorbed on the surface, and the sustained release was due to the dissolution of CTS (Zhang et al., 2007). Yu et al. (Yu et al., 2018) studied the release of proanthocyanidin from CTS microspheres, and the *in vitro* release study showed that 76.92% of proanthocyanidin was released from microspheres within 48 h. Therefore, the type of drug and the ratio of drug to the carrier will affect the release of the drug in the carrier.

Furthermore, the OVA-induced AR rat model was used to evaluate the effect of APS/CTS microspheres. Results revealed that, compared to the budesonide group, symptom scores of rats significantly reduced in the APS/CTS microspheres group. Eosinophils can invade the respiratory epithelium and produce a number of toxic mediators that may be responsible for some of the epithelial hyperplasia, hyalinosis, and damage (Johnson et al., 2007; Cho et al., 2015). Our results indicated that APS/CTS microsphere administration groups evidently reduced the infiltration of eosinophils and relieved submucosal vasodilatation and tissue edema. T lymphocytes are pivotal immune cells in allergic responses, especially Th1 and Th2. Th2 cells are characterized to secrete IL-4, which induces the production of IgE and contributes to the development of allergic inflammation (Liu et al., 2017; Shao et al., 2017). The positive signal of IL-4 in the nasal mucosa of the APS/CTS microsphere administration groups was significantly lower than that of the model group and budesonide group.

According to some studies (Senturk et al., 2018), cyclosporine nasal sprays have been used to treat AR in an animal model (54 healthy female Sprague-Dawley rats). In our study, APS/CTS microspheres were designed for nasal delivery in a total of 60 healthy Wistar rats. In the biochemical examination, Erol Senturk et al. (2018) studied the surface of the tissue tumor necrosis factor (TNF), interferon (IFN), interleukin (IL)-5, IL-13, IL-2, IL-4, IL-17A, and IgE. In a future experiment, we will further explore these responses and their application in human AR.

CONCLUSION

In this research, APS/CTS microspheres intended for nasal drug delivery were successfully prepared by the spray-drying method. The APS/CTS microspheres exhibited positive characteristics, such as uniform morphology, a particle size of 40–60 μm , which is suitable for nasal administration, and an excellent DL capacity of 9.11–21.50%. The DSC indicated that the APS was entrapped or partially entrapped in the APS/CTS microspheres. Furthermore, *in vitro* release revealed the potential of microspheres for extended release of APS. APS/CTS microspheres could alleviate allergic symptoms as well as reduce eosinophil infiltration and the expression of IL-4 in nasal mucosa of rats. In addition, APS/CTS microspheres did not display liver and kidney toxicity through HE-staining observation. Thus, our study has suggested that spray drying could serve as a simple and efficient method for preparing APS/CTS microspheres, which had excellent characteristics,

REFERENCES

- Abdel Mouez, M., Zaki, N. M., Mansour, S., and Geneidi, A. S. (2014). Bioavailability enhancement of verapamil HCl via intranasal chitosan microspheres. *Eur. J. Pharm. Sci.* 51, 59–66. doi: 10.1016/j.ejps.2013.08.029
- Behboudi-Jobbehdar, S., Soukoulis, C., Yonekura, L., and Fisk, I. (2013). Optimization of spray-drying process conditions for the production of maximally viable Microencapsulated *L. acidophilus* NCIMB 701748. *Dry Technol.* 31, 1274–1283. doi: 10.1080/07373937.2013.788509

therapeutic effects on rats with AR, and a promising potential for sustained local drug delivery. However, the study had some other limitations, and the next experimental research will be conducted by increasing sample size and studying other APS/CTS microsphere properties and how they should be applied to AR in humans.

DATA AVAILABILITY STATEMENT

The datasets generated for this study are available on request to the corresponding author.

ETHICS STATEMENT

All animal procedures were conducted in accordance with the US NIH Guidelines for the Care and Use of Laboratory Animals, and the animal study was approved by the Animal Ethical Committee of the Weifang Medical University.

AUTHOR CONTRIBUTIONS

SW prepared the APS/CTS microspheres by the spray-drying method, treated the AR of rats with them, and completed the yield, drug loading, and encapsulation efficiency of microspheres. YS performed the *in vitro* APS release studies and completed the moisture uptake and moisture content of microspheres. JZ performed the characterization of microspheres. XC, ZX, and DD performed the study of the swelling ratio and tap density of microspheres. LZ, WL, and WZ directed and planned the entire experiment.

FUNDING

This work was supported by the National Natural Science Foundation of China (Nos. 81973671 and 81774125) and Project of Collaborative Innovation Center for Target Drug Delivery System of the Weifang Medical University (2017).

SUPPLEMENTARY MATERIAL

The Supplementary Material for this article can be found online at: <https://www.frontiersin.org/articles/10.3389/fphar.2020.00230/full#supplementary-material>

- Brożek, J. L., Bousquet, J., Agache, I., Agarwal, A., Bachert, C., Bosnic-Anticevich, S., et al. (2017). Allergic rhinitis and its impact on asthma (ARIA) guidelines-2016 revision. *J. Allergy Clin. Immunol.* 140, 950–958. doi: 10.1016/j.jaci.2017.03.050
- Cho, J. S., Kang, J. H., Han, I. H., Um, J. Y., Park, I. H., Lee, S. H., et al. (2015). Antiallergic effects of trichostatin A in a murine model of allergic rhinitis. *Clin. Exp. Otorhinolaryngol.* 8, 243–249. doi: 10.3342/ceo.2015.8.3.243
- Daoud, A., Xie, Z. Z., Ma, Y. H., Wang, T. S., and Tan, G. L. (2014). Changes of T-helper type 1/2 cell balance by anticholinergic treatment in allergic

- mice. *Ann. Allergy Asthma Immunol.* 112, 249–255. doi: 10.1016/j.anaai.2013.12.014
- Fiegel, J., Fu, J., and Hanes, J. (2004). Poly(ether-anhydride) dry powder aerosols for sustained drug delivery in the lungs. *J. Control Release* 96, 411–423. doi: 10.1016/j.jconrel.2004.02.018
- Ghori, M. U., Mahdi, M. H., Smith, A. M., and Conway, B. R. (2015). Nasal drug delivery systems: an overview. *Am. J. Pharmacol. Sci.* 3, 110–119. doi: 10.12691/ajps-3-5-2
- Islam, M. A., Firdous, J., Choi, Y. J., Yun, C. H., and Cho, C. S. (2012). Design and application of chitosan microspheres as oral and nasal vaccine carriers: an updated review. *Int. J. Nanomedicine.* 7, 6077–6093. doi: 10.2147/IJN.S38330
- Jiang, H., Zhang, M., Mcknight, S., and Adhikari, B. (2013). Microencapsulation of α -Amylase by carrying out complex coacervation and drying in a single step using a novel three-fluid nozzle spray drying. *Dry Technol.* 31, 1901–1910. doi: 10.1080/07373937.2013.771365
- Johnson, V. J., Yucesoy, B., Reynolds, J. S., Fluharty, K., Wang, W., Richardson, D., et al. (2007). Inhalation of toluene diisocyanate vapor induces allergic rhinitis in mice. *J. Immunol.* 179, 1864–1871. doi: 10.4049/jimmunol.179.3.1864
- Liao, J. Z., Li, C. Y., Huang, J., Liu, W. P., Chen, H. C., Liao, S. Y., et al. (2018). Structure characterization of honey-processed astragalus polysaccharides and its anti-inflammatory activity in Vitro. *Molecules* 23, 168–178. doi: 10.3390/molecules23010168
- Liu, J. H. (2017). The influence of Astragli on the interleukin, IFN- γ and Th1Th2 balance in rats with airway inflammation. *Biomed.Res.* 28, 5831–5835. doi: 10.3382/ps/pez219
- Liu, K., Feng, Z. Q., Shan, L., Yang, T. T., Qin, M., Tang, J. B., et al. (2017). Preparation, characterization, and antioxidative activity of Bletilla striata polysaccharide/chitosan microspheres for oligomeric proanthocyanidins. *Dry Technol.* 35, 3889–3896. doi: 10.1080/07373937.2016.1269123
- Lu, J. Z., Chen, X., Zhang, Y. Y., Xu, J., Zhang, L. L., Li, Z., et al. (2013). Astragalus polysaccharide induces anti-inflammatory effects dependent on AMPK activity in palmitate-treated RAW264.7 cells. *Int. J. Mol. Med.* 31, 1463–1470. doi: 10.3892/ijmm.2013.1335
- Pandey, J., and Tripathi, P. K. (2016). Formulation and evaluation of levocetirizine loaded mucoadhesive microspheres for nasal delivery. *IJPSR* 7, 2242–2251.
- Ren, Q., Zhao, S. J., Ren, C. J., and Ma, Z. (2018). Astragalus polysaccharide alleviates LPS-induced inflammation injury by regulating miR-127 in H9c2 cardiomyoblasts. *Int. J. Immunopathol. Pharmacol.* 32, 1–11. doi: 10.1177/2058738418759180
- Seidman, M. D., Gurgel, R. K., Lin, S. Y., Schwartz, S. R., Baroody, F. M., Bonner, J. R., et al. (2015). Clinical practice guideline: allergic rhinitis executive summary. *Otolaryngol. Head Neck Surg.* 152, 197–206. doi: 10.1177/0194599814562166
- Senturk, E., Yildirim, Y. S., Dogan, R., Ozturan, O., Guler, E. M., Aydin, M. S., et al. (2018). Assessment of the effectiveness of cyclosporine nasal spray in an animal model of allergic rhinitis. *Eur. Arch. Otorhinolaryngol.* 275, 117–124. doi: 10.1007/s00405-017-4786-2
- Shao, Y. Y., Zhou, Y. M., Hu, M., Li, J. Z., Chen, C. J., Wang, Y. J., et al. (2017). The anti-allergic rhinitis effect of traditional Chinese medicine of shenqi by regulating mast cell degranulation and Th1/Th2 cytokine balance. *Molecules* 22, 1–11. doi: 10.3390/molecules22030504
- Tan, L. B., Wei, T., Yuan, A. W., He, J., Liu, J. H., Xu, D. J., et al. (2017). Dietary supplementation of astragalus polysaccharides enhanced immune components and growth factors EGF and IGF-1 in sow colostrum. *J. Immunol. Res.* 2017, 1–6. doi: 10.1155/2017/9253208
- Virtala, R., Ekman, A. K., Jansson, L., Westin, U., and Cardell, L. O. (2012). Airway inflammation evaluated in a human nasal lipopolysaccharide challenge model by investigating the effect of a CXCR2 inhibitor. *Clin. Exp. Allergy* 42, 590–596. doi: 10.1111/j.1365-2222.2011.03921.x
- Wang, W., Liu, Q. B., and Jing, W. (2019). Astragalus membranaceus improves therapeutic efficacy of asthmatic children by regulating the balance of Treg/Th17 cells. *Chin J Nat Med.* 17, 252–263. doi: 10.1016/S1875-5364(19)30029-9
- Yu, H. L., Feng, Z. Q., Zhang, J. J., Wang, Y. H., Ding, D. J., Gao, Y. Y., et al. (2018). The evaluation of proanthocyanidins/chitosan/lecithin microspheres as sustained drug delivery system. *BioMed Res. Int.* 2018, 1–11. doi: 10.1155/2018/9073420
- Zhang, W. F., Chen, X. G., Li, P. W., He, Q. Z., and Zhou, H. Y. (2007). Chitosan and Chitosan/ β -cyclodextrin microspheres as sustained-release drug carriers. *J. Appl. Polym. Sci.* 103, 1183–1190. doi: 10.1002/app.25373
- Zhang, W. F., Chen, X. G., Li, P. W., He, Q. Z., and Zhou, H. Y. (2008). Preparation and characterization of theophylline loaded chitosan/ β -cyclodextrin microspheres. *J. Mater. Sci. Mater. Med.* 19, 305–310. doi: 10.1007/s10856-006-0021-1
- Zhou, L. J., Liu, Z. J., Wang, Z. X., Yu, S., Long, T. T., Zhou, X., et al. (2017). Astragalus polysaccharides exerts immunomodulatory effects via TLR4-mediated MyD88-dependent signaling pathway in vitro and in vivo. *Sci. Rep.* 7, 44822–44834. doi: 10.1038/srep44822

Conflict of Interest: The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

Copyright © 2020 Wang, Sun, Zhang, Cui, Xu, Ding, Zhao, Li and Zhang. This is an open-access article distributed under the terms of the Creative Commons Attribution License (CC BY). The use, distribution or reproduction in other forums is permitted, provided the original author(s) and the copyright owner(s) are credited and that the original publication in this journal is cited, in accordance with accepted academic practice. No use, distribution or reproduction is permitted which does not comply with these terms.