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\*correspondence Dingjun Hao Mhdingjun@163.com

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# Effect of bone cement distribution on adjacent disc degeneration after vertebral augmentation for osteoporotic vertebral compression fractures in aging patients

Zhen Zhang, Jialang Zhang, Baorong He, Qi Dong and Dingjun Hao<sup>\*</sup>

Department of Spine Surgery, Xi'an Honghui Hospital, School of Medicine, Xi'an Jiaotong University, Xi'an, China

**Background:** The influence of vertebral augmentation on adjacent intervertebral discs remains controversial. The purpose of this study is to evaluate the effect of bone cement distribution on adjacent disc degeneration after vertebral augmentation for osteoporotic vertebral compression fractures (OVCFs).

**Methods:** Patients with single level OVCF and upper endplate injury who underwent vertebral augmentation were enrolled. The patients were divided into four groups: Group A: bone cement contacted both the cranial and the distal endplates; Group B: bone cement only contacted the cranial endplate; Group C: bone cement only contacted the distal endplate; and Group D: bone cement contacted neither the cranial nor the distal endplates. The cranial discs of the fractured vertebrae were defined as adjacent discs and the upper discs proximally to the adjacent discs were defined as control discs. Degenerative disc change (DDC) was defined as a deteriorated postoperative Pfirrmann score compared with the preoperative score on MR images. The number of DDC cases and the disc heights were analyzed among the groups.

**Results:** A total of 184 patients with an average follow-up time of 28.6 months were included. The number of DDC cases in the adjacent discs was significantly higher than in the control discs in groups A (p < 0.001), B (p = 0.002), and D (p = 0.028), whereas the difference in group C was not statistically significant (p = 0.237). The incidence of adjacent disc degeneration was significantly higher in group A than that in group C (p = 0.06). The adjacent disc heights decreased significantly in groups A, B, and D (p < 0.001, p < 0.001, and p = 0.012, respectively), but did not decrease significantly in group C (p = 0.079). However, no statistical differences were detected among the four groups with respect to the preoperative adjacent disc height, follow-up adjacent disc height.

**Conclusion:** Bone cement distribution influences adjacent disc degeneration after vertebral augmentation in OVCFs. Cement distribution proximal to the injured endplate can accelerate adjacent disc degeneration, and cement in contact with both the cranial and distal endplates can induce a higher incidence of adjacent disc degeneration.

#### KEYWORDS

cement distribution, disc degeneration, vertebral augmentation, osteoporotic vertebral compression fractures, vertebroplasty

## Introduction

Osteoporotic vertebral compression fractures (OVCFs), one of the most common and severe complications of osteoporosis, are becoming more common among the aging population. Vertebral augmentation was first applied by American doctors in patients with OVCFs in 1993 and obtained satisfactory efficacy. Since then, vertebral augmentation techniques, including percutaneous vertebroplasty and posterior kyphoplasty, have been widely used in the treatment of OVCFs and have received international recognition. Several studies show that vertebral augmentation improves clinical outcomes because it can achieve instant pain relief and stabilization of the fractured vertebral body (1-4). Nevertheless, several reports have indicated that vertebral augmentation may negatively affect adjacent segments (5, 6). Previous studies have mainly focused on the influence of vertebral augmentation on the adjacent vertebral body, as cement injection has been reported to increase the risk of adjacent vertebral fractures. Recently, the impact of vertebral augmentation on adjacent intervertebral discs, which has rarely been discussed, has been increasingly concerning. However, several studies that have attempted to determine whether vertebral augmentation can aggravate the degeneration of adjacent intervertebral discs have reached contradictory conclusions. Qian et al. (7) first conducted a prospective study and discovered a significantly higher incidence of adjacent disc degeneration above the fractured vertebrae in the cement augmentation group than in the control group. These findings were confirmed by retrospective studies by Lu et al. (8) and Wang et al. (9). However, a long-term follow-up study by König et al. (10), come to a different conclusion that vertebral cement augmentation through kyphoplasty had no significant influence on disc degeneration.

Cement distribution pattern is reportedly related to the occurrence of adjacent vertebrae fracture (11-14). These studies indicated that the cement distribution pattern may have an impact on the regional biomechanical stress. Moreover, cement distributed along the endplates can interfere with the endplate nutritional pathway and induce intervertebral disc degeneration in porcine and rabbit models (15, 16). Thus, the distribution of cement, which might have an impact on adjacent discs by altering both the regional biomechanical stress and the endplate nutritional pathway, should not be ignored when discussing the influence of vertebral augmentation on adjacent disc degeneration. Neglecting cement distribution patterns can lead to biased conclusions. However, to our knowledge, the influence of the cement distribution pattern on adjacent intervertebral discs has never been discussed. This study aimed to evaluate the effect of bone cement distribution on adjacent disc degeneration after vertebral augmentation in osteoporotic vertebral compression fractures.

# Materials and methods

#### Study population

Clinical data and radiographic images of patients with OVCF who underwent vertebroplasty at our spine surgery center between January 2015 and December 2020 were retrospectively reviewed. As endplate injury has been reported to affect intervertebral disc degeneration (17), we only included patients with upper endplate injuries in this study to reduce bias. The inclusion criteria were as follows: (1) patients with low back pain who were diagnosed with a fresh single vertebral compression fracture of the lumbar spine (L1-L5) with upper endplate injury, and with no compression of the spinal cord or cauda equina; (2) age  $\geq$ 55 years; (3) bone mineral density (BMD) of lumbar spine *T* score  $\leq -2.5$ ; (4) Pfirrmann score of the adjacent intervertebral discs above the fractured vertebral body  $\leq 2$ ; (5) at least 2 years follow-up. The exclusion criteria were as follows: (1) vertebral pathological fracture caused by infection or tumor, (2) previous history of lumbar vertebral fracture or lumbar surgery, (3) cement leakage into intervertebral discs, (4) severe adjacent disc injury, and (5) cement concentrated on one side of the vertebral body on the frontal x-ray image.

#### **Operation procedure**

All PVP procedures were performed using a unilateral transpedicular approach, with the patient in the prone position under local anesthesia. The fractured vertebrae were located, and a puncture needle was inserted through the unilateral pedicle paths under the guidance of C-arm fluoroscopy. The end of the needle was located in the middle of the vertebra on the anteroposterior film, and at 1/3 anterior-mid of the vertebral body on the lateral film. High-viscosity bone cement was slowly injected into the vertebral body using a hydraulic delivery system. After the injection was completed, the needle was removed, and the cement volume was recorded.

# Evaluation of clinical and radiological parameters

Age, sex, body mass index (BMI), number of smokers, and fracture segments were recorded. All patients were followed up for at least 2 years after surgery. Radiography, computed tomography, and MR imaging were performed before surgery. Radiographs were obtained on the first day, 3 months, 1 year, and 2 years after surgery, and MRI scans were performed only at the last follow-up visit for economical reasons.

The cranial discs of the fractured vertebrae were defined as adjacent discs and the upper discs proximal to the adjacent discs were defined as control discs (Figure 1). The degree of disc degeneration was evaluated using the Pfirrmann scoring system (18). Degenerative disc change (DDC) was defined as a deteriorated postoperative Pfirrmann score compared with the preoperative score (excluding deterioration from grade 1 to grade 2). Disc height was defined as the mean of the anterior, middle, and posterior disc heights on midsagittal T1W MR, according to a previous report (8).

#### Grouping method

According to lateral radiographs taken on the first day after surgery, patients were divided into four groups. Group A: bone



FIGURE 1 Definition of adjacent discs and control discs. In the mid-sagittal view of MRI, L1 was the fractured vertebral body, T12/L1 (\*) disc was defined as the adjacent disc, and T11/T12 ( $\circ$ ) disc was defined as the control disc.

cement contacted both the cranial and the distal endplates; Group B: bone cement only contacted the cranial endplate; Group C: bone cement only contacted the distal endplate; and Group D: bone cement located in the middle of the vertebral body, contacting neither the cranial nor distal endplate. In this study, "contact" was defined as bone cement covering at least 50% of vertebral endplates on lateral x-ray images (Figure 2).

#### Statistical analysis

Statistical analyses were performed using SPSS 26.0 (Chicago, Armonk, NY, USA). Continuous variables are presented as mean  $\pm$  standard deviation (SD). Counting data are expressed as numbers. The Kruskal-Wallis test was used to analyze patient age, BMI, time of follow-up, bone cement volume, and disc height among the groups. Pearson's chi-square test or Fisher's exact test was used to compare patient sex, number of smokers, fracture segment, and number of DDCs. Differences were considered statistically significant at p < 0.05.

## Results

A total of 184 patients including 51males and 133 females were finally enrolled in this study. The mean follow-up period was 28.6 months (ranging from 24 to 49 months). There were 73 patients in group A, 62 patients in group B, 28 patients in group C, and 21 patients in group D. No significant differences were found among the groups with respect to age, sex ratio, BMI, number of smokers, fracture segment, or follow-up time (Table 1).

At the final follow-up, 102 (55.4%) patients were found to have degeneration of the adjacent disc, of whom 48 (65.8%) were in group A, 32 (51.6%) in group B, 10 (35.7%) in group C, and 12 (57.1%) in group D. Forty-eight (26.1%) patients had control disc degeneration, of whom 22 (30.1%) were in group A, 15 (24.2%) in group B, 6 (21.4%) in group C, and 5 (23.8%) in group D. The number of DDC cases in the adjacent discs was significantly higher than in the control discs in groups A (p < 0.001), B (p = 0.002), and D (p = 0.028), whereas the difference in group C was not statistically significant (p = 0.237). The number of DDC cases in the adjacent discs was not significantly different among the four groups (p = 0.775). However, the number of DDC cases in the adjacent discs, was significantly different among the four groups (p = 0.047). The number of DDC cases was significantly higher in group A than



#### FIGURE 2

Four types of bone cement distribution: (A) bone cement contacted both the cranial and the distal endplates; (B) bone cement only contacted the cranial endplate; (C) bone cement only contacted the distal endplate; (D) bone cement contacted neither the cranial nor the distal endplate.

Characteristics	Group A ( <i>n</i> = 73)	Group B ( <i>n</i> = 62)	Group C ( <i>n</i> = 28)	Group D ( <i>n</i> = 21)	p value
Age	$64.4 \pm 6.2$	$66.0 \pm 6.4$	$64.8 \pm 6.4$	$64.9 \pm 7.4$	0.443
Gender (male/female)	20/53	17/45	10/18	4/17	0.640
BMI (kg/m <sup>2</sup> )	$22.0\pm4.2$	$21.5 \pm 3.4$	$23.3 \pm 2.5$	21.1 ± 3.3	0.312
Smoker number	11	7	3	1	0.208
Fracture segment					0.881
L1	32	30	17	9	
L2	22	16	5	6	
L3	10	11	4	2	
L4	7	4	2	4	
L5	2	1	0	0	
Bone cement volume (ml)	$4.8 \pm 1.1$	$4.1 \pm 1.3$	$4.6 \pm 1.8$	$4.7 \pm 1.5$	0.195
Follow-up period (months)	$30.3 \pm 6.1$	$27.2 \pm 5.2$	26.1 ± 3.9	$29.9\pm5.0$	0.387

TABLE 1 Demographic and clinical characteristics of patients.

TABLE 2 Numbers of DDC cases in adjacent discs and control discs at follow-up.

		Group A	Group B	Group C	Group D	<i>p</i> value
Adjacent disc	DDC	48	32	10	12	0.047
	Non DDC	25	30	18	9	
Control disc	DDC	22	15	6	5	0.775
	Non DDC	51	47	22	17	
p value		< 0.001	0.002	0.237	0.028	

that in group C (p = 0.06). The difference in the DDC number in the adjacent discs between groups A and B (p = 0.096), groups A and D (p = 0.469), groups B and C (p = 0.162), groups B and D (p = 0.661), and groups C and D (p = 0.136) was not statistically significant (Table 2).

The adjacent disc heights decreased significantly in groups A, B, and D (p < 0.001, p < 0.001, and p = 0.012, respectively), but did not decrease significantly in group C (p = 0.079). The follow-up control disc heights were not significantly different from the preoperative control disc heights in all of the four groups (p = 0.089, p = 0.138, p = 0.269, and p = 0.301, respectively). No statistical difference was detected among the four groups with respect to the preoperative control disc height, follow-up adjacent disc height, preoperative control disc height, nor follow-up control disc height (p = 0.346, p = 0.519, p = 0.496, p = 0.218, respectively) (Table 3).

TABLE 3 Adjacent disc heights and control disc heights preoperatively and at follow-up.

	Group A	Group B	Group C	Group D	p value		
Adjacent disc height							
Preoperative	$6.9 \pm 1.9$	$6.6 \pm 1.8$	$6.5 \pm 1.5$	$6.4 \pm 1.4$	0.346		
Follow-up	$6.1 \pm 1.7$	$6.0 \pm 1.8$	$6.2 \pm 1.7$	$6.0 \pm 1.5$	0.519		
p value	< 0.001	< 0.001	0.079	0.012			
Control disc height							
Preoperative	$5.7 \pm 1.8$	$5.7 \pm 1.6$	$6.0 \pm 1.9$	$5.3 \pm 1.7$	0.496		
Follow-up	$5.3 \pm 1.6$	$5.4 \pm 1.7$	$5.8 \pm 1.7$	5.1 ± 1.9	0.218		
p value	0.089	0.138	0.269	0.301			

#### Discussion

The advantages of the VCA include its minimally invasive nature, good biomechanical support, and satisfactory clinical outcomes. Regarding the adverse effects of vertebral augmentation, researchers have mainly focused on intraoperative complications, such as cement extravasation, and the postoperative negative effects of cement injection on adjacent vertebral bodies (6, 19). The influence of vertebral augmentation on adjacent intervertebral discs has rarely been discussed in previous studies. A prospective study of 97 patients conducted by Qian et al. (7) compared the grade of disc degeneration above the fractured vertebra on MR between the PVP t and conservative treatment groups. They discovered that the incidence of degeneration of the adjacent intervertebral disc above the fractured vertebra was significantly higher in the vertebral augmentation group than in the control group (52.5% vs. 29.0%). Similar results were indicated in retrospective studies conducted by Pachowsky et al. (20), Lu et al. (8), and Wang et al. (9). However, a long-term follow-up study by König et al. (10) found that vertebral cement augmentation using PKP had no significant effect on disc degeneration. As König's study included discs with preoperative Pfirrmann grade  $\geq$ 3, the endplate nutrition could have already been affected and could cause bias in evaluating the actual effect of cement augmentation. Li et al. (17) suggested that adjacent disc degeneration might be attributable to the endplate injury of the fractured vertebrae, which was ignored in the above studies. The design defects of the aforementioned studies might be the reason for the

discordance in the results. Furthermore, previous studies did not consider one key factor-cement distribution-that might have an impact on adjacent discs by altering both the nutrient supply to the discs and local biomechanics. To determine the effect of bone cement distribution on adjacent intervertebral disc degeneration after vertebral augmentation, we used strict inclusion criteria to reduce potential bias. In our study, we included patients only with upper endplate injuries and the Pfirrmann score of the adjacent discs  $\leq 2$ . Additionally, endplate injuries are often accompanied by disc injuries, which have been proven to have an important impact on disc degeneration (21) and could therefore influence the evaluation of the actual effect of cement augmentation. Therefore, the influence of disc injuries should be considered. Therefore, patients with severe adjacent disc injury were excluded, and the DDC definition excluded deterioration from grade 1 to grade 2 Pfirrmann scores to further diminish the bias induced by the potentially inaccurate evaluation of the preoperative Pfirrmann score of injured discs on MR.

Several patient characteristics, such as age, sex, body weight, and smoking, have been reported as risk factors for intervertebral disc degeneration (22, 23). In this study, these risk factors were evaluated to improve the reliability of our conclusions. None of these characteristics showed statistically significant difference among the four groups. In the present study, the incidence of degeneration in control discs was not significantly different among the four groups. The number of DDC cases in adjacent discs was significantly higher than that in control discs in groups A, B, and D, but the difference between adjacent and control discs in group C was not statistically significant. These results suggested less severe degenerative changes in the adjacent discs in group C. Further analysis showed a significant difference in the incidence of adjacent disc degeneration among groups A, B, C, and D. Compared with group C, patients in group A had a significantly higher number of DDC cases. Patients in groups B and D also had a higher number of DDC cases than those in group C, although the difference was not statistically significant. These results indicate that vertebral augmentation has an impact on adjacent disc degeneration, which is largely influenced by bone cement distribution. Cement distribution proximal to the injured endplate could accelerate the adjacent disc degeneration, and cement in contact with both the cranial and distal endplates might have a greater adverse impact on adjacent discs. However, cement distributed distally to the injured endplate may have no significant influence on disc degeneration. The alteration in the adjacent disc height further supports this conclusion. The adjacent disc heights decreased significantly at follow-up compared with baseline in groups A, B, and D, whereas the decrease in group C was not statistically significant. However, the control discs, did not exhibit a significant decrease in disc heights. These results were consistent with those of previous reports (9, 17), and further proved the fewer degenerative changes in the adjacent discs in group C. However, the adjacent disc heights at follow-up were not significantly different among the four groups. This might be attributed to the comparatively

short follow-up time, as the adjacent disc degeneration was still in the early stages and the decrease in disc height was minor. Similarly, in a previous report with comparable follow-up time (2 years), the height loss of adjacent disc in the vertebral augmentation group was not significantly different from that in the control group (7). Disc height is not strongly related to Pfirrmann scores from grade 1 to 4, and only significantly differentiate between grade 4 and 5 Pfirrmann scores (24, 25). However, no disc degenerated to grade 5 at final follow-up in this study, that might make the disc height change less significant. Significant disc height loss and high-grade disc degeneration were observed in some studies with long-term follow-up (ranging from 8 to 17 years) (26–28). Thus, prolonging the follow-up time may be helpful to observe the differences of disc height change among the four groups.

However, the pathogenesis of disc degeneration remains unclear. Nevertheless, alteration of local biomechanics and impairment of nutrient supply have been suggested to accelerate adjacent disc degeneration after vertebral augmentation according to previous reports. Biomechanical studies have shown significant decreases in adjacent disc pressure after vertebral fractures (29-31). A finite-element study by Luo et al. (29) reported that vertebral injury reduced the intradiscal pressure at the affected level to an average of 47% of the pre-fracture values. These results are consistent with those of previous studies (30, 31). Bone cement augmentation can enhance strain on the intervertebral disc by increasing the elastic modulus of the injured endplate and further altering the local biomechanical profile. A finite element study by Polikeit et al. (32) showed that the maximum pressure increased by 16% above the treated level and by 13% below the treated level. Ananthakrishnan et al. (30) also reported an increased nuclear pressure after augmentation treatment. Similar results have been reported in other finiteelement studies (31, 33, 34). Thus, cement distribution closer to the injured cranial endplate in groups A, B, and D may have made the endplates stiffer and induced a higher incidence of adjacent disc degeneration. Bone cement distributed distal to the injured endplate, as shown in group C, would accordingly exert less stress on the adjacent disc and therefore induce less disc degeneration. Additionally, clinical studies have suggested a correlation between disc degeneration and increased adjacent bone density (35, 36). Previous studies also reported that cement distribution close to the endplate is associated with a higher risk of adjacent vertebral fractures (13, 37). Sun et al. (13) reported that cement distribution proximal to the adjacent vertebral body (distributed at the disc level or endplate level) could increase the risk of post- vertebroplasty fractures in adjacent vertebral bodies. Similarly, Zhao et al. (37) found that the diffusion of bone cement into cracks in the injured endplate may increase the incidence of adjacent vertebral fractures. These results further explain the differences in the numbers of DDC cases induced by different cement distribution patterns. Furthermore, bone cement in group A contacted both the cranial and distal endplates could induce to higher elastic modulus as there were no "buffering bones", which might exert greater stress on peripheral structures and thus induce to greater disc degeneration.

Impairment of the nutrient supply to the disc has been identified as another important factor affecting adjacent disc degeneration. As the largest inert structure, the intervertebral disc is largely dependent on endplate diffusion for nutrient supply (38), and can be impaired by cement augmentation by damaging the capillaries underneath the endplate. Signs of adjacent disc degeneration followed vertebral augmentation were reported (15, 16). However, conclusions from adult animal models (goats, sheep, and dogs) are contradictory (39-41). Because the vertebrae in these animal models were intact, these conclusions may not be applicable to fractured vertebrae. Our study indicated that a combination of vertebral fracture and cement distribution proximal to the injured endplate may be required to influence the nutrient supply and accelerate the degeneration, as the incidence of disc degeneration increased in groups A, B, and D, but not in group C.

This study had several limitations. First, the strict inclusion and exclusion criteria may have led to sampling bias and comparatively small sample sizes in the subgroups. Second, the distribution of bone cement was only evaluated on x-ray films, owing to the lack of postoperative CT images. Third, the severity of endplate injuries was not evaluated due to the lack of a proper rating system, which may have resulted in biased results. Fourth, the average follow-up time was relatively short, which may not have been sufficient to fully evaluate the degenerative condition of the adjacent discs. As no disc degenerated to grade 5 in this study, it might make the disc height change less significant.

### Conclusion

The present study suggests that bone cement distribution influences adjacent disc degeneration after vertebral augmentation in osteoporotic vertebral compression fractures. Cement distribution proximal to the injured endplate can accelerate adjacent disc degeneration, and cement in contact with both the cranial and distal endplates can induce a higher incidence of adjacent disc degeneration.

### Data availability statement

The original contributions presented in the study are included in the article/Supplementary Material, further inquiries can be directed to the corresponding author.

# References

### Ethics statement

The studies involving humans were approved by the Ethics Committee of Xi'an Honghui Hospital, School of Medicine, Xi'an Jiaotong University. The studies were conducted in accordance with the local legislation and institutional requirements. The participants provided their written informed consent to participate in this study.

## Author contributions

ZZ: Data curation, Funding acquisition, Writing – original draft, Project administration. JZ: Data curation, Writing – review and editing. BH: Writing – review and editing, Methodology, Project administration, Supervision. QD: Writing – review and editing, Data curation. DH: Methodology, Project administration, Supervision, Writing – review and editing.

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# Conflict of interest

The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

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